

Integration of a polarizable interface for electrophoretic separation in a microfluidic device

Qiongdi Zhang

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Integration of a polarizable interface for electrophoretic separation in a microfluidic device

Thèse de doctorat de l'Université Paris-Saclay préparée à l'Université Paris-Sud

École doctorale n°575: Electrical, optical, bio-physics and engineering (EOBE) Spécialité de doctorat: électronique et optoélectronique, nano- et microtechnologies

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Titre : Intégration d'une interface polarisable pour la séparation électrophorétique dans un dispositif microfluidique

Mots clés : CNx, interface polarisable, transistor fluidique, microfluidique, flux électroosmotique

Résumé : L'électrophorèse est une technique puissante permettant de séparer des biomarqueurs liquides présents dans les biologiques. L'électrophorèse de zone libre transporte des molécules en milieu liquide sous l'influence de deux contributions : le flux électrophorétique et le flux électroosmotique (EOF). C'est ce dernier flux EOF qui permet d'optimiser la résolution analytique de la séparation et donc de simplifier le mélange avant sa détection. Notre équipe a développé un contrôle en temps réel de l'EOF en intégrant une interface polarisable diélectrique dans un dispositif microfluidique. Le carbone amorphe azoté (CNx avec x=15%) a été choisi comme ce matériau. Comme le CNx ne peut pas être déposé directement sur un substrat de verre à cause de sa faible adhérence, deux matériaux différents ont été proposés comme couche d'accroche : le carbure de silicium (SiC) et le platine (Pt). Nous avons tout d'abord optimisé l'adhésion entre le film CNx et la couche d'accroche SiC par différentes procédures

de fabrication. Cependant, en raison d'une faible adhérence, le film CNx s'est rapidement décollé en électrolyte liquide. Par contre, nous avons prouvé que certaines architectures hybrides incluant du Pt dans la couche d'accroche sont incroyablement robustes. Même après deux mois dans une solution millimolaire de KCl, le CNx adhérait toujours au verre sans aucune trace de délamination. Ce dispositif a fourni aussi une grande fenêtre de polarisabilité (de -1V à +1V). Nous avons enfin développé une architecture hybride « couche d'accroche isolée/couche électriquement polarisable /électrodes de grille enterrées/ polymère » afin d'éviter toute perte faradique dans l'électrolyte liquide ou vers les circuits conducteurs du dispositif. A l'issue de ces travaux, nous pensons être en mesure de proposer un composant fluidique complexe et robuste qui permet une modulation en temps réel de l'EOF lors de migrations électrophorétiques.

Title : Integration of a polarizable interface for electrophoretic separation in a microfluidic device

Keywords : CNx, polarizable interface, fluidic transistor, microfluidic, electroosmotic flow

Abstract : Electrophoresis is currently an efficient way to separate precious biomarkers from complex mixtures. It takes place to transport molecules under two contributions: the electrophoretic flow and the electroosmotic flow (EOF). The latter allows to optimize the analytical resolution of the separation. Our team has developed a real-time dynamic control of the EOF by integrating a dielectric polarizable interface in the microfluidic device. Amorphous carbon nitride (CNx with x=15%) has dielectric properties and was chosen to be the polarizable interface. Since it cannot be deposited directly onto glass substrate, we have proposed and studied two different materials as the sticking underlayer: silicon carbide (SiC) and platinum (Pt). In the case of SiC, we have optimized the adhesion between CNx film and SiC underlayer through different fabrication procedures.

However, due to poor adhesion, CNx film delaminated into liquid electrolyte quickly. Compared to SiC, Pt is a good sticking underlayer for CNx. It was found out that even after two months in KCl solution, CNx still stuck robustly to Pt. Meanwhile, the device provided a large window of polarizability (from -1V to +1V). Finally, to avoid any faradic loss in the liquid electrolyte or towards the conductive circuitry of the device, we have developed a sticking underlayer/electrically polarizable/polymeric hybrid architecture. This architecture appears to be the most robust existing polarizable interface for strong and long-term adhesion onto glass substrates.

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Abstract

Medical check-up and diagnostics require multiplexed sample treatments and high-resolution separations. After the separation steps, a sensitive detection of the biomarkers has to be carried out. One way to efficiently separate precious biomarkers from complex mixtures that are currently used by biochemists is electrophoresis. Electrophoresis takes place to transport molecules under two contributions: the electrophoretic mobility that is directly related to the ratio between weight and charge of molecules and the electroosmotic mobility that allows to optimize the analytical resolution of the separation. Most of the time analysts modulate electroosmotic flow (EOF) by adjusting pH of solution, or changing the ionic strength of buffer, or just using surface treatments. All these methods aim to tune the electrostatic charge state of the solid/liquid interface and to limit unspecific adsorption inside the microfluidic channel. However, these strategies cannot lead to real-time surface charge adjustment. Therefore, in our microfluidic transistor, a dielectric polarizable interface is integrated in order to achieve a dynamic control of the EOF. Such polarizable gate allows a real-time modulation of the zeta potential at the solid/liquid electrolyte interface under the application of low voltage. This fluidic transistor with its integrated gate voltage is thus engineered for a fast and efficient control of EOF independently from the electrophoretic field. Amorphous carbon nitride (CNx with x=15%) has been chosen to be the dielectric polarizable material for the gate. Since the CNx cannot be deposited directly on glass substrate, two different materials have been proposed and studied as sticking underlayer: silicon carbide (SiC) and platinum (Pt). In this work, we have studied the behavior of CNx film deposited on these two different materials for different architectures of the device. Due to poor adhesion between CNx and SiC, CNx film quickly delaminated into the liquid electrolyte. Compared to SiC, Pt is a good sticking underlayer for CNx that was found to be incredibly robust. Even after two months in KCl solution, CNx still adhered to Pt without any delamination. Moreover, to avoid any faradic loss in the liquid electrolyte or towards the conductive circuitry of the device, we have developed a hybrid architecture with polymeric insulating pads at the two extremities of the CNx gate electrode. This sticking layer/electrically polarizable/polymeric hybrid architecture appears to be the most robust existing polarizable interface for strong and long-term adhesion onto glass substrates.

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Abbreviations

- AC alternating current
- AFM atomic force microscopy
- CCD charge-coupled device
- CE capillary electrophoresis
- COC cyclic olefin copolymer
- COP cyclic olefin polymer
- DC direct current
- EBPVD electron-beam physical vapor deposition
- EDL electrical double layer
- EDS energy-dispersive X-ray spectroscopy
- EOF electroosmotic flow
- EP electrophoresis
- FET field effect transistor
- FFET flow field effect transistor
- HMDS hexamethyl disilazane
- HPCE high performance capillary electrophoresis
- IC integrated circuit
- IPA isopropyl alcohol
- LOC lab-on-a-chip
- MEMS micro-electro-mechanical systems
- MIE metal-isolator-electrolyte
- µFWB microfluidic Wheatstone bridge
- μTAS micro total analysis system
- NEMS nano-electro-mechanical systems

Opamp operational amplifier

- PC polycarbonate
- PCB printed circuit board
- PDMS poly (dimethyl siloxane)
- PEEK polyether-ether-ketone
- PET poly (ethylene terephthalate)
- PI polarizable interface
- PIA particle image anemometry
- PMMA poly (methyl methacrylate)
- POC point-of-care
- PS polystyrene
- PVC polyvinyl chloride
- PVD physical vapor deposition
- RF radio frequency
- RIE reactive-ion etching
- ROI region of interest
- RPM revolutions per minute
- UV ultraviolet
- XPS X-ray photoelectron spectroscopy

Chapter 0: General Introduction

For decades, benefitting from the advances in micro-electro-mechanical systems (MEMS), nanoelectro-mechanical systems (NEMS) and integrated circuit (IC) industries technologies, microfluidic technology has become an important tool for chemical, biological and medical researches. Meanwhile, capillary electrophoresis (CE) is a high-performance separation method for those analytical studies in liquid. One way to further improve this analytical method concerns the ability to control the electroosmotic flow (EOF) that competes with the electrophoretic flow. To achieve a dynamic realtime manipulation of the EOF, a gate electrode that is similar to the gate in electronics was integrated into a microfluidic device, called "flow field effect transistor" (FFET) [1]. Researchers have then developed different FFET variants. Among them, our team designed a polarizable interface FFET (PI-FFET) that integrated a polarizable material (CNx) as the gate of the device [2]. On the other hand, printed circuit board (PCB) technology has greatly reduced the space and weight of ICs. By combining a functional PCB with the PI-FFET device, it will be one day possible to realize a portable, space-saving, efficient and mass-production microfluidic separation analytical device. Before that, an urgent problem to be solved concerns the robustness of the transistor itself. In contact with aqueous liquids we observed delamination of the PI from the substrate. Indeed, the older generation of PI-FFET lasted no more than ten days. It is too short and its performances were not reliable after few days. In other words, the choice of the building materials and the architecture of the PI-FFET has to be fully thought over and it was the aim of this project.

Amorphous carbon nitride (CNx with x = 15%) as a dielectric polarizable material has rarely been studied to be integrated in a complex microfabricated device. As a pioneer to use such a material as gate material, along my PhD work, I have studied the way to improve its adhesion ability to the glass substrate. I have thus studied the roles of various factors of environment, of the fabrication process and of the material itself on CNx adhesion stability. I have also developed specific fabrication processes to integrated at the glass/CNx interface different underlayers.

The whole manuscript is divided into five sections.

Chapter 1 mainly introduces the background of microfluidic separation and the methods to improve it. The first Flow FET device is described as well as the birth of our PI-FFET device. Chapter 1 also gives a glance at the design structure and the EOF measurement method of the PI-FFET.

Chapter 2 simply presents a simplification of the EOF measurement equipment. It was done during the 1st year of my PhD to replace two classical electronic voltage followers by a small light printed circuit board (PCB). Theoretical analysis, design and simulation, as well as fabrication and experimental validation of this PCB card are presented successively.

Chapter 3 illustrates the whole fabrication process of PI-FFET device and the whole experimental bench set-up in detail.

Chapter 4 reports all my experimental studies with the three different configurations of the PI-FFET, each of them performing various testing to improve progressively CNx adhesion.

Chapter 5 as the last section gives a concise conclusion of my three-year PhD thesis work. I also add recommendations for future work.

REFERENCES:

- [1] R. B. M. Schasfoort, S. Schlautmann, J. Hendrikse, and A. van den Berg, "Field-effect flow control for microfabricated fluidic networks," *Science*, vol. 286, pp. 942-945, 1999.
- [2] A. Plecis, J. Tazid, A. Pallandre, P. Martinhon, C. Deslouis, Y. Chen, and A-M. Haghiri-Gosnet, "Flow field effect transistors with polarizable interface for EOF tunable microfluidic separation devices," *Lab Chip*, vol. 10, pp. 1245-1253, 2010.

Chapter 1: Background Introduction

1.1. Overview

In this chapter, the background around separation using electrophoresis is given as introduction. First of all, capillary electrophoresis is presented, in which the electroosmotic flow (EOF) plays an important role. Second, two major concepts related to the EOF, (i) the surface charge and (ii) the electrical double layer are presented successively. It allows us to define the zeta-potential, an essential factor for electroosmotic phenomenon. By controlling this zeta-potential, analysts can manipulate the EOF in order to better control separation and its resolution. Later, a dynamic mode to control zeta-potential, the first Flow Field Effect Transistor (FFET) designed by a team in Netherlands, is discussed and followed by an introduction of our polarizable interface FFET, which overcomes some disadvantages of the previous one. At the end of this chapter, an H-shaped microfluidic Wheatstone bridge (μ FWB) device is presented in detail.

1.2. Microfluidic Separation

As indicated by its name, microfluidics is a technology that manipulates small amounts of fluids (10^{-9} to 10^{-18} L) in channels with dimensions from tens to hundreds of micrometers [1, 2]. It has been widely used during the last tenth years for various applications: chemical analysis, molecular analysis, biodefence, molecular biology, medical diagnosis, even microelectronics engineering, and *etc.* [2-4]. By integrating microfluidic components onto a single chip, it has contributed to advances of lab-on-a-chip (LOC) devices [5], micro total analysis system (μ TAS) [6], and point-of-care (POC) diagnostic devices [3, 7]. In a word, microfluidics provides a rapid, efficient, inexpensive, and portable way for universal analysis.

Microfluidic handling on-a-chip consists of sample preparation (including purification, preconcentration and labeling), separation, and detection [8]. In the field of separation based on microfluidic system, various techniques have been developed and explored [9, 10]. For example, continuous hydrophoretic techniques [8], such as gel electrophoresis [11, 12] and electrophoresis [13-17]; and utilized external force techniques [18], like acoustophoresis [19-24], dielectrophoresis [25-32], magnetophoresis [33-38], mechanical forces [39-42], and optophoresis [43-45]. In my thesis, I will mainly present the free zone capillary electrophoresis separation and its improvement by a better control of the electroosmotic flow.

1.2.1. Capillary Electrophoresis

Before introducing more specifically free zone electrophoresis on-a-chip, let us briefly understand what is the general principle of electrophoresis from an experimental point of view. Under the application of an electric field, the charged particles move towards the electrode of opposite charge, so it is called electrophoresis. The electrophoretic phenomenon was first discovered by Russian professor F.F. Reuss at Moscow State University in 1807 [46]. Electrophoretic technique uses different moving velocities of charged particles in an electric field to achieve their separation. This method was invented by a Swedish researcher A.W.K. Tiselius in 1936. He designed and manufactured a moving

boundary electrophoresis instrument "Tiselius apparatus" that separated successfully three kinds of globulins from serum albumin of horse [47].

Capillary electrophoresis (CE), also called high performance capillary electrophoresis (HPCE), is a new type of liquid phase electrokinetic separation technology with submillimeter diameter capillaries as separation channels and high voltage DC electric field as driving force. Nowadays, miniaturized CE technology has already attracted lots of attentions. It has been used in various fields in laboratories and industries, owing to its fabulous advantages, such as its portability, low cost, reduction of sample consumption, fast analysis, and low voltage power supply [48]. So, how does the separation in miniaturized CE system happen?



Figure 1.1: Two opposite forces acting on a positive ion as it moves through a microfluidic channel, subjected to an electric field.

Figure 1.1 shows a positive ion placed in microfluidic channel under the influence of an electric field. Two forces act on the ion: the electrophoretic driving force F_{ep} that is given by the product of the ion valence z, elementary charge e, and electric field strength **E**, as shown in Formula 1-1:

$$F_{ep} = zeE \tag{1-1}$$

and the Stokes' drag force F_{drag} that is opposite to the former [49]. According to the Stokes's law, it is described as Formula 1-2:

$$\boldsymbol{F}_{drag} = -6\pi\eta r \boldsymbol{v}_{ep} \tag{1-2}$$

where η is the fluid viscosity, r is the effective radius of the ion, v_{ep} is the electrophoretic migration velocity. It should be noted that in this model the ion is a small spherical particle and it moves at a steady state velocity after a short period in a laminar flow.

For aqueous solutions containing ionic compounds, for example KCl salt in water, ion hydration always occurs. Ion hydration refers to a physical interaction between an ion and a neutral molecule that has a dipole, essentially as an electrostatic attraction: a cation attracts the partially negative end of a neutral polar molecule (K⁺ with oxygen atom of water molecule), while an anion attracts the partially positive end (Cl⁻ with hydrogen atom of water) [50]. There are two combination methods of ion-dipole interaction: either in the form of ion pairs, or one ion surrounded by a tightly bound atomic layer of several water molecules. Due to this, the effective radius of the ions is not the ionic radius but the hydrated radius.

After a few microseconds, the two forces are balanced, *i.e.* $\mathbf{F}_{ep} + \mathbf{F}_{drag} = \mathbf{0}$, thus the ion moves at a constant velocity. Then the electrophoretic migration velocity is obtained as shown in Formula 1-3:

$$v_{ep} = \frac{zeE}{6\pi\eta r} \tag{1-3}$$

Since \mathbf{v}_{ep} can also be expressed by the product of the mobility and electric field strength, then the electrophoretic mobility can be given as Formula 1-4:

$$\mu_{ep} = \frac{ze}{6\pi\eta r} \tag{1-4}$$

From Formula 1-3 and 1-4, it can be seen that both the electrophoretic velocity and mobility are proportional to the ionic charge, and inversely proportional to the hydrated radius, *i.e.* relating to the ionic radius, considering that the fluid viscosity and the electric field strength are fixed. Therefore, when different ionic species migrate through the same solution and are subjected to the same electric field, due to different sizes and charges of particles, they have different mobilities, *i.e.* different velocities, and eventually they separate. Except this electrophoretic velocity, there is another velocity in CE system that should be considered, the electroosmotic flow (EOF) of the buffer solution.

1.2.2. Electroosmotic Flow and Zeta-Potential

Before introducing EOF, let us first familiarize with two concepts: the surface charge and the double layer.





When a solid contacts to a liquid, its surface is not always neutral. Depending on the solid property and pH value of liquid, the surface could be positively or negatively charged. It is called surface ionization. Let us describe for example the case of fused-silica capillary, the material commonly used in CE system. When it is filled with a buffer solution at pH value greater than three, the silanol (Si-OH) groups that attach to the interior wall of capillary are ionized to negatively charged silanoate (Si-O⁻) groups [51]. This kind of surface ionization in capillary can be enhanced by flushing basic solution such as NaOH or KOH through the channel before introducing buffer solution [52].

In the case mentioned-above, the cations of the buffer solution will be attracted to those negatively charged silanoate groups, and then form a compact inner layer on the capillary interior wall, which is also called "Stern layer" or compact layer. Because the density of cations at the inner layer is not large enough to neutralize all the negative charges on the capillary surface, an outer diffuse layer is formed by cations and a few anions [53]. This layer is also called "Gouy-Chapman layer" or mobile layer. Thus, a diffuse double layer, *i.e.* electrical double layer (EDL) is formed, as represented in Figure 1.2.

The first EDL model was proposed by Helmholtz in 1853 [54]. In his model, the EDL was considered as a monolayer with counter ions on the surface and the potential dropped rapidly across the EDL. This model was too simple to explain the electrokinetic phenomenon. Later in the year between 1910 and 1913, Gouy and Chapman improved Helmholtz's model and proposed the Gouy-Chapman model [55, 56]. It was the first time that the diffuse layer was introduced in EDL, and the potential dropped in an exponential way. In 1924, Stern combined the two previous models and then introduced a double-layer in the EDL [53]. The first layer was called "Stern layer", as already mentioned above. In this layer, the change of potential was similar to the one in the Helmholtz model, while the second layer was similar to the diffuse layer in the "Gouy-Chapman" model, in which potential varies in an exponential way. The potential between these two layers was referred to as the zeta-potential.

In an electric field, the cations inside the mobile layer are pulled in the direction of cathode. Due to the ion hydration, also said ion solvation, when solvated cations move, they take along the surrounding water molecules, dragging the bulk buffer solution migrating together with the mobile layer due to the frictional forces [57, 58]. This dragging flow is called the electroosmotic flow. It is believed that EOF occurs due to the interaction between the charged ions on the surface of channel and the buffer solution [59].

The electroosmotic mobility can be defined by the Smoluchowski equation [60], as shown in Formula 1-5:

$$\mu_{eof} = \frac{\varepsilon_0 \varepsilon_r \zeta}{\eta} \tag{1-5}$$

where ε_0 is the permittivity of vacuum, ε_r is the relative permittivity of the buffer solution, ζ is the zetapotential. As the electroosmotic velocity is the product of its mobility and the electric field strength, similar to Formula 1-3, thus, it can be described as Formula 1-6 as follow:

$$v_{eof} = \mu_{eof} E = \frac{\varepsilon_0 \varepsilon_r \zeta E}{\eta}$$
 (1-6)

By combining the electrophoretic migration and the electroosmotic migration, Formula 1-7 shows the effective velocity of an analyte in an electric field:

$$\boldsymbol{v_{eff}} = \boldsymbol{v_{ep}} + \boldsymbol{v_{eof}} = \left(\mu_{ep} + \mu_{eof}\right)\boldsymbol{E} = \left(\frac{ze}{6\pi\eta r} + \frac{\varepsilon_0\varepsilon_r\zeta}{\eta}\right)\boldsymbol{E}$$
(1-7)



Figure 1.3: Velocity profiles for the pumped flow (left) and the electroosmotic flow (right).

The velocity profile of EOF is different to the pressure-driven laminar flow (Poiseuille flow), as shown in Figure 1.3. Compared to the latter, the EOF profile is flat, plug-like, and has narrow band-broadening. That means, it has less variation in its velocity profile when passing through the detection window. This is a great advantage for CE system because all pressure differences during electrophoretic separation should be eliminated at thus limits the band-broadening coming from the laminar parabolic profile [61, 62]. The resolution factor R_s gives a link between EOF and the quality of separation, as described in Formula 1-8 [63, 64]:

$$R_{s} = A \frac{(\mu_{a} - \mu_{b})}{\sqrt{(\mu_{a} + \mu_{b})/2 - \mu_{eof}}}$$
(1-8)

where A is a constant, μ_a and μ_b are electrophoretic mobilities of two analytes injected in the microchannel. This formula quantifies the ability to distinguish two successive peaks of analytes that the electroosmotic mobility μ_{eof} fits to the averaged electrophoretic mobility of the analytes [63, 64].



Figure 1.4: The order of EOF separation of charged and neutral analytes in a fused-silica capillary channel according to their size and electrical charge.

Since electroosmosis often occurs along with electrophoresis, and the EOF of buffer solution is generally five to seven times greater than the electrophoretic flow of analytes, as long as the channel is long enough, all analytes can be separated in the end. Figure 1.4 illustrates the separation. Assuming in fused-silica capillary, cations move towards the cathode and can be separated firstly with the aid of

the EOF, whereas anions move back towards the anode, counter to the EOF, thus separated at last. The multiply charged cations migrate most quickly while the multiply charged anions migrate most slowly. The neutral analytes have no electrophoretic mobility so they move with buffer solution driven by EOF mobility and are separated after cations. Therefore, a separation of sample is achieved. It should be noted that only the electrophoretic force acts to separate analytes.



Figure 1.5: Possible reasons for EOF instability (image derived from [65]).

Modulation of the EOF allows optimizing a high analytical resolution separation that outperforms the traditional free zone CE [63, 64]. However, control of the EOF is not easy, since it depends on several parameters. Figure 1.5 presents those possible reasons that may affect the EOF [65]. It can be seen that the instability of the EOF comes from two main factors: the zeta-potential and the viscosity. The latter depends on the temperature and buffer composition, which is normally stable as long as the power is not too high. While the former, greatly depending on surface charge, is the key role to be manipulated. It should be noted that despite buffer concentration being another important factor for the zeta-potential, however, it can be easily kept constant [65]. Besides, working with low buffer concentration has few influences on the change of the absolute permittivity (product of the permittivity of vacuum and the relative permittivity as shown in Formula 1-5), i.e. the dielectric constant [65]. Therefore, the optimization and enhancement of separation resolution is dominated by the zeta-potential, *i.e.* the charge density of the channel wall. Several methods have been reported to adjust pH value of buffer solution [66-68], and to modify buffer solution [66, 69]. Analysts also used surface treatments such as polymer coating, self-assembled monolayer, etc. [70, 71]. However, all of these methods are non-dynamic and they are optimized for one kind of separation. Thus, scientists started to find a dynamic method to modify the zeta-potential by using an external electric field [72, 73].

1.3. Flow FET and Microfluidic Wheatstone Bridge

In 1999, the team of A. van den Berg first developed a microdevice named "flowFET" [72]. The interest was to control variation of zeta-potential in real time by adding an external gate electrode. They were able to generate electric field strength of 1.5×10^8 V/m by applying a voltage of 50V over the channel. And they also demonstrated a greater control of EOF at lower pH values of 3.5 and 4.5. Later in 2005, the same team improved the Flow FET (FFET) device to stop and even reverse the direction of EOF, and they showed an almost linear relation between the applied gate voltage and zeta-potential [73]. Based on their concept, our team has also proposed and developed a novel FFET microdevice with an electrically polarizable interface in direct contact with the electrolyte [64]. This configuration allowed a control of zeta-potential under several volts, thus at very low gate voltages compared to previous results, probing thus the concept of EOF control by polarizable interface.

1.3.1. From MIE-FFET to PI-FFET



Figure 1.6: The classical MIE-FFET. (A)- The configuration. (B)- The simplified model of EDL. (C)- The three-capacitor model representing the substrate/electrolyte interface. From (A) to (C): images taken from [64]. (D)- The photograph of two MIE-FFETs integrated with a channel junction (left) and the SEM image of this channel junction (right), images taken from [72]. (E)- The photograph of the final device, image taken from [73].

Figure 1.6A shows the configuration of the conventional metal-insulator-electrolyte (MIE)-FFET [64]. It can be seen that this configuration is analogous to that of the solid-state field-effect transistor (FET) in microelectronics, where the perpendicular field generated by the gate electrode manipulates electric current. In this layout, the two electrodes at the both ends of channel play similarly to the source and drain electrodes in FET and the third gate electrode attached to the outside of the channel wall manipulates the EOF [72]. Noted that V_{gate} is the applied gate voltage and V_{ext} is the external transverse voltage, *i.e.* electrophoretic voltage to perform electrophoresis. In this single gate electrode configuration, a non-homogeneous surface charge distribution along the x-axis is observed. The simplified model of EDL of the MIE-FFET is presented in Figure 1.6B [64]. Its corresponding three-capacitor model is represented in Figure 1.6C [64]. Here, V is the gate electrode potential depending on applied gate voltage V_{gate} , Ψ is the surface potential of the insulator surface, ϕ is the electrolyte potential. The potential distribution in the insulator can be represented as a linear drop across it, which means that the field effect is proportional to the insulator thickness and to V_{gate} .

The three capacitances are: C_i capacitance of the insulator; C_s capacitance of the Stern layer; and C_{edl} capacitance of the EDL. The value of C_i can be approximated by Formula 1-9:

$$C_i = \frac{\varepsilon_0 \varepsilon_r A}{d} = \frac{\varepsilon A}{d} \tag{1-9}$$

where ε is the absolute permittivity of material, *i.e.* the dielectric constant, A is the electrode area, and d is the thickness of the insulating layer. It is undoubted that the thicker the layer is, the lower is its capacitance. The Stern capacitance is often neglected because it is only significant in the electrical circuit for solutions with large electrolyte concentrations or for dilute media with large polarization [73]. Besides, it is much larger than C_i and C_{edl} since the Stern layer has only a few Å and the EDL has a few tens of nanometers, while insulator is much thicker (C_s > C_{edl} > C_i) [64, 72]. The value of C_{edl} can be simplified and described by Formula 1-10 [73, 74]:

$$C_{edl} = 228z\sqrt{c}\cosh(19.5z\zeta) \tag{1-10}$$

where z is the ion valence, c is the electrolyte concentration. This formula is only valid for dilute aqueous solutions at 25°C.

Therefore, the variation of zeta-potential can be induced by the gate voltage V_{gate} as given in Formula 1-11 [73]:

$$\Delta \zeta = \frac{C_i}{C_{edl}} \left(V_{gate} - \varphi \right) \tag{1-11}$$

From the Formula 1-11, it is clear that the zeta-potential variation is proportional to the insulator capacitance and the gate voltage, and inversely proportional to the EDL capacitance. Taking account of C_i, its increase corresponds to a high dielectric constant for a very thin insulator. Meanwhile, to keep the gate voltage low, an extremely thin wall (<1 μ m) is also required [72]. Thus, the insulating material should have a high value of electrical breakdown strength. However, considering about C_{edl} that also depends on zeta-potential, the relation between $\Delta \zeta$ and V_{gate} is more complicated.

Figure 1.6D and E exhibit the photographs of the first MIE-FFET device (Figure 1.6D) and the second improved device (Figure 1.6E) respectively. These devices have demonstrated ability to control the

zeta-potential by tuning the external perpendicular gate field, resulting in a fast and dynamic manipulation.



Figure 1.7: The PI-FFET developed by our team. (A)- The configuration. (B)- The simplified layout of EDL. (C)- The two-capacitor model representing the substrate/electrolyte interface. (D)- The photograph of the final device. Images taken from [64].

Figure 1.7 shows the polarizable interface based FFET designed by our team and called PI-FFET [64]. Its configuration is illustrated in Figure 1.7A. As it can be seen, there is no insulator; the commanded layer is directly immerged into the electrolyte. The control of zeta-potential is achieved by applying a potential difference between these two layers. This potential difference between the electrolyte potential ϕ and the control gate electrode V is called over-potential γ (= V- ϕ), and the variation of γ ($\Delta\gamma$) allows the variation of zeta-potential ($\Delta\zeta$). To get such $\Delta\zeta$, the commanded layer should be polarizable, called "polarizable interface".

Figure 1.7B and C represent the simplified layout of the PI-FFET configuration and its two-capacitor model respectively [64]. Since there are no insulating layer, the surface potential is equal to the gate electrode potential ($\Psi = V$). Meanwhile, there is no more insulator capacitance C_i. Thus, the variation of induced zeta-potential can be given as Formula 1-12 [64]:

$$\Delta \zeta (\gamma) = \frac{c_s}{c_s + c_{edl}} (\gamma) \tag{1-12}$$

Due to the Stern capacitance that is larger than EDL capacitance, the Formula 1-12 can be simplified and approximated by Formula 1-13 [64]:

$$\Delta \zeta (\gamma) \approx \gamma \tag{1-13}$$

Since the over-potential is controlled by applying a voltage difference with the nearest external electrode called ΔV_{gate} , the Formula 1-13 can be modified by Formula 1-14 [64]:

$$\Delta \zeta (x) \approx \Delta V_{gate} \tag{1-14}$$

which means, as long as the gate voltage remains within the admissible potential window, the zetapotential, *i.e.* the manipulation of EOF only depends on the experimental gate voltage, the external longitudinal electric field is independent to this control and does not influence it, so as to the other factors.

Based on this concept, our team has designed, fabricated and experimented the PI-FFET device, as shown in Figure 1.7D. Compared to the MIE-FFET, PI-FFET overcame the difficulties met with the former: as dual gate electrodes integrated at both ends of channel wall, the surface charge along the channel is more homogeneous; as no insulator existing in PI-FFET, there is no risk of breaking the insulator (insulating layer becomes porous and current leakages occur with the MIE-FFET configuration); as the ratio of the insulator capacitance to the EDL capacitance is very small (cause of layer thickness), MIE-FFET requires large gate voltage according to Formula 1-11. With this PI-FFET device, our team has successfully tuned zeta-potential in a large potential window with very low gate voltages from -2V to +2V [64].





Figure 1.8: The analogy of microflows to electrical currents. (A)- Pressure-driven Poiseuille flow and its analogy to electrical current. (B)- Electroosmosis-driven plug-like flow and its analogy to electrical current. (C)- The analogy of the mixture flows. Image taken from [63].

The measurement of EOF in such a PI-FFET device is performed by using a H-shaped fluidic network, called "microfluidic Wheatstone bridge (μ FWB)", a configuration designed by our team more than a decade ago [75]. The conception was inspired based on an analogy of microflows to electrical currents as shown in Figure 1.8 [63].

There are two typical flow profiles existing in rectangular microchannels: the Poiseuille flow and the electroosmotic flow. The former is a pressure-driven flow with a parabolic velocity profile, which can be seen in Figure 1.3. This kind of flow is valid at low Reynold's number (laminar flows). It can thus be considered as incompressible Newtonian fluid and the average flow rate J can therefore be expressed by Navier-Stokes equations [76]. The analogy of Poiseuille flow to electrical current can be illustrated as shown in Figure 1.8A [63]. The pressure P_1 generated by pumps or syringe can be considered as a voltage source, the mass P_0 can be equivalent to the atmospheric pressure, the flow rate J corresponds to the generated current. In this case, there is no electric field thus no electrical current injected across the channel. The second flow is the electroosmosis-driven flow with a plug-like velocity profile (see Figure 1.3). The analogy of electroosmotic flow to electrical current is displayed in Figure 1.8B [63]. There is no driven pressure, the electroosmotic flow can thus be modeled by a current source, producing a flow rate J (the EOF J_{eof}) that only depends on zeta-potential ζ and injected electrical current I, as described by Formula 1-15 [75]:

$$J_{eof} = \sigma \, \frac{\varepsilon_0 \varepsilon_r \zeta}{\eta} \, I \tag{1-15}$$

where σ , $\varepsilon_0\varepsilon_r$ and η is the conductivity, permittivity and viscosity of the solution respectively that normally do not change. Figure 1.8C shows the superimposition of Poiseuille flow and EOF, in which the total flow rate is the sum of two, resulting in a zero-net flow. As the outlet is plugged (like open switch in electrical system), a counter flow J_p is generated. Due to the mass conservation, J_p = -J_{eof} [63].



Figure 1.9: The analogy of μFWB to electrical Wheatstone bridge. (A)- The general analogy. (B)- The analogy in EOF mode, under electric field, leading to the fluidic resistance calibration. (C)- The analogy in Poiseuille mode without electric field, leading to the Poiseuille calibration. Image taken from [63].

Based on the above analogy, our H-shaped μ FWB system was designed as shown in Figure 1.9 [63]. The left figure in part A shows the configuration of the H-shaped μ FWB device, Figure 1.9A illustrates the analogy between the μ FWB and the electrical Wheatstone bridge.

Before measurements of EOF, two calibrations should be done. These calibrations are shown in Figure 1.9B and C respectively [63]. When an electric field is applied in the central channel (part B), the generated EOF causes four Poiseuille flows in four arms (side channels), proportional to the EOF flow rate J_{eof} , following Formula 1-16 [75]:

$$J_{eof} = \alpha_i J_i \ (i = 1, 2, 3, 4) \tag{1-16}$$

where J_i is the side flow rate of each arm, α_i is the corresponding proportionality factor and it can be described as Formula 1-17 [75]:

$$\alpha_i = f(g_1, g_2, g_3, g_4) \tag{1-17}$$

where g_i (i = 1,2,3,4) is the relative fluidic conductance values that can be calculated as Formula 1-18 [75]:

$$g_i = \frac{R_p}{R_i} \ (i = 1, 2, 3, 4) \tag{1-18}$$

i.e. the ratio of the fluidic resistance of the central channel R_p to that of each arm R_i.

The first calibration corresponds to the fluidic resistance calibration as shown in Figure 1.9B. According to the Formula 1-16, we have three equations of the form of $J_{eof} = \alpha_i (g_1, g_2, g_3, g_4) J_i$ with five unknown parameters (J_{eof} , g_1 , g_2 , g_3 , g_4). It should be noted that J_i of each side channel could be measured. Also, according to the flow conservation, one flow rate of the side channel can be expressed by another three, for example $J_4 = J_1 + J_3 - J_2$. However, this is not enough for us to calculate EOF. Thus, we need a second calibration, *i.e.* the Poiseuille calibration, described in Figure 1.9C [63].

During this second calibration, no electric field is applied in the central channel. Instead, a pressure gradient is applied in the device, in which the flow rate of each arm depends on the fluidic resistance, just like in an electrical circuit where current depends on the resistance. Similarly to the first calibration, we obtain three equations of $I_p = f(g_1, g_2, g_3, g_4, I_i)$, where I_p is the flow rate crossing central channel and I_i is the measured flow rate of each side channel. Thus, the only unknown is I_p . In total, for the six equations with six unknowns, we can solve all the parameters: J_{eof} , I_p , g_1 , g_2 , g_3 , g_4 , $expressed by J_1$, J_2 , J_3 , J_4 and I_1 , I_2 , I_3 , I_4 . The proportionality factor α_1 , α_2 , α_3 , α_4 can also be expressed by J_i and I_i . It is important that the four fluidic resistances should be different to make sure that flow can pass through the central channel, otherwise this H-shaped μ FWB is worthless. That is why two of the side arms are designed to have restriction channel (see Figure 3.3B).

After these two calibrations, EOF flow rate J_{eof} in the central channel can be simply deduced by only measuring flow rate J_i in one of four arms. This H-shaped μ FWB device is an indirect method to measure EOF. It has several advantages: first, the calibrations can check out the presence of any fluid leakage or channel clogging; second, this indirect flow rate measurement in lateral arms can avoid any influence of unknown electrophoretic velocity because there is no electric field there; third, this is a highly effective method, the calibration could be performed 8 times within 10mn, and the EOF measurement could be achieved every 30s with a great accuracy [75].

1.3.3. Polarizable Interface and Polarizability Window



Figure 1.10: Schemes of two behaviors of the interface ideally non-polarizable (left) and polarizable (right), image taken from [77].

When two electrodes are placed in a liquid electrolyte and applied by a potential difference, two behaviors exist: either the charge transfer takes place immediately at the solid-liquid interface and the electrons can be transferred from one electrode to the other by the ionic carriers of liquid; or the charge transfer does not take place at the interface but instead by the accumulation of charges at the solid-liquid interface. The former is called ideally non-polarizable interface (see left image of Figure 1.10 [77]), resulting in immediately electrochemical reaction and faradic current, while the latter is called ideally polarizable interface (see right image of Figure 1.10 [77]), resulting in purely capacitive behavior and no charges transfer, in other word, no faradic current.



Figure 1.11: The faradic current curve under function of over-potential for a symmetric interface.

The window of polarizability is a limited range of over-potential γ where the faradic current cannot be observed with a weak linear dependence [77]. In a case of symmetric interface, this faradic current can be described as Formula 1-19 [77]:

$$I_F = I^0 \sinh(\frac{\gamma}{\gamma^0}) \tag{1-19}$$

where I^0 is the typical surface current, γ^0 is the energy barrier potential. The polarizability window is the area that γ varies within γ^0 , as shown in Figure 1.11. However, in reality, this window is rarely symmetric due to the electrochemical reactions, such as the reduction and the oxidation. Moreover, changes in liquid electrolyte will also influence on the polarizability window, like adding another electrolyte or diluting the electrolyte.

1.4. Conclusions

This chapter gives an overview of the thesis background, from the basic of the CE to the birth of the μ FWB that has improved CE technology. During the last ten years, the μ FWB configuration has been developed and improved to better adapt to hydrodynamics and electrodes implantation. In my thesis work, I used the 3rd generation of this device that will be explained and detailed in Chapter 3. And I mainly concentrated my work about the adhesion ability of the polarizable interface (a CNx film that was few studied in the world) on two major sticking underlayers (SiC and Pt) for three different PI-FFET configurations, as well as some microfluidic experiments to study PI-FFET.

REFERENCES:

- Q. Zhang, M. Zhang, L. Djeghlaf, J. Bataille, J. Gamby, A-M. Haghiri-Gosnet, and A. Pallandre, "Logic digital fluidic in miniaturized functional devices: Perspective to the next generation of microfluidic lab-on-chips," *Electrophoresis*, vol. 38, pp. 953-976, 2017.
- [2] G. M. Whitesides, "The origins and the future of microfluidics," *Nature*, vol. 442, pp. 368-373, 2006.
- [3] N-T. Nguyen, M. Hejazian, C. H. Ooi, and N. Kashaninejad, "Recent advances and future perspectives on microfluidic liquid handling," *Micromachines*, vol. 8, pp. 186-206, 2017.
- [4] N-T. Nguyen and S. T. Wereley, "Fundamentals and applications of microfluidics," Artech House, London, UK, 2002.
- [5] N-T. Nguyen, S. A. M. Shaegh, N. Kashaninejad, and D-T. Phan, "Design, fabrication and characterization of drug delivery systems based on lab-on-a-chip technology," *Adv. Drug Deliv. Rev.*, vol. 65, pp. 1403-1419, 2013.
- [6] D. R. Reyes, D. Iossifidis, P-A. Auroux, and A. Manz, "Micro total analysis systems. 1. Introduction, theory, and technology," *Anal. Chem.*, vol. 74, pp. 2623-2636, 2002.
- [7] W. Jung, J. Han, J-W. Choi, and C. H. Ahn, "Point-of-care testing (POCT) diagnostic systems using microfluidic lab-on-a-chip technologies," *Microelectron. Eng.*, vol. 132, pp. 46-57, 2015.
- [8] M. Sonker, V. Sahore, and A. T. Woolley, "Recent advances in microfluidic sample preparation and separation techniques for molecular biomarker analysis: A critical review," *Anal. Chim. Acta*, vol. 986, pp. 1-11, 2017.

- [9] K. K. R. Tetala and M. A. Vijayalakshmi, "A review on recent developments for biomolecule separation at analytical scale using microfluidics devices," *Anal. Chim. Acta*, vol. 906, pp. 7-21, 2016.
- [10] J. V. Pagaduan, V. Sahore, and A. T. Woolley, "Applications of microfluidics and microchip electrophoresis for potential clinical biomarker analysis," *Anal. Bioanal. Chem.*, vol. 407, pp. 6911-6922, 2015.
- [11] S. M. Shameli and C. L. Ren, "Microfluidic two-dimensional separation of proteins combining temperature gradient focusing and sodium dodecyl sulfate-polyacrylamide gel electrophoresis," *Anal. Chem.*, vol. 87, pp. 3593-3597, 2015.
- [12] R. Wu, Y. P. Seah, and Z. Wang, "Microfluidic chip for stacking, separation and extraction of multiple DNA fragments," J. Chromatogr. A, vol. 1437, pp. 219-225, 2016.
- [13] E. A. Redman, N. G. Batz, J. S. Mellors, and J. M. Ramsey, "Integrated microfluidic capillary electrophoresis-electrospray ionization devices with online MS detection for the separation and characterization of intact monoclonal antibody variants," *Anal. Chem.*, vol. 87, pp. 2264-2272, 2015.
- [14] P. Batalla, A. Martin, M. A. Lopez, M. C. Gonzalez, and A. Escarpa, "Enzyme-based microfluidic chip coupled to graphene electrodes for the detection of d-amino acid enantiomerbiomarkers," Anal. Chem., vol. 87, pp. 5074-5078, 2015.
- [15] J. V. Pagaduan, M. Ramsden, K. O'Neill, and A. T. Woolley, "Microchip immunoaffinity electrophoresis of antibody-thymidine kinase 1 complex," *Electrophoresis*, vol. 36, pp. 813-817, 2015.
- [16] V. Sahore, S. Kumar, C. I. Rogers, J. K. Jensen, M. Sonker, and A. T. Woolley, "Pressure-actuated microfluidic devices for electrophoretic separation of pre-term birth biomarkers," *Anal. Bioanal. Chem.*, vol. 408, pp. 599-607, 2016.
- [17] F. Lin, S. Yu, L. Gu, X. Zhu, J. Wang, H. Zhu, Y. Lu, Y. Wang, Y. Deng, and L. Geng, "In situ photoimmobilized pH gradient isoelectric focusing and zone electrophoresis integrated twodimensional microfluidic chip electrophoresis for protein separation," *Microchim. Acta*, vol. 182, pp. 2321-2328, 2015.
- [18] A. J. Laki, "Microfluidic particle separation techniques for biomedical use," PhD thesis, Pazmany Peter Catholic University, 2015.
- [19] J. Shi, S. Yazdi, S-C. S. Lin, X. Ding, I-K. Chiang, K. Sharp, and T. J. Huang, "Three-dimensional continuous particle focusing in a microfluidic channel via standing surface acoustic waves (SSAW)," *Lab Chip*, vol. 11, pp. 2319-2324, 2011.
- [20] J. Shi, H. Huang, Z. Stratton, Y. Huang, and T. J. Huang, "Continuous particle separation in a microfluidic channel via standing surface acoustic waves (SSAW)," *Lab Chip*, vol. 9, pp. 3354-3359, 2009.

- [21] J. Nam, H. Lim, D. Kim, and S. Shin, "Separation of platelets from whole blood using standing surface acoustic waves in a microchannel," *Lab Chip*, vol. 11, pp. 3361-3364, 2011.
- [22] T. Laurell, F. Petersson, and A. Nilsson, "Chip integrated strategies for acoustic separation and manipulation of cells and particles," *Chem. Soc. Rev.*, vol. 36, pp. 492-506, 2007.
- [23] J. Shi, X. Mao, D. Ahmed, A. Colletti, and T. J. Huang, "Focusing microparticles in a microfluidic channel with standing surface acoustic waves (SSAW)," *Lab Chip*, vol. 8, pp. 221-223, 2008.
- [24] T. Franke, S. Braunmuller, L. Schmid, A. Wixforth, and D. A. Weitz, "Surface acoustic wave actuated cell sorting (SAWACS)," *Lab Chip*, vol. 10, pp. 789-794, 2010.
- [25] Y. Li, C. Dalton, H. J. Crabtree, G. Nilsson, and K. V. I. S. Kaler, "Continuous dielectrophoretic cell separation microfluidic device," *Lab Chip*, vol. 7, pp. 239-248, 2007.
- [26] A. Valero, T. Braschler, A. Rauch, N. Demierre, Y. Barral, and P. Renaud, "Tracking and synchronization of the yeast cell cycle using dielectrophoretic opacity," *Lab Chip*, vol. 11, pp. 1754-1760, 2011.
- [27] M. J. Hilhorst, G. W. Somsen, and G. J. de Jong, "Capillary electrokinetic separation techniques for profiling of drugs and related products," *Electrophoresis*, vol. 22, pp. 2542-2564, 2001.
- [28] H-H. Cui, J. Voldman, X-F. He, and K-M. Lim, "Separation of particles by pulsed dielectrophoresis," *Lab Chip*, vol. 9, pp. 2306-2312, 2009.
- [29] S-I. Han, S-M. Lee, Y-D. Joo, and K-H. Han, "Lateral dielectrophoretic microseparators to measure the size distribution of blood cells," *Lab Chip*, vol. 11, pp. 3864-3872, 2011.
- [30] M. D. Vahey and J. Voldman, "Emergent behavior in particle-laden microfluidic systems informs strategies for improving cell and particle separations," *Lab Chip*, vol. 11, pp. 2071-2080, 2011.
- [31] L. Wang, L. A. Flanagan, N. L. Jeon, E. Monuki, and A. P. Lee, "Dielectrophoresis switching with vertical sidewall electrodes for microfluidic flow cytometry," *Lab Chip*, vol. 7, pp. 1114-1120, 2007.
- [32] H-S. Moon, K. Kwon, S-I. Kim, H. Han, J. Sohn, S. Lee, and H-I. Jung, "Continuous separation of breast cancer cells from blood samples using multi-orifice flow fractionation (MOFF) and dielectrophoresis (DEP)," Lab Chip, vol. 11, pp. 1118-1125, 2011.
- [33] H. Lee, J. Jung, S-I. Han, and K-H. Han, "High-speed RNA microextraction technology using magnetic oligo-dT beads and lateral magnetophoresis," *Lab Chip*, vol. 10, pp. 2764-2770, 2010.
- [34] F. Shen, H. Hwang, Y. K. Hahn, and J-K. Park, "Label-free cell separation using a tunable magnetophoretic repulsion force," *Anal. Chem.*, vol. 84, pp. 3075-3081, 2012.
- [35] T. Zhu, R. Cheng, S. A. Lee, E. Rajaraman, M. A. Eiteman, T. D. Querec, E. R. Unger, and L. Mao,
 "Continuous-flow ferrohydrodynamic sorting of particles and cells in microfluidic devices," *Microfluid Nanofluidics*, vol. 13, pp. 645-654, 2012.

- [36] A. I. Rodriguez-Villarreal, M. D. Tarn, L. A. Madden, J. B. Lutz, J. Greenman, J. Samitier, and N.
 Pamme, "Flow focusing of particles and cells based on their intrinsic properties using a simple diamagnetic repulsion setup," *Lab Chip*, vol. 11, pp. 1240-1248, 2011.
- [37] D. Robert, N. Pamme, H. Conjeaud, F. Gazeau, A. Iles, and C. Wilhelm, "Cell sorting by endocytotic capacity in a microfluidic magnetophoresis device," *Lab Chip*, vol. 11, pp. 1902-1910, 2011.
- [38] N. Pamme and C. Wilhelm, "Continuous sorting of magnetic cells via on-chip free-flow magnetophoresis," *Lab Chip*, vol. 6, pp. 974-980, 2006.
- [39] P. Bhardwaj, P. Bagdi, and A. K. Sen, "Microfluidic device based on a microhydrocyclone for particle-liquid separation," *Lab Chip*, vol. 11, pp. 4012-4021, 2011.
- [40] D. Huh, J. H. Bahng, Y. Ling, H-H. Wei, O. D. Kripfgans, J. B. Fowlkes, J. B. Grotberg, and S. Takayama, "Gravity-driven microfluidic particle sorting device with hydrodynamic separation amplification," *Anal. Chem.*, vol. 79, pp. 1369-1376, 2007.
- [41] R. Gorkin, J. Park, J. Siegrist, M. Amasia, B. S. Lee, J-M. Park, J. Kim, H. Kim, M. Madou, and Y-K. Cho, "Centrifugal microfluidics for biomedical applications," *Lab Chip*, vol. 10, pp. 1758-1773, 2010.
- [42] S. Haeberle, T. Brenner, R. Zengerle, and J. Ducree, "Centrifugal extraction of plasma from whole blood on a rotating disk," *Lab Chip*, vol. 6, pp. 776-781, 2006.
- [43] H. Zhang, E. Tu, N. D. Hagen, C. A. Schnabel, M. J. Paliotti, W. S. Hoo, P. M. Nguyen, J. R. Kohrumel, W. F. Butler, M. Chachisvillis, and P. J. Marchand, "Time-of-flight optophoresis analysis of live whole cells in microfluidic channels," *Biomed. Microdevices*, vol. 6, pp. 11-21, 2004.
- [44] B. S. Zhao, Y-M. Koo, and D. S. Chung, "Separations based on the mechanical forces of light," *Anal. Chim. Acta*, vol. 556, pp. 97-103, 2006.
- [45] T-H. Wu, Y. Chen, S-Y. Park, J. Hong, T. Teslaa, J. F. Zhong, D. D. Carlo, M. A. Teitell, and P-Y. Chiou, "Pulsed laser triggered high speed microfluidic fluorescence activated cell sorter," *Lab Chip*, vol. 12, pp. 1378-1383, 2012.
- [46] F. F. Reuss, "Sur un nouvel effet de l'électricité galvanique," Mémoires de la Société Impériale des Naturalistes de Moscou, vol. 2, pp. 327-337, 1809.
- [47] A. Tiselius, "A new apparatus for electrophoretic analysis of colloidal mixtures," *Trans. Faraday Soc.*, vol. 33, pp. 524-531, 1937.
- [48] D. Janasek, J. Franzke, and A. Manz, "Scaling and the design of miniaturized chemical-analysis systems," *Nature*, vol. 442, pp. 374-380, 2006.
- [49] H. Bruus, "Theoretical microfluidics," Oxford University Press, Oxford, UK, 2008.
- [50] "Ion-Dipole Forces," <u>https://www.chem.purdue.edu/gchelp/liquids/iondip.html</u>.

- [51] M. X. Zhou and J. P. Foley, "Quantitative theory of electroosmotic flow in fused-silica capillaries using an extended site-dissociation-site-binding model," *Anal. Chem.*, vol. 78, pp. 1849-1858, 2006.
- [52] D. R. Baker, "Capillary electrophoresis," Wiley-Interscience, New York, USA, 1995.
- [53] O. Z. Stern, "Theory of the electrical double layer," *Electrochem*, vol. 30, pp. 508-516, 1924.
- [54] H. L. F. von Helmholtz, "Ueber einige Gesetze der Vertheilung elektrischer Ströme in körperlichen Leitern mit Anwendung auf die thierisch-elektrischen Versuche," Annalen der Physik, vol. 165, pp. 211-233, 1853.
- [55] L. G. Gouy, "Sur la constitution de la charge électrique à la surface d'un électrolyte," *J. Phys. Theor. Appl.*, vol. 9, pp. 457-468, 1910.
- [56] D. L. Chapman, "A contribution to the theory of electrocapillarity," *Philos. Mag.*, vol. 25, pp. 475-481, 1913.
- [57] M. Smoluchowski, "Elektrische endosmose und strömungsströme," Handbuch der Elektrizität und des Magnetismus, vol. 2, pp. 366-428, B. GRAETZ, Leipzig, 1914.
- [58] C. Gerthsen, H. O. Kneser, and H. Vogel, "Physik," 16th Edition, Springer Berlin, Germany, 1989.
- [59] A. Manz, C. S. S. Effenhauser, N. Burggraf, D. J. Harrison, K. Seiler, and K. Fluri, "Electroosmotic pumping and electrophoretic separations for miniaturized chemical analysis systems," J. *Micromech. Microeng.*, vol. 4, pp. 257-265, 1994.
- [60] A. Sze, D. Erickson, L. Ren, and D. Li, "Zeta-potential measurement using the Smoluchowski equation and the slope of the current-time relationship in electroosmotic flow," J. Colloid Interface Sci., vol. 261, pp. 402-410, 2003.
- [61] E. K. Zholkovskij, A. E. Yaroshchuk, J. H. Masliyah, and J. D. Ribas, "Broadening of neutral solute band in electroosmotic flow through submicron channel with longitudinal non-uniformity of zeta potential," *Colloids Surf. A*, vol. 354, pp. 338-346, 2010.
- [62] E. K. Zholkovskij and J. H. Masliyah, "Influence of cross-section geometry on band broadening in plug-flow microchannels," *Chem. Eng. Sci.*, vol. 61, pp. 4155-4164, 2006.
- [63] A. Pallandre, "Intégration du transistor fluidique à effet de champs et à interface polarisable dans un pont de Wheatstone," HDR, Université Paris-Sud, 2015.
- [64] A. Plecis, J. Tazid, A. Pallandre, P. Martinhon, C. Deslouis, Y. Chen, and A-M. Haghiri-Gosnet, "Flow field effect transistors with polarizable interface for EOF tunable microfluidic separation devices," *Lab Chip*, vol. 10, pp. 1245-1253, 2010.
- [65] L. Baur, C. S. van de Griend, and H. Wätzig, "Electroosmotic flow variations caused by the volatility of buffer components: diagnosis and therapy," J. Chromatogr. A, vol. 979, pp. 97-103, 2002.
- [66] W. Schüetzner and E. Kenndler, "Electrophoresis in synthetic organic polymer capillaries: variation of electroosmotic velocity and zeta potential with pH and solvent composition," *Anal. Chem.*, vol. 64, pp. 1991-1995, 1992.
- [67] M. A. Hayes, I. Kheterpal, and A. G. Ewing, "Effects of buffer pH on electroosmotic flow control by an applied radial voltage for capillary zone electrophoresis," *Anal. Chem.*, vol. 65, pp. 27-31, 1993.
- [68] B. J. Kirby and E. F. Hasselbrink Jr., "Zeta potential of microfluidic substrates: 1. Theory, experimental techniques, and effects on separations," *Electrophoresis*, vol. 25, pp. 187-202, 2004.
- [69] A. Varenne and S. Descroix, "Recent strategies to improve resolution in capillary electrophoresis: A review," *Anal. Chim. Acta*, vol. 628, pp. 9-23, 2008.
- [70] E. A. S. Doherty, R. J. Meagher, M. N. Albarghouthi, and A. E. Barron, "Microchannel wall coatings for protein separations by capillary and chip electrophoresis," *Electrophoresis*, vol. 24, pp. 34-54, 2003.
- [71] A. Pallandre, B. de Lambert, R. Attia, A. M. Jonas, and J-L. Viovy, "Surface treatment and characterization : perspectives to electrophoresis and lab-on-chips," *Electrophoresis*, vol. 27, pp. 584-610, 2006.
- [72] R. B. M. Schasfoort, S. Schlautmann, J. Hendrikse, and A. van den Berg, "Field-effect flow control for microfabricated fluidic networks," *Science*, vol. 286, pp. 942-945, 1999.
- [73] E. J. van der Wouden, T. Heuser, D. C. Hermes, R. E. Oosterbroek, J. G. E. Gardeniers, and A. van den Berg, "Field-effect control of electro-osmotic flow in microfluidic networks," *Colloids Surf. A*, vol. 267, pp. 110-116, 2005.
- [74] A. J. Bard and L. R. Faulkner, "Electrochemical methods," John Wiley & Sons, New York, USA, 1980.
- [75] A. Plecis and Y. Chen, "Microfluidic analogy of the Wheatstone bridge for systematic investigations of electro-osmotic flows," *Anal. Chem.*, vol. 80, pp. 3736-3742, 2008.
- [76] G. Desmet and G. V. Baron, "Chromatographic explanation for the side-wall induced band broadening in pressure-driven and shear-driven flows through channels with a high aspect-ratio rectangular cross-section," *J. Chromatogr. A*, vol. 946, pp. 51-58, 2002.
- [77] A. Plecis, "Etude et contrôle de la charge de surface dans les dispositifs micro/nanofluidiques : nouveaux outils pour les sciences séparatives," PhD thesis, Université Paris-Sud, 2008.

Chapter 2: Simplification of EOF Measurement Equipment

2.1. Overview

In the early Section 1.3.1, we have presented the polarizable interface flow field effect transistor (PI-FFET) designed by our team (Figure 1.7A). An ideal polarizable interface fluidic transistor should have no electrochemical reactions, such as electronic transfer or faradic current from solid to the electrolyte, which is normally caused by reduction or oxidation of chemical substance at the electrode [1, 2]. As we have already known that the over-potential γ is a potential difference between the electrolyte potential ϕ and the control gate voltage V (see details in Section 1.3.1). As long as it remains within a potential window $|\gamma| < \gamma_0$, the faradic current could be negligible [3]. The factor γ_0 is called the faradic over-potential, depending on the conduction layer-electrolyte couple [4]. Therefore, to avoid such electrochemical reactions, we have integrated two electrolyte measuring electrodes, *i.e.* reference electrolyte potential ϕ at both ends of the fluidic transistor in order to accurately apply the control gate voltage V on the two PI-FFET control electrodes, *i.e.* gate electrodes, thus making sure that $|V-\phi|$ = $|\gamma| < \gamma_0$, as illustrated in Figure 2.1 [5].



Figure 2.1: The simplified electronic configuration of the PI-FFET, image taken from [5].

The outermost pair of electrodes provides the transverse electrophoretic field. Two voltage followers circled in yellow were two big equipments in the past, as shown in Figure 3.8 of Section 3.3.1. In this chapter, we will present a small portable printed circuit board (PCB) that replaces these two big heavy boxes.

2.2. Theoretical Analysis



Figure 2.2: The electronic conception of the voltage follower (above) and its electronic model (below).

The conception of the voltage follower is shown in the image above of Figure 2.2. The electrophoretic field is applied by a +15V/ground source meter unit or power supply unit with low current. V1 and V4 represent the voltage of the electrolyte that the two followers read about, while V2 and V3 represent the voltage employed on the gate electrodes according to V1 and V4 respectively. The difference between V1 and V2 or V4 and V3 should remain within the potential window, which is from -3.5V to +3.5V of this device [6]. To be on the safe side, ΔV is chosen within -1V/+1V. Such voltage follower is very simple in electronic model, as shown in image below of Figure 2.2: four voltage followers without gain, two adders, and one regulator. In the following part, we will introduce design of each part.

2.2.1. Adder



Figure 2.3: The electronic circuit schema of the adder.

The adder is designed based on negative feedback non-inverting amplifier, one kind of the operational amplifiers (opamp). An ideal negative feedback opamp has following properties: the input impedance is infinite so that the current between the inverting input and the non-inverting input is approximately to zero [7]; the output impedance approaches to zero so that the output voltage is nearly constant; the value of inverting input equals to that of non-inverting input. According to these properties, the electronic circuit schema of adder can be designed as shown in Figure 2.3.

According to Millman's theorem [8], we have Equation 2-1 and 2-2:

$$V + = \frac{\frac{\Delta V}{R_1} + \frac{V_{in}}{R_2}}{\frac{1}{R_1} + \frac{1}{R_2}}$$
(2-1)

$$V_{-} = \frac{\frac{0}{R_{3}} + \frac{V_{out}}{R_{4}}}{\frac{1}{R_{3}} + \frac{1}{R_{4}}}$$
(2-2)

Also V+ = V-, then we have Equation 2-1 equaling to Equation 2-2, after simplifying, we obtain Equation 2-3:

$$\frac{\Delta V \times R2 + V_{in} \times R1}{R2 + R1} = \frac{V_{out} \times R3}{R4 + R3}$$
(2-3)

As we want $V_{in} + \Delta V = V_{out}$, to achieve this, R1 = R2 = R3 = R4.

2.2.2. Voltage Follower



Figure 2.4: The electronic circuit schema of the voltage follower.

The voltage follower is also based on negative feedback non-inverting opamp, its electronic schema is presented in Figure 2.4. In this case, we have $V_{+} = V_{in}$, $V_{-} = V_{out}$, as $V_{+} = V_{-}$, then we get $V_{out} = V_{in}$, with gain = 1. It indeed follows the input voltage. The reason of using no-gain follower before the adder is to reduce the influence of fluctuant potential of electrolyte, providing a more constant input to the adder. Similarly, adding follower after the adder makes sure that any unstable fluctuant output will not affect the voltage applied on the gate electrode.

2.2.3. Regulator



Figure 2.5: The electronic circuit schema of the regulator.

The regulator is inspired by voltage divider, *i.e.* potential divider. As the name implies, it distributes the input voltage among components [9]. The electronic schema of regulator is illustrated as Figure 2.5. The voltage sources are fixed to +15V/-15V not only for the regulator but also for all the opamps, agreeing with the voltage of the electrophoretic field. As we want the output voltage ΔV range from - 1V to +1V, the distribution of resistances should be like Equation 2-4:

$$\frac{R2}{R1+R2} = \frac{1}{15} \tag{2-4}$$

thus, we have R1 = 14R2. The output is a potentiometer, by regulating its resistance distribution, we will obtain different output voltages.

2.3. Simulation, Fabrication and Experimental Validation

Based on the mentioned-above structures, the whole electronic schema was finished and simulated on NI Multisim[™], then the real device was packaged on Altium Designer[®] and fabricated in a company in Shenzhen, China. Table 1 gives a list of all the components.

Table 1: List of components of the PCB card.

Components	Manufacturers	Manufacturer References	Prices (€)/piece
Opamp AD711KN	Analog Devices	AD711KNZ	6.53
Opamp AD712JN	Analog Devices	AD712JNZ	4.8
Potentiometer 10kΩ	Bourns	3682S-1-103L	31.68
Resistance CMS 10kΩ	TE Connectivity	CRG1206F10K	0.004
Resistance CMS 715Ω	Panasonic	ERA3AEB7150V	0.068
Capacitor ceramic 100nF	KEMET	C0603C104K3RACTU	0.013
Capacitor tantalum 1µF	AVX	TAJB105K035RNJ	0.301

2.3.1. Simulation



Figure 2.6: The complete simulation circuit of the PCB card.

The schema of the complete simulation circuit is shown in Figure 2.6, where the power supply of the device, the regulator, the voltage followers, and the adders are represented in black, green, purple and red circles respectively. The input voltages V1 and V4 are drawn in green lines, the output voltage ΔV of regulator is in blue line, and the output voltages of adder V2 and V3 are drawn in yellow lines.





Figure 2.7: The results of simulation on one of the oscilloscopes, where $V1 + \Delta V = V2$. From top to bottom: $\Delta V = +1V$, 0V, -1V. Blue line: ΔV . Red line: V1. Green line: V2.

The simulation was performed on software NI Multisim^M, Figure 2.7 displays the results of one oscilloscope. Top, middle, and bottom images show the case that ΔV (blue line) = +1V, 0V, and -1V respectively. In all the cases, V1 (red line) + ΔV = V2 (green line) was validated. The other oscilloscope showed the same results. This simulation showed a good working status of the PCB card.

2.3.2. PCB Fabrication



Figure 2.8: The complete electronic circuit of the PCB card.



Figure 2.9: The top side (left) and bottom side (right) of the schema of package.

The package of the circuit was realized on software Altium Designer[®]. Figure 2.8 shows the whole electronic circuit of the PCB card, similarly to the schema of simulation. V1, V4 and V2, V3 represent the corresponding reference electrodes and gate electrodes of Figure 2.2. Figure 2.9 gives a glance at the schema of package.



Figure 2.10: The fabricated PCB device with 5 cm of each side. Left: top view. Right: side view.

Figure 2.10 shows the fabricated and installed PCB card. The total device is applied by +15V/-15V power supply. The potentiometer is regulated by four buttons in the range of 00, 01, 02, ..., 98, 99. As we want ΔV vary like: -1V, -0.8V, -0.6V, -0.4V, -0.2V, 0V, 0.2V, 0.4V, 0.6V, 0.8V, 1V, the adjustment of potentiometer should be: 99, 90, 80, 70, 60, 50, 40, 30, 20, 10, 00. V1, V4 and V2, V3 represent the reference voltages and gate voltages respectively. The dimension of the PCB is 5 cm by 5 cm, and the fabrication price of single piece is 20 yuan (~2.5 euros), including the delivery fee from China to France.

2.3.3. PCB Experimental Validation

The experimental validation of the PCB card consists of three parts: the range of its linearity that reads about the potential of electrolyte through reference electrodes then gives an adding voltage ΔV on the gate electrodes; the response time of circuit to achieve add operation; and the linearity of potentiometer.



The range of linearity



Figure 2.11: The results of range of linearity of the PCB when $\Delta V = -1V$ (top) and +1V (bottom) respectively. X-axis indicates the input voltage on reference electrode V1 and V4, Y-axis indicates the output voltage on gate electrode V2 (red line) and V3 (blue line) correspondingly.

Figure 2.11 shows the results of range of linearity. I have done three measurements of ΔV set to -1V, 0, and +1V respectively. For each value of ΔV , I changed input voltage of reference electrode V1 and V4, and measured output voltage of gate electrode V2 and V3 correspondingly. V1 (or V4) varied from -15V to +15V with an interval of 1V. When $\Delta V = -1V$ (top image), both V2 (= V1+ ΔV) and V3 (= V4+ ΔV) varied from -13V to +14V. When $\Delta V = +1V$ (bottom image), both V2 and V3 varied from -14V to +13V. Although the PCB cannot reach to +16V or -16V when $\Delta V = +1V$ or -1V, this range of linearity has been good enough for the EOF measurement, because the potential of electrolyte is normally inferior to +15V and superior to -15V. It can also be seen that the PCB works symmetrically.



Figure 2.12: The result of response time of the PCB card with $\Delta V = -1V$. Orange line indicates the input signal. Blue line indicates the output signal.

Figure 2.12 shows the response time of the PCB card. A square signal with amplitude of 10Vpp and frequency of 1KHz was given to the input V1 and V4, I set $\Delta V = -1V$ and +1V separately, and I measured

the response time of the output V2 and V3 correspondingly. The response time is about 80µs, already rapid enough for analytical separation.



The linear function of potentiometer

Figure 2.13: Output voltage by varying the value of the potentiometer with an input voltage set to 13V. X-axis indicates the ΔV , Y-axis indicates the measured output voltage.

Figure 2.13 shows the result of the potentiometer linearity. The input voltages on reference electrode V1 and V4 were set to +13V and -13V respectively. I regulated the potentiometer, making ΔV range from -1V to +1V with an interval of 0.1V, then I measured the output voltages on gate electrode V2 and V3 correspondingly. All the results indicated a good linearity of the potentiometer, the output voltage increased almost linearly as ΔV increasing.

2.4. Conclusions

Two big equipments for the EOF measurement were simplified and replaced by a small light cheap PCB card. This PCB card has a large range of linearity, a fast response speed and a functional potentiometer.

REFERENCES:

- [1] D. A. Skoog, F. J. Holler, and S. R. Crouch, "Principles of instrumental analysis," 7th Edition, CENGAGE Learning, Boston, USA, 2017.
- [2] J. Cazes, "Analytical instrumentation handbook," 3rd Edition, CRC Press, Boca Raton, USA, 2004.
- [3] A. Plecis, J. Tazid, A. Pallandre, P. Martinhon, C. Deslouis, Y. Chen, and A-M. Haghiri-Gosnet, "Flow field effect transistors with polarizable interface for EOF tunable microfluidic separation devices," *Lab Chip*, vol. 10, pp. 1245-1253, 2010.
- [4] T. L. Brown, H. E. LeMay Jr., B. E. Bursten, and J. R. Burdge, "Chemistry: The central science," 9th Edition, Pearson Education, UK, 2003.

- [5] A. Pallandre, "Intégration du transistor fluidique à effet de champs et à interface polarisable dans un pont de Wheatstone," HDR, Université Paris-Sud, 2015.
- [6] J. Gamby, "Stratégies de transduction en puces microfluidiques pour applications bioanalytiques," HDR, Sorbonne Université, 2014.
- [7] P. Horowitz and W. Hill, "The art of electronics," Cambridge University Press, Cambridge, UK, 1989.
- [8] J. Millman, "Microelectronics: Digital and analog circuits and systems," McGraw-Hill, USA, 1979.
- [9] "Voltage divider," <u>https://en.wikipedia.org/wiki/Voltage_divider</u>.

Chapter 3: Device Fabrication and Experimental System

3.1. Overview

The microfluidic fabrication is a long, complex and uncertain process. First, many of the fabrication methods require special equipment in cleanroom facilities, which can take advantages from the advent and the advance of IC and MEMS miniaturization technology [1]. Second, different fabrication methods can directly affect different end devices performances and behaviors. It has been proved in literatures that the zeta-potential and the EOF measurements (and thus the EOF mobility) can vary according to fabrication methods [2, 3]. Moreover, the microfluidic fabrication faces numerous difficulties concerning materials, which is the case about polarizable material studied in this thesis. For these reasons, the fabrication processes play very important role in the microfluidic technology.

A wide range of materials have been used for microfluidic devices [4, 5], from conventional hard materials, *i.e.* silicon-based materials [4-8], to soft materials, *i.e.* polymer-based materials [3, 5, 6, 9-11]. One should also note that more recently new materials have emerged from innovative hydrogel [12-18] and paper-based materials [19-23] to hybrid and composite materials [24-27].

The polymer-based materials, being the most-commonly used nowadays for microfluidic devices, offer a great flexibility [28, 29], a rapid fabrication and an inexpensive cost. According to their physical properties, they can be classified into three groups [5]: the elastomers, the thermosets, and the thermoplastics.

The elastomer is a sort of polymers with viscoelasticity, low Young's modulus and high failure strain [30]. It consists of cross-linked polymer chains in which those covalent cross-linkages make the elastomer stretch or compress under external force and return to the original shape when the force is removed [5, 30]. The most popular elastomer used in microfluidics is polydimethylsiloxane (PDMS) [31, 32].

PDMS is a flexible polymer with high elasticity, allowing easy and low-cost microfabrication [33]. Due to its low surface free energy, PDMS behaves itself in a hydrophobic way for which there is no need of any surface pretreatments [9]. Moreover, PDMS exhibits a high biocompatibility, which makes it broadly used in bio-related researches. However, there are notable limitations of PDMS, the two most major problems are its permeation of gases and adsorption of samples. Because of a porous matrix of Si-O backbones covered with alkyl groups in PDMS, water evaporation happens through PDMS channel walls [34], which leads to a change in concentration of solution and let it be restricted for aqueous solutions [35]. The contamination of PDMS is nonnegligible, such as the absorption of small hydrophobic molecules into channel walls and adsorption of biomolecules onto channel surfaces [5]. These influence biological results and more often surface treatments are needed [36, 37]. Moreover, since those adsorbed molecules are difficult to be removed which makes PDMS a disposable material [38]. Another inconvenience of PDMS concerns the difficulty to integrate electrodes directly on its surface, particularly in our case.

The thermoset is an irreversible material when heated or radiated [39], which means it cannot be reshaped once cured. Thermosets (*e.g.* SU-8 photoresist and polyimide) have some good properties, such as stability at high temperatures, resistance to most solvents, and good optical transparency [5],

meaning that they can be adapted for the fabrication of microfluidic channels [29, 40], and even more for the true 3D microfabrication of high-aspect ratio and free-standing structures [41, 42]. As every coin has two sides, thermosets are less served to flexible configuration because of its high stiffness and the microfabrication by thermosets costs a lot.

Unlike the thermoset, the thermoplastic can be reshaped multiple times by reheating after being cured [5]. Typical thermoplastic materials are: PMMA; PEEK; PS; PC; PET; PVC; *etc.* [6, 10, 11, 29, 43]. In contrast with PDMS, these materials have a low permeability to gas even if they exhibit a better solvent compatibility [5].

Aside from the organic polymers mentioned above, cyclic olefin copolymer (COC) or cyclic olefin polymer (COP) is a relatively new class of amorphous polymers used in a vast range of applications [44]. Owing to its excellent chemical resistance, it is a popular material for lab-on-a-chip that I have also used as microfluidic channels during my internship at Institute Curie [5, 45, 46].

Before the polymer-based materials, the silicon-based materials such as silica or glass have also been largely used for the first-generation of microfluidic devices thank to the development of micro- and nano-technologies in the semiconductor industry [47, 48]. Despite that the silica or glass microchip fabrication often needs very strict environments such as clean room, and high temperature and pressure for bonding, the specific properties of glass like thermostability, organic solvent compatibility, gas impermeability, and especially simple metal depositing make it still popular in microfluidics [49, 50]. Silicon is one material which was used as substrate for a long time in micro/nanoelectronics, however, it is opaque and not insulating. For all these reasons, for my thesis, we chose bare borosilicate glass as our microchip substrate.

Glass is an amorphous material with many advantages: first it is highly non-reactive to a variety of aggressive chemicals, such as acids, aggressive bases like NaOH and KOH, and alcohols [51, 52], which make it usable in biological and chemical experimental apparatus [7, 8]; second it is optically transparent, which is very good for the optical detection [53]; third it has high thermoconductivity and stable electroosmotic mobility on its surface [5]; finally since it is an insulating material, electrodes can be deposited directly on its surface. Table 2 shows the advantages and disadvantages of each material that has been described in this introduction.

	Advantages	Disadvantages
PDMS	High elasticity Low costs Low surface free energy High biocompatibility	Gas permeation Sample adsorption Difficult electrodes integration Organic solvents incompatibility
Thermosets	High temperature stability Solvents resistance Optically transparent 3D microfabrication High-aspect ratio structure Free-standing structure	Irreversible High stiffness High costs
Thermoplastics	Reversible and reshaped Gas impermeability Solvents compatibility	Bad contact with other surface
COC/COP	Excellent chemical resistance	
Silicon	Thermostability Organic solvent compatibility Gas impermeability	Clean room needs High temperature and pressure bonding High costs Opaque Semiconductor
Glass	Aggressive chemical resistance Optically transparent High thermoconductivity Stable electroosmotic mobility on surface Electrically insulating	Special etching needs [54]

Table 2: Summary of advantages and disadvantages of common materials for microfluidics.

This chapter started with a presentation of typical microfabrication processes for our microchip, then followed by a description of experimental system including the bench, the microchip installation, the measure launching, and the data analysis.

3.2. Step-by-Step Fabrication Processes for Microfluidic Devices

The fabrication of the whole microfluidic chip has three steps: the microfabrication of PI-FFET on the glass substrate; the fabrication of the fluidic microchannels based on PDMS or Dry film resist; and the bonding of these two parts for sealing the fluidic device.

3.2.1. Typical Microfabrication Processes of PI-FFET on Glass Substrate

The PI-FFET device consists of three different layers: a sticking underlayer, an electronic circuit layer, and a top polarizable layer. Thus, the total fabrication process needs three lithography steps with alignment, deposition of materials (metals and CNx) and resist lift-off respectively.



Figure 3.1: Top view photographs and micrographs of three layers. (A)- Optical micrograph of the sticking underlayer. (B)- Photograph of the electronic circuit layer. (C)- Zoom of three pairs of electrodes. (D)- Zoom of the right center part of the microfabricated substrate.

Figure 3.1 shows the designs of each layer from the sticking underlayer to the electronic circuit channel and the final top polarizable interface. Figure 3.1A displays the structure of the sticking underlayer,

which is very simple, just a rectangle pattern. The length and width of it are 2400 µm and 250 µm (masque 1) respectively. The pattern of the top polarizable CNx layer has the same rectangle except its length and width are bigger, being 2411 µm and 250 µm (masque 2) (see Figure 3.1D where CNx appears in dark tan). Figure 3.1B illustrates the configuration of the electronic level. It has a symmetrical structure based on three pairs of electrodes: 1 and 1' for the electrophoretic electrodes, 2 and 2' for the reference electrodes, 3 and 3' for the gate electrodes. These six electronic pads converge to the center of the design, as marked in red in Figure 3.1B. Figure 3.1C is a zoomed photograph of the red part, which can be observed more clearly. The first pair of electrodes concerns the electrophoretic electrodes, appearing as three-meniscus shape. These electrodes allow applying an electric field and thus modulating the electrophoretic voltage. Concerning the second pair of electrodes named reference electrodes, as their name implies, their function is to adjust the overvoltage of the gate electrodes by precisely measuring the potential of the electrolyte. The last pair of electrodes are the working electrodes, named gate electrodes, which modulate the surface charge of the CNx film, thus controlling the electroosmotic flow. Finally Figure 3.1D shows the zoom of right side of the electronic channel and depositions of the sticking underlayer (dark blue) and the CNx film (dark tan) in the center, together forming the polarizable interface. Noted that the gate electrode is sandwiched between the sticking underlayer and the CNx layer.



Figure 3.2: Cross-sectional description in 10 steps of the microfabrication of PI-FFET on glass substrate. 1- Piranha cleaning of the glass substrate. 2- Spin coating of the photoresist AZ 5214. 3- UV

insolation of AZ 5214. 4- Flood exposure (no mask) of AZ 5214. 5- Development of AZ 5214. 6- RIE of the residual resist. 7- Sticking underlayer deposition by sputtering. 8- Lift-off of the photoresist. 9-Repeat from step 2 to 8 for the electronic circuit layer deposition. 10- Repeat from step 2 to 8 for the polarizable layer deposition.

A step-by-step fabrication process is presented as follow:

- 1. The first step is substrate cleaning (see step 1 of Figure 3.2). First, the substrate is put into a beaker with one third of acetone then the beaker is put in an ultrasonic machine with parameters of 37 kHz, 30% power, under the clean-room temperature during 3 minutes. This step is used to remove the inorganic residues on the substrate. Then, the substrate is taken out and rinsed by isopropanol and dried by nitrogen N₂ gas. Later, the piranha solution is prepared with a mixture of 95% sulfuric acid (H₂SO₄) and 30% hydrogen peroxide (H₂O₂) in a proportion of 3:1 V/V (in our case). Noted that the solution should always be prepared in the order of H₂SO₄ followed by H₂O₂ to favor the apparition of heat from the exothermic mixing reaction. The substrate is put into this piranha solution for 20 minutes, then rinsed by deionized water for 10 minutes, dried by N₂ at last. This piranha step is to clean organic residues off glass substrate. Unlike chromic acid solution, piranha solution does not contaminate glassware with heavy metal ions [55].
- 2. The second step is photoresist spin coating (see step 2 of Figure 3.2). Generally, photoresists can be classified to three types: positive, negative and reversible. The positive photoresist is the one that the exposed areas are dissolved in the development solution, copying the same pattern of the mask, like AZ9260, S1805, S1828, etc. On the contrary, the negative photoresist is the one that the exposed areas are almost insoluble in developer because of the crosslinking, transforming a reversal pattern of the mask to the sample, such as maN2405, nLof2070, SU8, etc. As the name implies, the reversible photoresist is the one with the property to change its polarity after annealing or an irradiation flood. For example, the resist AZ 5214 E, which is the most commonly used reversible photoresist in our lab and basically for lift-off technique. Prior to spin coating, 5 minutes of dehydration bake for the clean substrate is necessary to avoid the surface moisture, which often allows the developer penetrating the photoresist/substrate interface and undercutting the photoresist pattern [56, 57]. The AZ 5214 is deposited to the center of rotating substrate, and the spin performs with a fixed program, which sets the final coating thickness and allows a homogenous photoresist. Here, the spin rotates during 30s with a speed of 4000 rpm and an acceleration of 2000 rpm. The final thickness of AZ 5214 depends on its viscosity, around 1.4 μm thick in our case. Then the resist is baked during 1mn 30s at 125°C on hot plate to drive off residual solvents and solidify the photoresist film.
- 3. The third step is the first insolation (see step 3 of Figure 3.2). SUSS MicroTec MJB4 mask aligner is employed for the optical lithography. After exposure under a 320 nm wavelength ultraviolet (UV) light for 5s (corresponding to an energy of 10 mW/cm²), the substrate is then taken to the second bake, named "reversal-bake", during 2mn at 125°C. This step is important, because it makes the exposed areas crosslink and insoluble in developer and no longer light sensitive, whereas, the unexposed areas remain as a normal positive photoresist [58].
- 4. The fourth step is the second insolation, named "flood" (see step 4 of Figure 3.2). It is a kind of insolation without any mask. The duration of flood step is 60s with the same energy as the first one. After the flood exposure, the unexposed areas during the first lithography are dissolved in developer while the exposed areas remain onto the substrate.

- 5. The fifth step is the development (see step 5 of Figure 3.2). The developer for AZ 5214 is AZ MIF 826 and the duration ranges from 20s to 2mn, depending on the quality of developer and the complexity of pattern. As a result, a negative image of the mask pattern is reproduced on the substrate.
- 6. The sixth step is the reactive-ion etching (RIE) (see step 6 of Figure 3.2). It is a kind of dry etching generated by chemically reactive plasma and produces a directionally and anisotropically etching profile. This process is provided by NEXTRAL NE100 in our lab and is effectuated by a program "OxyAlu" with SF₆/O₂ gas flow for 30s. The aim is to remove the probable residual photoresist.
- 7. The seventh step is the sticking underlayer deposition (see step 7 of Figure 3.2). Here, it is considered to be SiC. This step is realized by Plassys MPS800 through sputtering, a kind of physical vapor deposition (PVD). The SiC film is deposited with a power of 500W, a pressure of 1Pa and a speed of 2.27 Å/s during 1mn 21s, allowing a thickness around 20 nm.
- 8. The last step to finish the deposition of sticking underlayer is lift-off process (see step 8 of Figure 3.2). It is to remove the rest of photoresist by using acetone solution. The detailed operation is to leave the substrate in acetone solution for half an hour, then finished by ultrasonic oscillation. The duration depends on the progress of lift-off, which should be checked out under the optical microscope from time to time.
- 9. The ninth step is the repeat from step 2 to 8 except for the deposition of step 7, it is the electronic circuit layer to be deposited at this time (see step 9 of Figure 3.2). The layer consists of a 5 nm sticking film of Ti and a 25 nm conductive film of Pt. The deposition is effectuated by Alcatel SCM600 through electron-beam physical vapor deposition (EBPVD).
- 10. The last step for the microfabrication of the PI-FFET is the final deposition of the polarizable interface, *i.e.* the CNx layer (see step 10 of Figure 3.2). This step also repeats from step 2 to 8 except step 7, which is replaced by the CNx layer. The CNx deposition is also effectuated by sputtering, unlike the SiC film is deposited under pure argon (Ar) gas, the carbon film is doped with nitrogen (N₂) under a mixture gas of Ar and N₂. The N₂/(N₂+Ar) ratio of gas, *i.e.* ratio of pressure or of flow in this equipment, is suggested to be 14.9:100. However, it is often calculated to be around 20% at the final deposited film. This proportion makes the CNx film work as dielectric. The final fabricated pattern is shown in the last photograph of Figure 3.2.

3.2.2. Two Microstructuring Methods of Microfluidic Channels

In this section, two methods for the microchannel structuring are presented successively.



Figure 3.3: Top view photographs and micrograph of microchannel design. (A)- Photograph of total view of microfluidic channels. (B)- Zoom of the central channel. (C)- Optical micrograph of the central channel.

Figure 3.3A shows the total design of the microfluidic channels. As it can be seen, it is a symmetric pattern with four branches and four reservoirs at the corner, as well as one central channel (circled in red rectangle). Those reservoirs are connected to the external cannula and pipe connectors to let the liquid circulate through the microchannels. The six pads surrounding the channels are prepared to connect the external electronic instrumentation (power supply units and voltage followers). The red parts in Figure 3.3B indicate two restrictions of microfluidic branch with a width of only 80 μ m, compared to the normal branch having 200 μ m width channels. These restrictions can provide different fluidic resistance and allow to determine the fluidic resistance of central channel. Figure 3.3C zooms in the central channel, the two round reservoirs superpose on the three-meniscus shaped electrophoretic electrodes in Figure 3.1C.

Fabrication Processes of Microchannels Based on PDMS

A common method to mold microfluidic channels in PDMS is to create a mold from a photoresist, for example, the SU-8 family on silicon wafer. SU-8 is a negative photoresist, which means the exposed areas remain. Figure 3.4 illustrates the fabrication steps for the creation of a SU-8 mold and a PDMS-based microfluidic channels [59].



Figure 3.4: Cross-sectional description in 6 steps of the fabrication of PDMS-based microfluidic channels. 1- Piranha cleaning of the Si wafer. 2- Spin coating of the photoresist SU-8 2050. 3- UV insolation of SU-8 2050. 4- Development of SU-8 2050. 5- PDMS pouring, degassing, and curing. 6-PDMS peeling and the final created PDMS-based microfluidic channel.

- 1. The first step is Si wafer cleaning by piranha solution to remove any surface contamination (see step 1 of Figure 3.4) that has been detailed in Section 3.2.1.
- 2. The second step is to deposit the photoresist SU8 2050 in a homogenous way by spin coating (see step 2 of Figure 3.4). The spin speed is 2700 rpm during 30s with an acceleration of 2000 rpm, determining a layer thickness of 40 μm, *i.e.* the thickness of SU-8 mold directly determines the microfluidic channel depth. Then, the wafer is soft baked at 65°C during 2mn and at 95°C during 7mn to remove the solvents in the resist and to relax the polymeric matrix.
- 3. The third step is the insolation by UV light through a mask that defines the mold pattern (see step 3 of Figure 3.4). The duration of the exposure lasts for 25s. Before the development, a hard bake is applied (see above step 2).
- 4. The fourth step is the development of SU-8 by its proper developer for about 2mn 30s, then rinsing it by isopropanol (see step 4 of Figure 3.4). It results in SU-8 mold more mechanically and chemically robust [60].
- 5. The PDMS is prepared in advance: the PDMS elastomer and a curing agent are mixed together at a ratio of 9:1 w/w. The proportion of curing agent determines the elastic and mechanical properties of PDMS, the more curing agent is the less elastic is PDMS. The mixture is placed in a centrifuge machine following 3mn rotation to have adequately mixing. Then the PDMS mixing is poured onto the SU-8 mold. Because the mixture of PDMS often introduces bubbles that must be removed before curing. Thus, the total mold is placed in a glass desiccator connected to a membrane vacuum pump to degas bubbles. After degassing, the mold and the liquid PDMS are put into oven at 60°C for one night to let the mixture crosslinking. Therefore, a PDMS mold is finished (see step 5 of Figure 3.4).
- 6. The sixth step is to peel off PDMS mold from SU-8 master (see step 6 of Figure 3.4). Thus, a real PDMS-based microfluidic channel is then created.

Fabrication Processes of Microchannels Based on Dry Film

Dry film is a negative dry photoresist with a thickness of 35 μ m that means the depth of microfluidic channel is 35 μ m. It is a three-layer film with two transparent protective films and one blue photosensitive film. The structuring of dry film-based microchannels is descripted in Figure 3.5.



Figure 3.5: Cross-sectional description in 4 steps of the fabrication of dry film-based microfluidic channels, following the tenth step of Figure 3.2. 1- Deposition of dry film by a laminator. 2- UV insolation of dry film. 3- Development of dry film. 4- Annealing of dry film. 5- Photograph of the laminator ©PEAK POUCH LAMINATORS. 6- Micrograph of the fabricated dry film-based microfluidic channel.

- The first step is the dry film lamination (see step 1 of Figure 3.5), which is done by PEAK POUCH LAMINATORS Peak High Speed PHS-330 laminator, as shown in Figure 3.5-5. The deposition is performed under a temperature of 100°C with a median speed. One of transparent films is peeled off, the photosensitive blue film is deposited onto microfabricated PI-FFET substrate, then the whole substrate is put into the laminator. Once the deposition is finished, the dry film is soft baked on a hot plate at 90°C during 5mn.
- The second step is the UV exposure with wavelength of 320 nm, power of 10 mW/cm² during 9s (see step 2 of Figure 3.5). Then second transparent film on the other side is peeled off and the dry film is hard baked (see above step 1).

- 3. The third step is the dry film development by 8.5 g/L Na₂CO₃ solution (see step 3 of Figure 3.5). The duration of development depends on the disappearance of blue microchannels, which can be observed directly by eyes, a typical duration of 2mn is generally sufficient.
- 4. The last step is the dry film annealing (see step 4 of Figure 3.5). The dry film is placed in oven at 200°C for at least one hour. The change of dry film color occurs after annealing from blue to yellow green, if not, the annealing time is not sufficient.

3.2.3. Integration of PI-FFET and Microchannels

The integration of PI-FFET and microfluidic channels has two distinct routes, depending on what kind of material will be used to define the microfluidic network (PDMS-based or dry film-based). Figure 3.6 describes both two routes.



Figure 3.6: Cross-sectional descriptions and photographs of the integration of the PI-FFET and the PDMS-based (A and B)/dry film-based (C to F) microfluidic channels. (A, E)- PDMS bonding to glass substrate by oxygen plasma. (B)- Top view photograph of the final PDMS-based microdevice. (C)-Photograph of the mold for micro-sandblasting. (D)- Glass hood bonding to dry film by press. (F)- Top view photograph of the final dry film-based microdevice. The green paths in (B) and (F) indicate the fluidic channels.

In the case of PDMS, first of all, the cured PDMS is cut and pierced by a punch for inlets/outlets formation. After rinsing and drying the substrate and PDMS piece by isopropanol, an oxygen plasma is applied to active the silanol groups on the PDMS surface [61], allowing a permanent bonding between PDMS and glass substrate (see Figure 3.6A). This step is performed in NANONEX CORPORATION Ultra-100 plasma cleaner/coater in our lab. After finishing plasma, the PDMS piece is aligned and bonded to the substrate under optical binoculars. This alignment is often difficult and requires high precision because the central channel of PDMS has to be exactly superposed onto the polarizable interface of

substrate. After that, six electronic pins are welded to the corresponding pads on the substrate and fixed by LOCTITE® EA 3430 epoxy adhesive. Figure 3.6B shows the final fabricated microfluidic device.

In the case of dry film, at first, a new glass substrate is sandblasted according to the pattern on the mold (see Figure 3.6C). The micro-sandblasting is a delicate operation where a stream of abrasive material is propelled from the machine under high pressure and grinds or shapes a pattern on a surface. Here, the abrasive material is glass beads with a diameter from 30 to 45 µm, it is also called microsandblasting. This sandblasted glass substrate is a hood to close the open microchannel of dry film. Figure 3.6D shows the bonding of dry film to the glass substrate effectuated by Specac® manual and hydraulic press under 100°C, 3 tons for more than one hour. Noted that before bonding, all the holes of the glass substrate should be aligned with the dry film. After that, four pierced PDMS pieces are bonded by oxygen plasma to the top of the hood, and aligned to the four inlets/outlets of microfluidic channels (see Figure 3.6E). At last, Figure 3.6F shows the final fabricated dry film-based microfluidic device with electronic pins.



3.3. **Description for Experimental System**

CCD camera and its power supply. (D)- Chip holder. (E)- Matlab® command interface. (F)- Fluid multiplexer and pressure controller. (G, H)- Footswitch and hand throttle.

Figure 3.7: Total view photographs of the experimental bench. (A)- Inverted optical microscope. (B, C)-

3.3.1. Experimental Bench

Figure 3.7 shows the total view of the experimental bench. Figure 3.7A is an inverted optical microscope that often allows experts to observe the fluorescent targets. Figure 3.7B and C together constitute the CCD camera, which is sensitive and responds to the light, converting the video signal to the digital signal. The CCD camera is often used in the photometry, here we use it to observe and measure the speed of the fluorescent beads. Figure 3.7D shows the chip holder on the microscope and the connected microfluidic device. The window in Figure 3.7E presents the command interface, which was coded and enslaved by Matlab[®]. This greatly facilitates the fluid management and allows the beads speed measurement and the data acquisition automatically. Figure 3.7F presents the fluid multiplexer and the pressure controller. This system controls the fluid circulation in the microfluidic channels through hydraulic pressure. The footswitch in Figure 3.7G and the hand throttle in Figure 3.7H together constitute the external system to simplify the manipulation. The former allows to manage the fluid circulation by feet: "flush" (the liquid enters to the microchannels by one side, for example, either through reservoir 1 and 2 thus reservoir 3 and 4 will be the outlets or the opposite situation seeing in Figure 3.3), "equilibrium" (the liquid enters to all the four entrances in the same time with the same pressure), and "stop" (no liquid flowing in the channels). The hand throttle offers the possibility to manually modify the value of pressure in real time.



Figure 3.8: Photographs of the external electronic equipment. (A)- Generator for the electrophoretic field. (B, C)- Two old generation followers and the power supply to adjust the V_{gate} (two channels in the same source meter unit).

As the measurement takes place under the electrophoretic field (an electric field providing a voltage of +15V), thus, a generator is employed to this function (as shown in Figure 3.8A). Figure 3.8B and C show the two followers and its power supply. The follower is connected between the reference electrode and the gate electrode, its function is to modify the potential on the gate electrode in terms of the potential regarding to liquid potential measured by the reference electrode. This relation between the liquid potential and the V_{gate} is crucial to avoid electrochemical reactions in the separation channel.

3.3.2. Step-by-Step Experimental Description

The experimental manipulation consists of three parts: the installation of the microfluidic device that includes the preparation of the fluorescent beads and the connection to the external cannula and pipes; the experimental launching on Matlab[®] and the way of measurement; the data treatment and analysis.



Figure 3.9: Description of the experimental schema.

Figure 3.9 shows the simplified schema of the experimental setup. The air is pushed into the pressure controller driving out the millimolar aqueous KCl solution flowing in one of the channels of multiplexer. Two outlets of the multiplexer are connected to the four reservoirs of the device. The liquid enters into one side of channels and flows out of another side, *i.e.* two reservoirs at left or at right, this is "flush" mode. Whereas, the same pressure can also be applied at the four reservoirs of the microfluidic bridge, it is the "equilibrium" mode. The fluidic path is colored in blue. The red and black path represent the voltage and the mass applied to the device respectively, providing an electric field to realize the electrophoresis on the polarizable surface at the central channel. Two followers are connected to the reference and gate electrodes as colored in green.

Microfluidic Chip Installation

The microfluidic device installation consists of two steps: the installation onto chip holder and the injection of fluorescent beads. The following steps describe the microfluidic chip installation.

- First of all, we prepare two bottles, one of deionized water, and another of aqueous KCl solution with a molarity of 10⁻³M (the concentration can be changed). The molar mass of KCl is 74.5 g/mol, so to have 500 mL of 10⁻³M, we need 37.25 mg of dry KCl powder to be dissolved in 500 mL of deionized water.
- 2. Second, the microfluidic device is installed onto the chip holder and fixed by scotch tapes. After evacuating the air bubbles in both cannula and pipes, the device is connected to them one by one under the function of "flush" phase. Thus, both four cannulas are inserted to the holes of PDMS and the liquid can thus flow into the microfluidic channels. Normally, the insertion of cannula is often along with the generation of air bubbles at the inlets, therefore, a program named "bubbleout.m" was designed to evacuate these bubbles, which consists of 2 cycles of "equilibrium" and 1 cycle of "flush", working one after the other successively until all the bubbles are evacuated.
- 3. Then, we replace the deionized water by KCl solution carefully and prepare the fluorescent beads. The recipe is 10 mL of KCl 10^{-3} M, plus 150 μ L of fluorescent polystyrene microspheres FX100 with

diameter of 1 μ m, plus 200 μ L of TWEEN[®] 20 nonionic detergent (an aqueous solution containing 0.5% of tween V/V) for a stable mixture by reducing the particles adsorption on the glass substrate surface. Once the beads are prepared, they are then injected into one side of the cannula inlets by syringe, here for example, the reservoirs 1 and 2 in Figure 3.3A. Then, a "flush" phase is applied to branches 1 and 2 to push the beads flow into the channels. When we observe that fluorescent beads are inside the bridge, and after checking that there are no air bubbles under inverted microscope, we can launch the EOF measurement. There is a little tip to identify if there were small bubbles in the microfluidic device or not: when applying "equilibrium" phase, if the beads move, that means that there are bubbles inside, and the moving direction helps to find the location of the bubbles by simply following the beads in the fluidic network.



Experimental Launching

Figure 3.10: Picture of the experimental Matlab graphic user interface.

Figure 3.10 shows the experimental manipulating interface, which is a program based on Matlab[®] to simplify the manipulation of measurement. The following steps indicate the launching process.

- 1. First of all, initiating the program by clicking the "Initialization", when it turns to green, meaning that the program can be settled and all instruments communicated with PC are ready.
- 2. In the window of "Electrophoresis", setting the electrophoresis voltage to be 15V. For the rest two parameters, they can be remained as default.
- 3. Then passing to the window of "Transistor". The number of measurements is normally to be 5. The gate voltage can be changed between -1V/+1V manually at each measurement. Noted that, if we

use the PCB card mentioned-above in Chapter 2, we do not need to modify the value of gate voltage in this window because the PCB card will take place its function.

- 4. The window of "Pressure Controller" shows the value of pressure applied, which can be controlled by the hand throttle. And in the window of "Save", we can note down the "File name" that the results can be saved automatically.
- 5. After confirming all the numbers, clicking "Pressure" to apply 300 mbar. And applying "equilibrium" phase to remain a hydrodynamically stable state. Then, choosing a region of interest (ROI), normally, it is in an area of restriction channel. At last, clicking "EOF measure", the measurement of the speed of the fluorescent beads will be effectuated automatically and successively, allowing the calculation of the EOF.

Briefly, the EOF measurement includes two steps. The first step is two calibrations. The fluidic resistance calibration is achieved firstly. In this calibration, it measures the velocity of fluid in each arm of the μ FWB (see Figure 1.9B of Section 1.3.2), the results are stored in Matlab file. Then it repeats the same way in the second Poiseuille calibration, all the steps aim to determine the proportionality factor α_i (i = 1, 2, 3, 4) of each arm. Then, we can choose one arm of the μ FWB to perform the EOF measurement.

Data Treatment

The method used to measure the flow rate of beads is particle image anemometry (PIA) that can determine flow rate within a few milliseconds. It has been coded to perform a full frame cross-correlation algorithm of the successive CCD images of the fluorescent beads in motion [62]. The determined flow rate will be expressed in pixel/s that we should convert it to μ m/s. It is easily done after a scale calibration with microscope and Image J analysis of the CCD image. Precisely, measuring the length of one of the channels in μ m under microscope and its corresponding length in pixel that is determined by Image J software. Thus, the flow rate in μ m/s can be studied.

Formula 3-1 gives the calculation of the EOF mobility. It is automatically performed by our Matlab code after storing and analyzing a series of CCD image. v_i is the flow rate measured by PIA. I is the length of the central channel that can be measured under microscope. ΔV is the value of the electrophoretic voltage chosen by experimenter. Among these four parameters, α_i , I and ΔV are fixed. The aim is to modify the gate voltage and obtain its corresponding v_i . After calculating μ_{eof} , the result will be a curve of μ_{eof} under the function of V_{gate} .

$$\mu_{eof} = \frac{\alpha_i \times v_i \times l}{\Delta V} \tag{3-1}$$

3.4. Conclusions

This chapter first presented different materials for the microfluidic, among them we chose glass because it is optically transparent, electrically insulating, and chemically resistant. Then it described typical fabrication process of the PI-FFET in detail, of which the CNx is the essential core of the configuration as it plays as the polarizable interface. The chapter also presented two ways to create the microfluidic channels: PDMS and dry film. The latter is a new technology used on our device, which was under testing by one of the postdoc students when I arrived in our team. At the end, this chapter presented the total experimental bench and the computer interface behind the EOF measurement

manipulation. The hand throttle, the footswitch and the Matlab code together facilitate the control of liquid, as well as the acquisition and the treatment of data.

REFERENCES:

- [1] S-S. Li and C-M. Cheng, "Analogy among microfluidics, micromechanics, and microelectronics," *Lab Chip*, vol. 13, pp. 3782-3788, 2013.
- [2] A. P. Lewis, "An investigation into separation enhancement methods for miniaturized planar capillary electrophoresis devices," PhD thesis, University of Southampton, 2013.
- [3] Z. F. Wang, Y. X. Wu, and K. Puttachat, "Electroosmosis flow (EOF) mobility measurement in polymer micro channels," SIMTech technical reports, 2009.
- [4] H. Becker and A. Manz, "Miniaturized chemical analysis systems-materials and bonding," in *IEE Colloquium on Assembly and Connections in Microsystems*, London, UK, 1997.
- [5] K. Ren, J. Zhou, and H. Wu, "Materials for microfluidic chip fabrication," Acc. Chem. Res., vol. 46, pp. 2396-2406, 2013.
- [6] M. Pumera, A. Merkoçi, and S. Alegret, "New materials for electrochemical sensing VII. Microfluidic chip platforms," *TrAC*, vol. 25, pp. 219-235, 2006.
- [7] A. Berthold, F. Laugere, H. Schellevis, C. R. de Boer, M. Laros, R. M. Guijt, P. M. Sarro, and M. J. Vellekoop, "Fabrication of a glass-implemented microcapillary electrophoresis device with integrated contactless conductivity detection," *Electrophoresis*, vol. 23, pp. 3511-3519, 2002.
- [8] A. Berthold, L. Nicola, P. M. Sarro, and M. J. Vellekoop, "Glass-to-glass anodic bonding with standard IC technology thin films as intermediate layers," *Sens. Actuator A-Phys.*, vol. 82, pp. 224-228, 2000.
- [9] J. Monahan, A. A. Gewirth, and R. G. Nuzzo, "A method for filling complex polymeric microfluidic devices and arrays," *Anal. Chem.*, vol. 73, pp. 3193-3197, 2001.
- [10] M. Pumera, "Analysis of explosives via microchip electrophoresis and conventional capillary electrophoresis: A review," *Electrophoresis*, vol. 27, pp. 244-256, 2006.
- [11] H. Mühlberger, H. Wonhee, A. E. Guber, V. Saile, and W. Hoffmann, "Polymer lab-on-a-chip system with electrical detection," *IEEE Sens. J.*, vol. 8, pp. 572-579, 2008.
- [12] A. M. Ghaemmaghami, M. J. Hancock, H. Harrington, H. Kaji, and A. Khademhosseini, "Biomimetic tissues on a chip for drug discovery," *Drug Discov. Today*, vol. 17, pp. 173-181, 2012.
- [13] P. Domachuk, K. Tsioris, F. G. Omenetto, and D. L. Kaplan, "Bio-microfluidics: Biomaterials and biomimetic designs," *Adv. Mater.*, vol. 22, pp. 249-260, 2010.
- [14] L. G. Griffith and M. A. Swartz, "Capturing complex 3D tissue physiology in vitro," *Nat. Rev. Mol. Cell Biol.*, vol. 7, pp. 211-224, 2006.

- [15] N. W. Choi, M. Cabodi, B. Held, J. P. Gleghorn, L. J. Bonassar, and A. D. Stroock, "Microfluidic scaffolds for tissue engineering," *Nat. Mater.*, vol. 6, pp. 908-915, 2007.
- [16] M. W. Tibbitt and K. S. Anseth, "Hydrogels as extracellular matrix mimics for 3D cell culture," *Biotechnol. Bioeng.*, vol. 103, pp. 655-663, 2009.
- [17] G. Y. Huang, L. H. Zhou, Q. C. Zhang, Y. M. Chen, W. Sun, F. Xu, and T. J. Lu, "Microfluidic hydrogels for tissue engineering," *Biofabrication*, vol. 3, pp. 012001, 2011.
- [18] A. Khademhosseini, J. P. Vacanti, and R. Langer, "Progress in tissue engineering," *Sci. Am.*, vol. 300, pp. 64-71, 2009.
- [19] A. W. Martinez, S. T. Phillips, M. J. Butte, and G. M. Whitesides, "Patterned paper as a platform for inexpensive, low-volume, portable bioassays," *Angew. Chem. Int. Ed.*, vol. 46, pp. 1318-1320, 2007.
- [20] A. W. Martinez, S. T. Phillips, E. Carrilho, S. W. Thomas, H. Sindi, and G. M. Whitesides, "Simple telemedicine for developing regions: Camera phones and paper-based microfluidic devices for real-time, off-site diagnosis," *Anal. Chem.*, vol. 80, pp. 3699-3707, 2008.
- [21] X. Li, D. R. Ballerini, and W. Shen, "A perspective on paper-based microfluidics: Current status and future trends," *Biomicrofluidics*, vol. 6, pp. 011301, 2012.
- [22] A. W. Martinez, S. T. Phillips, and G. M. Whitesides, "Three-dimensional microfluidic devices fabricated in layered paper and tape," *PNAS Proc. Natl. Acad. Sci. U.S.A.*, vol. 105, pp. 19606-19611, 2008.
- [23] R. Derda, S. K. Y. Tang, A. Laromaine, B. Mosadegh, E. Hong, M. Mwangi, A. Mammoto, D. E. Ingber, and G. M. Whitesides, "Multizone paper platform for 3D cell cultures," *PLoS One*, vol. 6, pp. e18940, 2011.
- [24] H. Wu, B. Huang, and R. N. Zare, "Generation of complex, static solution gradients in microfluidic channels," *J. Am. Chem. Soc.*, vol. 128, pp. 4194-4195, 2006.
- [25] J. H. Zhou, H. Yan, Y. Z. Zheng, and H. K. Wu, "A gold nanocrystal/poly(dimethylsiloxane) composite for plasmonic heating on microfluidic chips," *Adv. Mater.*, vol. 24, pp. 94-98, 2012.
- [26] D. J. Beebe, J. S. Moore, J. M. Bauer, Q. Yu, R. H. Liu, C. Devadoss, and B. H. Jo, "Functional hydrogel structures for autonomous flow control inside microfluidic channels," *Nature*, vol. 404, pp. 588-590, 2000.
- [27] R. G. Blazej, P. Kumaresan, and R. A. Mathies, "Microfabricated bioprocessor for integrated nanoliter-scale sanger DNA sequencing," *PNAS Proc. Natl. Acad. Sci. U.S.A.*, vol. 103, pp. 7240-7245, 2006.
- [28] E. Sollier, C. Murray, P. Maoddi, and D. Di Carlo, "Rapid prototyping polymers for microfluidic devices and high pressure injections," *Lab Chip*, vol. 11, pp. 3752-3765, 2011.

- [29] H. Becker and C. Gäertner, "Polymer microfabrication technologies for microfluidic systems," *Anal. Bioanal. Chem.*, vol. 390, pp. 89-111, 2007.
- [30] "Elastomer," <u>https://en.wikipedia.org/wiki/Elastomer</u>.
- [31] J. C. Mcdonald and G. M. Whitesides, "Poly(dimethylsiloxane) as a material for fabricating microfluidic devices," *Acc. Chem. Res.*, vol. 35, pp. 491-499, 2002.
- [32] A. D. Stroock and G. M. Whitesides, "Controlling flows in microchannels with patterned surface charge and topography," *Acc. Chem. Res.*, vol. 36, pp. 597-604, 2003.
- [33] J. C. Mcdonald, D. C. Duffy, J. R. Anderson, D. T. Chiu, H. K. Wu, O. J. A. Schueller, and G. M. Whitesides, "Fabrication of microfluidic systems in poly(dimethylsiloxane)," *Electrophoresis*, vol. 21, pp. 27-40, 2000.
- [34] R. Mukhopadhyay, "When PDMS isn't the best," Anal. Chem., vol. 79, pp. 3248-3253, 2007.
- [35] J. U. Shim, G. Cristobal, D. R. Link, T. Thorsen, Y. W. Jia, K. Piattelli, and S. Fraden, "Control and measurement of the phase behavior of aqueous solutions using microfluidics," J. Am. Chem. Soc., vol. 129, pp. 8825-8835, 2007.
- [36] A. Paguirigan and D. Beebe, "From the cellular perspective: Exploring differences in the cellular baseline in macroscale and microfluidic cultures," *Integr. Biol.*, vol. 1, pp. 182-195, 2009.
- [37] J. Zhou and A. E. N. Voelcker, "Recent developments in PDMS surface modification for microfluidic devices," *Electrophoresis*, vol. 31, pp. 2-16, 2010.
- [38] W. K. T. Coltro, S. M. Lunte, and E. Carrilho, "Comparison of the analytical performance of electrophoresis microchannels fabricated in PDMS, glass, and polyester-toner," *Electrophoresis*, vol. 29, pp. 4928-4937, 2008.
- [39] "Thermosetting polymer," <u>https://en.wikipedia.org/wiki/Thermosetting_polymer</u>.
- [40] R. J. Jackman, T. M. Floyd, R. Ghodssi, M. A. Schmidt, and K. F. Jensen, "Microfluidic systems with on-line UV detection fabricated in photodefinable epoxy," *J. Micromech. Microeng.*, vol. 11, pp. 263-269, 2001.
- [41] H. Sato, H. Matsumura, S. Keino, and S. Shoji, "An all SU-8 microfluidic chip with built-in 3D fine microstructures," *J. Micromech. Microeng.*, vol. 16, pp. 2318-2322, 2006.
- [42] Y. Z. Zheng, W. Dai, D. Ryan, and H. K. Wu, "Fabrication of freestanding, microperforated membranes and their applications in microfluidics," *Biomicrofluidics*, vol. 4, pp. 036504, 2010.
- [43] "Thermoplastic," <u>https://en.wikipedia.org/wiki/Thermoplastic</u>.
- [44] "Cyclic olefin copolymer," <u>https://en.wikipedia.org/wiki/Cyclic_olefin_copolymer</u>.
- [45] P. Nunes, P. Ohlsson, O. Ordeig, and J. Kutter, "Cyclic olefin polymers: Emerging materials for lab-on-a-chip applications," *Microfluid Nanofluidics*, vol. 9, pp. 145-161, 2010.

- [46] I. Hernandez-Neuta, I. Pereiro, A. Ahlford, D. Ferraro, Q. Zhang, J-L. Viovy, S. Descroix, and M. Nilsson, "Microfluidic magnetic fluidized bed for DNA analysis in continuous flow mode," Biosens. Bioelectron., vol. 102, pp. 531-539, 2018.
- [47] D. R. Reyes, D. Iossifidis, P. A. Auroux, and A. Manz, "Micro total analysis systems. 1. Introduction, theory, and technology," *Anal. Chem.*, vol. 74, pp. 2623-2636, 2002.
- [48] G. M. Whitesides, "The origins and the future of microfluidics," *Nature*, vol. 442, pp. 368-373, 2006.
- [49] B. K. H. Yen, A. Günther, M. A. Schmidt, K. F. Jensen, and M. G. Bawendi, "A microfabricated gas-liquid segmented flow reactor for high-temperature synthesis: The case of Cd-Se quantum dots," *Angew. Chem. Int. Ed.*, vol. 44, pp. 5447-5451, 2005.
- [50] P. J. A. Kenis, R. F. Ismagilov, S. Takayama, G. M. Whitesides, S. L. Li, and H. S. White, "Fabrication inside microchannels using fluid flow," *Acc. Chem. Res.*, vol. 33, pp. 841-847, 2000.
- [51] C. Lin, G. Lee, Y. Lin, and G. Chang, "A fast prototyping process for fabrication of microfluidic systems on soda-lime glass," *J. Micromech. Microeng.*, vol. 11, pp. 726-732, 2001.
- [52] A. Grosse, M. Grewe, and H. Fouckhardt, "Deep wet etching for fused silica glass for hollow capillary optical leaky waveguides in microfluidic devices," J. Micromech. Microeng., vol. 11, pp. 257-262, 2001.
- [53] Y. Jeong, S. Kim, K. Chun, J. Chang, and D. S. Chung, "Methodology for miniaturized CE and insulation on a silicon substrate," *Lab Chip*, vol. 1, pp. 143-147, 2001.
- [54] X. Mu, Q. L. Liang, P. Hu, K. N. Ren, Y. M. Wang, and G. A. Luo, "Laminar flow used as liquid etch mask in wet chemical etching to generate glass microstructures with an improved aspect ratio," *Lab Chip*, vol. 9, pp. 1994-1996, 2009.
- [55] "Piranha solution," <u>https://en.wikipedia.org/wiki/Piranha_solution</u>.
- [56] "Lithography Process Overview," <u>http://www.imicromaterials.com/technical/lithography-process-overview</u>.
- [57] R. R. Dammel, "Diazonaphthoquinone-based resists," 5th printing, vol. TT11, *SPIE Optical Engineering Press*, Bellingham, Washington, U.S.A., 1993.
- [58] "AZ 5214 E Image Reversal Photoresist," <u>http://dvh.physics.illinois.edu/pdf/AZ5214E.pdf</u>.
- [59] A. Pallandre, "Intégration du transistor fluidique à effet de champs et à interface polarisable dans un pont de Wheatstone," HDR, Université Paris-Sud, 2015.
- [60] F. Ru and J. F. Richard, "Influence of processing conditions on the thermal and mechanical properties of SU8 negative photoresist coatings," J. Micromech. Microeng., vol. 13, pp. 80-88, 2003.

- [61] R. S. Martin, A. J. Gawron, S. M. Lunte, and C. S. Henry, "Dual-electrode electrochemical detection for poly(dimethylsiloxane)-fabricated capillary electrophoresis microchips," *Anal. Chem.*, vol. 72, pp. 3196-3202, 2000.
- [62] A. Plecis, L. Malaquin, and Y. Chen, "A particle image anemometry technique for the noninvasive, quick determination of average flow rates in microchannels," *Proc. MicroTAS*, 2007.

Chapter 4: Experimental Work

4.1. Overview

In this chapter, we will present the improvement of CNx adhesion to two major sticking underlayers: SiC and Pt, this will be seen in Experiment 1, 2 and 3. In Experiment 4 and 5, we will show a new architecture that improves greatly the adhesion issues. The last Experiment 6 gives a summary of the behavior of CNx onto different dielectric and metallic materials.

4.2. Experiment 1: Insulating SiC Sticking Underlayer and Its Adhesion Optimizations

4.2.1. Aims of Experiment 1

The primary aim of Experiment 1 was to investigate the stability of sticking underlayer silicon carbide (SiC) for CNx and its adhesion optimizations. Four consecutive tests were performed through various aging experiments including silicon nitride (Si_3N_4) compared testing, piranha etching testing, variation of deposition parameters and annealing at high temperature testing. Measurements of sheet resistance of CNx film over time and in different environments have also been done.

4.2.2. Experiment 1.1: Choice of SiC as Sticking Underlayer

The first experiment was to study the behavior of a thin CNx film (~100 nm) deposited directly on clean glass substrate (see Figure 4.1). Without any sticking underlayer, CNx began to detach just one day after the deposition, observing black dendritic structures. It is worthwhile to note that Figure 4.1 only shows a part of 2-inch sample while these detachments behaved in the same way on the other parts. Therefore, two materials were chosen to be sticking underlayer.



Figure 4.1: Optical microscope picture showing a part of the CNx deposition directly on glass substrate after one day in air at clean-room temperature.

Silicon carbide (SiC) is a semiconductor with a wide bandgap (2.0 eV $\leq E_g \leq$ 7.0 eV) and good tolerance for high temperature, high pressure and friction, it also has a good chemical passivation [1, 2]. While silicon nitride (Si₃N₄) is an insulating material which can be lifted off as good as SiC, however, it is

transparent as thin film, making lithography alignment difficult. Nevertheless, two adhesion tests were still effectuated between SiC and Si_3N_4 .



Figure 4.2: (A)- Photographs of CNx deposited on Si₃N₄ sticking underlayer after 5 days in air at room temperature, the red part circles the boundary between detached part and adhered part. (B)-Photography of CNx deposited on SiC sticking underlayer after 5 days in air at clean-room temperature.

Figure 4.2 shows the behaviors of CNx film deposited on Si_3N_4 (Figure 4.2A) and SiC (Figure 4.2B) sticking underlayers. The samples were first deposited by very thin film (~20 nm) of Si_3N_4 and SiC respectively, then a film of CNx (~100 nm under the same conditions for Si_3N_4 and SiC). Later, the two samples were placed in air at clean-room temperature for five days. The cracking and detachment of the CNx-on-Si₃N₄ film were evident and expanding, while the adhesion of CNx-on-SiC film was instead qualitatively good. To continue investigating the quality of the interfaces between thin layers, a H-shape architecture was fabricated.



Figure 4.3: Top view of the processes to fabricate the H-shape architecture by achieving multiple liftoff. 1- The cleaning process of glass substrate which was detailed in Section 3.2.1. 2- The 20 nm SiC sputtering deposition. 3- The 20 nm Si₃N₄ sputtering deposition in parallel. 4- The 20 nm CNx sputtering deposition across over two parallel films. The letters are given to point out a specific location later in the discussion.

Sample 1 was fabricated based on a 2-inch glass substrate, seeing in Figure 4.3. Three depositions were effectuated on one device to have a good comparison: first was the SiC film deposition (deep blue rectangle in Figure 4.3-2); then the Si_3N_4 deposition which was in parallel to it (light blue in Figure 4.3-3); the CNx film was at last deposited simultaneously across over both the SiC film and the Si_3N_4 film in the same time, forming a H-shape configuration and allowing us to confidently relate the differences in the CNx film properties to the sticking underlayers and not to the CNx deposition parameters. The thickness of these three films was 20 nm.



Figure 4.4: Top view micrographs of the total H-shape architecture (A) and after three weeks in air at clean-room temperature (B).

Figure 4.4A shows the top view of the Sample 1 just after the fabrication. In the horizontal direction, the top layer is Si_3N_4 film while the bottom one is SiC film. The CNx film is in vertical. Noted that there are five spots (a, b, c, d, e) to be observed: spot a is the part that CNx was deposited directly on glass substrate, spot b is SiC deposited on glass, spot c is CNx deposited on SiC, spot d is Si_3N_4 deposited on glass, and spot e is CNx deposited on Si_3N_4 . Figure 4.4B shows the same part of Sample 1 but after 3 weeks in air at clean-room temperature. It is interesting to see that the levels of CNx film detachment on different materials (on the same device and under the exact same environment) were totally different. The local surface morphology and the surface mechanical property of the deposited films were studied before any CNx detachment by means of phase-imaging AFM (PI-AFM). A Veeco Instruments Nanoman DI 3100 AFM was employed for these analyses in our clean room.

PI-AFM is one of the extensions of regular tapping mode AFM. The phase imaging refers to recording the phase shift signal when the probe taps slightly on the sample surface. It can be regarded as a delay in the mechanical oscillation of the cantilever. The nature of phase imaging is the measurement of energy dissipation during the contact between the tip and the sample [3]. The phase shift signal changes to be registered as bright and dark regions in phase images when the probe encounters different areas. Because phase images often produce extraordinary contrast of the variations in composition, adhesion, friction, viscoelasticity, *etc.* that the phase contrast becomes one of the most
commonly used technique to study the mechanical properties of the films [4]. Elastic interactions between tip and sample indicate that the regions are much more crystalline or harder, leading to less phase shift and appear much brighter in phase images [5, 6]. While the inelastic interactions describe more amorphous or softer regions that appear much darker in phase images [7].





Figure 4.5: AFM analysis images of five local surfaces of the deposited films before any CNx detachment. (A)- 1 μm by 1 μm topography (left) and phase (right) images of CNx on glass. (B, C)- 1 μm by 1 μm topography (left) and phase (right) images of (B) SiC on glass and (C) CNx on SiC. (D, E)- 1 μm by 1 μm topography (left) and phase (right) images of (D) Si₃N₄ on glass and (E) CNx on Si₃N₄.

Figure 4.5 displays representative images of topography and phase obtained for a CNx film deposited onto SiC, Si₃N₄ films and glass substrate. Each measurement is presented as a pair of images, the left one represents the topography, and the right one shows the phase image, they were recorded simultaneously. Figure 4.5A shows the CNx film deposited directly onto glass substrate, it can be seen that the CNx film consists of a lot of very small grains that have an important polydispersity and appear heterogeneous. The phase image of Figure 4.5A follows this variation. Figure 4.5B displays the bare SiC film deposited onto glass substrate, the feature indicates the hard grain cores surrounded by softer periphery that can also be seen in its phase image. The image on the left-hand side of Figure 4.5C shows the topography of a CNx film deposited onto the SiC film. The topography images of Figure 4.5B and C are fundamentally quite similar as the CNx film follows partially the topography of the SiC film. However, the phase image of Figure 4.5C clearly shows that the CNx film is more homogenous because there is less variation in the phase shift signal between the cores and the periphery of individual grains. Taken together, we may conclude that the CNx film was deposited on the top of each SiC grain in a relatively uniform way. Figure 4.5D shows the topography (left-hand side) and the phase image (righthand side) of Si₃N₄ film deposited onto glass substrate. Compared to previous images, the Si₃N₄ film appears much smaller grains than those of SiC and CNx films. Moreover, its phase image indicates greater contrast between hard grain cores and their peripheries, which reflects the roughness of the surface or local variation of the composition of the film. From Figure 4.5E it can be seen that the CNx on Si₃N₄ follows the morphology of the previous one, and there is a good correlation between the topography and the phase image. Furthermore, if we compare two phase images of part C and E, it is no doubt that the CNx on Si_3N_4 looks much more heterogenous than the CNx on SiC. This difference probably explains the different adhesions of CNx film on these two sticking underlayers.

This Experiment 1.1 verified that the CNx film detached from glass substrate very soon, around one day after deposition. The adhesion is prolonged when the CNx film deposited onto sticking underlayers. According to the results and AFM analyses of Sample 1, both of the SiC, Si_3N_4 and CNx films exhibited a grainy surface microstructure with important polydispersity and density. On the contrary, the SiC material was a better choice as a robust sticking underlayer for CNx. Further to this, the cleaning or the treatment of the sticking layer prior to the deposition of CNx may have a significant effect over the quality of the structure made of superposed thin layers. We will try to optimize such treatment at the surface of the sticking layer to improve the global robustness of the fluidic transistor in the next section.

4.2.3. Experiment 1.2: Adhering Optimization by Short Piranha Treatment

The aim of Experiment 1.2 was to see how different durations of piranha treatment for SiC film surface influenced on the adhesion of CNx onto SiC, as piranha mixture often effected on the thickness and the roughness of common micro- and nano- fabrication materials [8]. In this experiment, three independent tests were performed progressively.



Figure 4.6: Top view of the processes to fabricate Sample 2. 1- The cleaning process of glass substrate. 2- The 20 nm SiC sputtering deposition. 3- The short piranha treatment on SiC film surface. 4- The 20 nm CNx sputtering deposition on the SiC film with a half shift.

Figure 4.6 shows the fabrication processes of Sample 2 on a 2-inch glass substrate. The total fabrication consisted of two depositions: first was the 20 nm SiC film deposition (deep blue rectangle in Figure 4.6-2); second was the 20 nm CNx film deposition (tan rectangle in Figure 4.6-4) on a half of SiC film, before which a short piranha etching (Figure 4.6-3) was performed. Four samples were prepared with different durations of piranha etching: without piranha, 10s, 20s, and 30s of piranha respectively.

The film roughness and properties were determined by means of AFM. For each sample, the first roughness analysis was carried out on area a of Figure 4.6-4 just after the SiC film deposition. After piranha treatment, the second analysis was carried out on area b. The third scanning was performed on area c after the CNx deposition.



Figure 4.7: AFM analysis images of the sample without piranha (A, B, C) and the top view micrograph after one day in air at clean-room temperature (D). (A)- 1 μm by 1 μm topography image of the SiC film on the glass substrate. (B,C)- 1 μm by 1 μm topography (B) and phase (C) images of the CNx film on the SiC sticking underlayer. (D)- Top view micrograph of the total sample after one day in air.

Figure 4.7 shows the images of the sample without piranha. Figure 4.7A displays the topography of the SiC film deposited on glass substrate, of which the calculated root mean square (rms) value was 1.19 nm. Figure 4.7B and C are the topography (B) and phase (C) images of the CNx deposited on the SiC film, it can be seen that there is a good correlation between them. However, compared to Figure 4.5C, this time was less homogenous. This phenomenon probably came from the contaminations before or during the CNx deposition. Nevertheless, this did not influence the testing because the comparison between the roughness of surface for different time of piranha treatment was the most important. Figure 4.7D shows that the CNx film (the rectangle in the left with lots of black spots) begins to detach from both glass substrate and the SiC film only one day after the deposition.





Figure 4.8: AFM analysis images of the sample with 10s piranha etching (A, B, C) and the top view micrograph after three weeks in air at clean-room temperature (D). (A)- 1 μm by 1 μm topography (left) and phase (right) images of the SiC film on the glass substrate before piranha etching. (B)- 1 μm by 1 μm topography (left) and phase (right) images of the SiC film on the glass substrate after 10s piranha etching. (C)- 1 μm by 1 μm topography (left) and phase (right) images of the CNx film on the SiC sticking underlayer. (D)- Top view micrograph of the CNx onto glass (dark area) and SiC (light area) after three weeks in air.

Figure 4.8 presents the AFM images and the total view of the sample with 10s piranha bath on the SiC surface. Figure 4.8A shows the topography (left-hand) and phase (right-hand) images of the SiC on glass before piranha treatment, it can be seen that the surface of the SiC film is quite heterogeneous with some peaks reaching to 14.5 nm. The root mean square value was calculated to be 1.26 nm. However, after 10s of piranha etching, the surface became much more homogenous as seen in topography (left) of Figure 4.8B, and the roughness value decreased to 0.606 nm. From the phase image (right) of Figure 4.8C, in which the CNx film deposited onto the SiC film, the CNx grains become much smaller and have less contrast compared to what we observed in Figure 4.7. Both indicated that the piranha etching made the SiC surface smoother. Figure 4.8D shows the view of the CNx onto glass and SiC after three weeks, it seems like 10s-piranha etching enhance the adhesion between CNx and SiC.





Figure 4.9: AFM analysis images of the sample with 20s piranha etching (A, B, C) and the top view micrograph after three weeks in air at clean-room temperature (D). (A)- 1 μm by 1 μm topography (left) and phase (right) images of the SiC film on the glass substrate before piranha etching. (B)- 1 μm by 1 μm topography (left) and phase (right) images of the SiC film on the glass substrate after 20s piranha etching. (C)- 1 μm by 1 μm topography (left) and phase (right) images of the CNx film onto the SiC sticking underlayer. (D)- Top view micrograph of the CNx onto glass (dark area) and SiC (light area) after three weeks in air.

Figure 4.9 presents nearly the same experiment except that the piranha etching time was 20s. If we compare the topography (left) and phase (right) images of Figure 4.9A and B, it is clear that before piranha (A) the SiC surface consisted of relatively big grains surrounded by soft periphery. Whereas, after 20s piranha treatment (B), these grains became smaller and seemed to be greatly etched. Moreover, from the phase image of Figure 4.9B, there is a huge contrast compared to what can be seen in Figure 4.8B. This indicated that 20s piranha etching was much stronger than 10s one, which could also be reflected in the root mean square value of the SiC surface that decreased from 1.11 nm to 0.379 nm. Figure 4.9D shows areas of the CNx film deposited on the glass substrate and on the SiC film after three weeks in air. Compared to the surface shown in Figure 4.8D, these detached spots were bigger but with less density.





Figure 4.10: AFM analysis images of the sample with 30s piranha etching (A, B, C) and the top view micrograph after three weeks in air at clean-room temperature (D). (A)- 1 μm by 1 μm topography (left) and phase (right) images of the SiC film on the glass substrate before piranha etching. (B)- 1 μm by 1 μm topography (left) and phase (right) images of the SiC film on the glass substrate after 30s piranha etching. (C)- 1 μm by 1 μm topography (left) and phase (right) images of the CNx film on the SiC sticking underlayer. (D)- Top view micrograph of the CNx onto glass (dark area) and SiC (light area) after three weeks in air.

Figure 4.10 shows the AFM analysis results of the sample with 30s piranha etching. An additional ten seconds did not change a lot the roughness value that was calculated to be 0.587 nm, and before etching the value was 1.39 nm. Both 20s or 30s piranha offered a significant smoothening of the SiC surface. Figure 4.10D tells that there is no big difference between 20s and 30s piranha treatment.

Despite that after the piranha treatment, the SiC surface was smoothened. However, it was hard to say whether it came from the chemical effect or the thermic effect, since the piranha mixture generated a mass of heat (exothermic reaction). Further to this, an extra experiment was performed. Two clean substrates were prepared with a SiC-deposition in the same conditions. Then one was taken for a 30s piranha etching with a temperature measurement of the bath. The other was baked in an oven during one hour at the maximal measured temperature of the piranha bath. After that we compared again their roughness values. It should be paid attention that the temperature of piranha solution was not stable at the beginning, it increased rapidly up to 80°C few seconds after doing the mixture between peroxide water and sulfuric acid. To assure the repeatability of the piranha treatment, we decided to put the sample in the beaker when the piranha solution attained to 80°C.



Figure 4.11: 1 μm by 1 μm AFM topography (left) and AFM phase (right) images of the SiC film on the glass substrate after 30s piranha etching at 80°C (A) and 1h annealing at 80°C (B).

Figure 4.11 shows the AFM analysis topography (left-hand) and phase (right-hand) images of the two samples: Figure 4.11A for the one with piranha and Figure 4.11B for the one with annealing. By comparing the two topography images, it can be seen that the piranha solution indeed etched the SiC grains (A) because they appear smaller than what can be observed on the sample after annealing at 80°C (B). Although we could not get any other information from the phase images, however, the calculations of root mean square value turned to be 0.476 nm for 30s piranha etching while 1.06 nm for 80°C annealing. As the roughness values were around 1.1 to 1.3 nm before any treatment, this result probably explained the cause of the smoothening of SiC surface: both the chemical effect (piranha etching) and the thermic effect modified the topography of the surface, whereas, the former was more essential than the latter. This conclusion will also be confirmed in the following part.



Figure 4.12: Tilted SEM micrographs of the SiC-film surfaces without any treatment (left), with piranha etching during 30s at 80°C (middle) and with annealing during 1h at 80°C (right).

Figure 4.12 displays three representative scanning electron microscope (SEM) images of different treatments of the SiC film surface. The left image shows the morphology of the SiC surface without any treatment, the left above area is the contact metallic pad. It can be seen those little grains of SiC on the surface. Compared to it, the morphology of the right image appears smoother due to one-hour annealing at 80°C in the oven. Nevertheless, the surface is still rougher than the middle one, where the surface was etched by piranha for 30s at about 80°C. These three images confirmed once again the conclusion obtained above that piranha etching had a great influence to lower the surface roughness. To further investigate this influence on the CNx adhesion in KCl solution, another experiment was carried out below.



Figure 4.13: Top view photographs (A, B, C, D) of the CNx polarizable films (marked in blue rectangle) of four samples. From (A) to (D) are: no piranha etching, 10s etching, 20s, and 30s respectively. (E, F)-Micrographs of the CNx film of the samples with (E) 20s piranha etching and (F) 30s correspondingly. Noted that all the samples were immersed in the same 10⁻³M KCl solution at clean-room temperature for three days.

Further experiments were performed to see the aging of adhesion between the SiC sticking underlayer and the CNx film in aqueous KCl environment. Four samples were prepared with the same configuration as described in the Figure 3.2 of Section 3.2.1. Once after the deposition of CNx, the total microfabricated substrates were immersed in KCl solution with concentration of 10⁻³M during three days. The reason of testing in KCl was that the KCl solution plays as the reference electrolyte for the microfluidic transistor polarization study. As it can be seen in Figure 4.13, for the sample without piranha etching (A) and only 10s etching (B) of the SiC film surface, there was no CNx film remained. Whereas, for the sample of 20s piranha (C), the CNx film remained in the end. Thus, behind the roughness evolution, this observation demonstrates that this surface treatment was better than others. The cracks observed on the surface of the film in Figure 4.13E can be attributed to the permeation of the salt solution (after the test in KCl). Figure 4.13D and F shows an interesting phenomenon with the one of 30s etching, the entire CNx film detached from one side and ended at the other side. This may explicate that the adhesion problem between CNx and SiC did not come from the CNx film itself but from the adhesion properties of the interface at the molecular level. To conclude, these results are coherent with the previous part of this manuscript: a 20s piranha treatment provided the smoothest SiC surface for a longer adhesion time of this bi-layered structure.

Table 3: Comparison of calculated root mean square (R _{rms}) of SiC surfaces before and after differer	nt
piranha treatments.	

Roughness R _{rms} (nm)	Before piranha treatment	After piranha treatment	Etching proportion
No piranha	1.19	1.19	0%
Piranha 10s	1.26	0.606	52%
Piranha 20s	1.11	0.379	66%
Piranha 30s	1.39	0.587	58%

Table 4: Comparison of calculated root mean square (Rrms) of SiC surfaces between chemical andthermic effect.

	Roughness R _{rms} (nm)
No piranha no annealing	1.238
Piranha treatment 30s with 80°C	0.476
Annealing 1h with 80°C	1.06

The Experiment 1.2 demonstrated that a short piranha treatment (20s) indeed contributed to a better adhesion between the CNx polarizable film and the SiC sticking underlayer. According to the AFM analyses that the results were summarized in Table 3 and Table 4, the 20s piranha treatment reduced the surface roughness, with an etching proportion of 65.856% (((1.11-0.379)/1.11) x100%), while the others did not make such a significance. The Table 4 also presented the change of roughness that was mostly influenced by piranha (chemical effect), but in lower proportion by thermic effect.

4.2.4. Experiment 1.3: Adhering Optimization by Investigating CNx Deposition Conditions

Generally, the amorphous carbon nitride (CNx) film on sticking underlayers was prepared by radio frequency magnetron cathodic sputtering from a carbon target in a plasma of an Ar/N_2 mixture. The total gas pressure during deposition procedure was 0.4 Pa (3.0 mTorr) with 14.9% of N₂. The magnetron power was set to 200W for 13mn40s. With this set of sputtering parameters, the final thickness of the deposit was expected to be approximately 100 nm. In this section, we investigated the effect of deposition parameters such as RF power and gas pressure on the adhesion resistance property of CNx thin films, prepared by RF magnetron sputtering.

First of all, let us review some knowledge about the sputtering deposition.

Sputtering deposition is one of the physical vapor deposition (PVD) technologies. It defines as the energetic particles, usually argon gas ions bombard the surface of target (or source), because that the bombardment energy is greater than the surface binding energy, thus, the atoms on the surface would be ejected and deposited onto the substrate. The nature of sputtering is an exchange of momentum between the ions and atoms on the surface of target due to collisions. Conventional sputtering is always performed in a vacuum condition full of noble gases (do not react to the target), by applying high voltage, the gases are ionized, forming an ions flow to hit the cathodic target. The advantage of sputtering is that it can realize the film deposition of high melting point materials at low temperature environment.

There are a lot of types of sputtering, among them, the magnetron sputtering promotes the sputter yield by introducing a magnetic field on the surface of cathodic target. Its principle can be expressed as follow: under the function of electric field, the collisions between electrons and argon atoms happen on the path of electrons moving towards the substrate. These collisions ionize argon atoms and produce new electrons. While the electrons continue moving toward the substrate, the argon ions are accelerated and move towards the target, bombarding it with high energy and generating secondary electrons. Because of the correlation of the electric field and magnetic field, the secondary electrons are forced to have E x B drift, prolonged their paths and tied to the vicinity of the target surface. This increases the collision probability between electrons and argon atoms, thus, realizing high speed deposition. The secondary electrons will be deposited onto the substrate in the end when they run out of their energies. And due to their basically low energy, the temperature of substrate could be maintained at a lower level. The advantages of magnetron sputtering are: high speed deposition, low working pressure, low substrate temperature, and large area deposition.

The magnetron sputtering could be classified to DC (direct current) and RF (radio frequency) methods. In RF magnetron sputtering, an AC (alternating current) system replaces DC system, because its frequency is around 5-30 MHz (13.56 MHz internationally used frequency), so called radio frequency. Normally, DC magnetron sputtering cannot be employed for depositing insulating materials, because the positive ions would accumulate on the cathodic target surface and lead to the increase of surface potential, that would finally repel bombarding positive ions and stop sputtering. Therefore, RF magnetron sputtering is designed to overcome this problem. Since the positive and negative polarity of the AC system alternates, when the target is in the positive half cycle, the electrons flow towards target surface, neutralize the positive charge accumulated on the surface, and gather electrons. This causes the surface to exhibit a negative bias, resulting in attraction of positive ions to bombard the target in the negative half cycle, thus achieving continuous sputtering. RF magnetron sputtering is suitable not only for metal targets, but also for insulating targets. Another advantage is that is able to produce self-bias effect. Taken together, RF magnetron sputtering allows a high speed, low temperature and pressure, and no limit of materials deposition.

Theoretically speaking, the power is greater, the sputtering rate is higher, thus the deposited film is less uniform. On the other hand, the gas pressure is higher, the deposition velocity is faster, resulting in a less uniform film; meanwhile the chamber is less vacuum, thereby the probability of contamination is larger, and the deposited film is less compact. To verify whether the power and pressure effect on the CNx film or not, an experiment was carried out as bellow.

The fabrication of Sample 3 was based on the typical fabrication process of PI-FFET as described in Figure 3.2 of Section 3.2.1, except an extra 20s piranha treatment was applied before CNx deposition. There were totally five samples, each sample was given different deposition condition. After the deposition, all samples were immersed in 10⁻³M KCl solution for four days, in clean-room. The observations under optical microscope were systematically done.



Figure 4.14: Top view micrographs of CNx polarizable films with different RF magnetron sputtering deposition conditions. (A)- 200W of power and 0.4 Pa of gas pressure. (B)- 220W and 0.4 Pa. (C)- 240W and 0.4 Pa. (D)- 200W and 0.6 Pa. (E)- 200W and 0.8 Pa. Noted that all the samples were immersed in the same 10⁻³M KCl solution at clean-room temperature for four days.

Figure 4.14 shows different situations of the CNx films under different deposition conditions after four days in KCl solution. Figure 4.14A, B and C compared different RF powers for sputtering deposition

with the same gas pressure 0.4 Pa. From A to C were: 200W, 220W and 240W, respectively. Both of them show detachments of the CNx, and it occurred always from the edges of central channel to progress toward the center. This can be explained that the CNx film was a little bit larger than that of the sticking underlayer, thus some parts of the CNx adhered to the glass substrate, which had less adhesion resistance to the CNx. It was evident that increment of applied power led to poorer adhesion quality, this may be due to an increase of the substrate temperature with increasing power [9], and the difference of coefficient of thermal expansion and contraction of the CNx comparted to the sticking underlayer.

Comparing Figure 4.14A, D and E that shared the same power but different gas pressures: 0.4 Pa, 0.6 Pa and 0.8 Pa respectively, it was clearly seen that the CNx films in Figure 4.14D and E detached totally, except the portions left on the gate electrodes. It revealed that an increment of pressure hindered a good adhesion between the CNx and the sticking underlayer.

Thickness (nm)	200W	220W	240W
0.4 Pa	100	120	140
0.6 Pa	110		
0.8 Pa	120		

Table 5: Measurement comparison of the CNx film thickness with different deposition conditions.

Measurements of the CNx film thickness for each sample were also effectuated, which was shown in Table 5. The going up of power and gas pressure increases the CNx film thickness.

In this section, the CNx films under various deposition conditions of RF power and gas pressure were deposited on SiC sticking underlayer by using RF magnetron sputtering method. Based on the Experiment 1.3, the optimal deposition conditions of CNx film regarding to RF power and gas pressure were 200W and 0.4 Pa, respectively. It can be seen that the CNx adhesion resistance was much affected by changes in sputtering power. An increment in power and pressure caused a degradation of CNx thin layer. However, properties of CNx film not only depended on sputtering power and gas pressure, but also related to other parameters such as N/C ratio, target to substrate distance, the nature of the target and the substrate, even the cleanliness of the vacuum chamber. To fully understand the relation between the deposition parameters and the final CNx properties, all of these parameters need to be investigated. Besides, only three sets of power and pressure were not enough to explain those effects, further study with a series numbers should be completed. Last but not least, AFM and SEM could be employed to observe roughness and particle morphology and size of CNx film under different deposition conditions, X-ray photoelectron spectroscopy (XPS) and Auger electron spectroscopy could be applied to analyze chemical composition of CNx, infrared spectroscopy could be used to study chemical bonding inside CNx, even nanoindentation system could reveal the studying of CNx mechanical properties [10, 11].

4.2.5. Experiment 1.4: Adhering Investigation by Introducing Post-annealing after CNx Deposition Residual stress often exists inside thin film after deposition, normally, the stress relief is a thermomechanical process. However, the reaction rate is quite slow at room temperature. In order to accelerate this release, an annealing process is introduced. In metallurgy and materials engineering, annealing is a heat treatment process that not only changes the microstructure of a material and

thereby changes mechanical properties such as hardness and ductility, but also eliminates residual stress, reduces deformation and crack tendency, uniforms material structure and composition, as well as minimizes interfacial reactions between film and its substrate for a better adhesion [12-14].

Four chemical clean 2-inch glass substrates were prepared for thin layer deposition. Two had only one layer of 100 nm CNx deposited directly on substrate, while other two had a sticking underlayer of 20 nm SiC deposited before CNx. After depositions, I took one sample of each set for an annealing of one hour at 450°C. Then all of them were put in aqueous environment (deionized water) to observe their adhesion aging.



Figure 4.15: Micrographs (A, B, C) and photograph (D) of post-annealing control experiments. (A)-CNx deposited onto SiC without post-annealing, five days after in deionized water. (B)- CNx deposited onto SiC with one-hour post-annealing at 450°C, one day after in deionized water. (C)- CNx deposited onto glass substrate without post-annealing, one day after in deionized water. (D)- CNx deposited onto glass substrate with one-hour post-annealing at 450°C, the photography was taken right after the immersion in deionized water.

Figure 4.15 shows the adhesion aging results without post-annealing (A and C) and with annealing (B and D). Figure 4.15A and B represent deposited CNx onto a SiC sticking underlayer. Without annealing and after five days in deionized water, several individual detaching grains appeared in CNx film (A). However, after one-hour annealing at 450°C and only one day in deionized water, the detaching grains grew up and clustered (B). The cracks observed in the film may be due to the difference of coefficient of thermal expansion and contraction of CNx and substrate. Those little black spots in Figure 4.15B also shows that a lot of detachments in the film were happening. Curiously it is found that post-annealing did not make adhesion better but worse. The glass transition temperature of the glass substrate is

below the room temperature and the glass is probably relaxing too much and this molecular motion is probably responsible for the poor adhesion of the thin film. The same phenomenon can also be seen in Figure 4.15C and D. Both represent CNx deposited directly onto glass substrate, in which Figure 4.15C shows the behavior of CNx just one day in deionized water without doing annealing. Compared to Figure 4.15A, the detaching grains were bigger and heavier that once again confirms how important is the sticking underlayer. However, with a post-annealing and without sticking underlayer, the CNx film cannot bear in deionized water for even a moment, it detached as soon as it hit the water, no CNx left at all (see Figure 4.15D).

The post-annealing temperature for CNx is set to be 450°C for the first test. In fact, we did not know the adequate temperature for CNx, 450°C was only appropriate for SiC. Based on the Experiment 1.4, a post-annealing of 450°C did not improve the adhesion quality but it was worse. However, we did not know if it was because this CNx material has a relaxing temperature far away from 450°C. To further clarify the effect of annealing on CNx, a series numbers of temperature should be set along with observations of morphology by SEM and AFM, as well as measurements of residual stress and strain distribution in CNx film [13, 15].

4.2.6. Experiment 1.5: Sheet Resistance Measurements of CNx by 4-point Probes Method

Sheet resistance is a measure of film resistance with a uniform thin (normally <1 μ m) thickness. Fourpoint probes method is mainly used for accurate measurement of resistance value by avoiding contact resistance, however it could also be used in sheet resistance measurement [16, 17]. In a regular threedimensional conductor, it is acknowledged that the resistance can be described as:

$$R = \rho \frac{L}{A} = \rho \frac{L}{Wt}$$
(4-1)

where R is the resistance (in Ω), ρ is the resistivity (in $\Omega \cdot m$), L is the length of film (in m), A is the crosssectional area (in m²) of film and can be split into the width W (in m) and the sheet thickness t (in m). If we combine the resistivity with the thickness, Formula 4-1 can then be written as:

$$R = \frac{\rho}{t} \frac{L}{W} = R_s \frac{L}{W}$$
(4-2)

where R_s is the sheet resistance, which can also be described as:

$$R_s = \frac{\rho}{t} \tag{4-3}$$

According to Formula 4-3, the unit of sheet resistance should be ohms (Ω), however, its common unit is "ohms per square" (denoted as Ω/\Box). This is exclusively used for sheet resistance that considers film as a two-dimensional system, which is equivalent to the concept of resistivity used in three-dimensional system.

In Experiment 1.5, three sets of measurement of sheet resistance were effectuated by 4-point probes method. Three chemically clean glass substrates were first used to deposit a 20 nm rectangle SiC thin film, and the measurements of sheet resistance of SiC film of three samples were recorded. Then all the samples received a 100 nm CNx thin film, which has the exact same shape and size as the first SiC film, and a second measurement of CNx sheet resistance of three samples was done. After two days placed in air, or in deionized water, or in 10⁻³M KCl solution, respectively, a third measurement of CNx sheet resistance of each sample was effectuated. The experiment gave a comparison to see how sheet

resistance of CNx changed over time and how different environments influenced on this parameter. Noted that all the measurements were carried out at clean-room temperature to avoid any temperature influence. Table 6 gives a summary of the measurement results.

Sheet resistance (MΩ)	In air	In deionized water	In KCl solution
SiC	1.085*10 ³	1.107*10 ³	1.157*10 ³
CNx	20.377	16.474	30.897
CNx after 2 days in different environments	24.525	22.562	52.272

Table 6: Summary of sheet resistance measurements of CNx film.

The sheet resistance of SiC film was really great and ranged from $1 \text{ G}\Omega$ to $1.2 \text{ G}\Omega$ that explained exactly the insulating status of SiC. Whereas the results of CNx film varied a lot, from 16 M Ω to 30 M Ω . The reason may come from operational deviation. Even though the deviations existed, the third set of measurement still reflected the environmental evolution of the assembly. After two days in air, the sheet resistance of CNx increased 17%, this may be explained by detachments of CNx film. Similarly, the one in deionized water led to even bigger increase, which reached to 27%, accompanying with an even worse deformation of film. Compared to the first two samples, the third one in KCl solution had the worst situation and the greater increment of resistance, reaching to 41%. Therefore, we may say: the changing of CNx sheet resistance was directly correlated to film degradation.

4.2.7. Experiment 1.6: First Measurement of EOF and Polarizability Window

In Experiment 1.6, a completely fabricated dry film based microdevice (as shown in Figure 3.6F of Section 3.2.3) was connected to the experimental bench and had a first EOF measurement. The two former followers (as shown in Figure 3.8B of Section 3.3.1) were replaced by the designed and fabricated electronic card (as shown in Figure 2.10 of Section 2.3.2). Later, a measurement of the polarizability window was performed on a Metrohm Autolab instrument potentiostat-galvanostat.



Figure 4.16: Relative EOF measurement curve under function of gate voltage in 10⁻³M KCl electrolyte.

Figure 4.16 shows the first measurement of EOF modulation with the integrated polarizable CNx gate in an asymmetric PI-FFET microfluidic device. The measurement was performed under fluid pressure of 300 mbar, electrophoretic voltage of 20V and aqueous KCI solution concentration of 10^{-3} M. The relative EOF flow curve was coming from the measurement of the relative velocity of the fluorescent beads in unit of pixel/s, and modulated under function of gate voltage (V_{gate}) with Δ V ranging from -1V to +1V. Because of degradations of CNx thin layer in liquid electrolyte, only one cycle of measurements was successfully carried out.



Figure. 4.17: Polarizability window of CNx film deposited onto SiC sticking underlayer.

Figure 4.17 presents the polarizability window of CNx film deposited onto SiC sticking underlayer (see architecture of Figure 3.2). It can be seen that all the curves are asymmetric, this is due to the different nature of electrochemical reactions that occur at the anode and cathode. The limit of the polarizability window at the anode is the oxidation of Cl^- ions, *i.e.* release of Cl_2 gases. While the limitation at the cathode is the reduction of water, *i.e.* release of H_2 gases. The chemical reaction equations can be expressed as follow:

$$2KCl + 2H_2O \rightarrow 2KOH + H_2 \uparrow + Cl_2 \uparrow$$
 (Equation 4-1)

$$2Cl^{-} - 2e^{-} = Cl_2 \uparrow \qquad (Equation 4-2)$$

$$2H^+ + 2e^- = H_2 \uparrow$$
 (Equation 4-3)

where Equation 4-1 represents the total reaction, Equation 4-2 represents the oxidation, Equation 4-3 represents the reduction. It can also be seen that the concentration of KCl solution is smaller, the window is broader.



Figure 4.18: SEM micrographs of the CNx film deposited onto SiC film. (A)- Adhered area. (B)-Detached area. (C)- Interface between two areas.

The adhesion ability of the SiC sticking underlayer is too weak and CNx can only remain a little time in KCl electrolyte. However, interestingly it was found that even in detached area of CNx film (see Figure 4.18B), those grains of CNx were compact to each other. We did not observe evident crack on the detached sheet compared to well stuck area (see Figure 4.18A). Figure 4.18C shows the interface between the stuck and detached areas. It can be seen that such a detachment did not influence the continuity of CNx film itself, which was also reflected in Figure 4.13F.

Table 7: EDS analyzed chemical composition of good and degraded areas of CNx film.

Mass proportion (%)	С	N	0
Good area	48.12	6.67	48.14
Degraded area	46.75	41.13	12.12

To further understand the chemical composition of the good area and degraded area of CNx, an energy-dispersive X-ray spectroscopy (EDS) analysis was employed. A selected good status area had a composition of 48.12% of C, 6.67% of N and 48.14% of O, whereas a degraded area had 46.75% of C, 41.13% of N and 12.12% of O (see Table 7). The proportion of C did not change a lot. However, the concentration of N increased greatly in bad area while the one of O reduced a lot. Well, it is still hard to say if there was a direct correlation between the measured concentration and the adhesion quality since oxygen can leave the thin CNx layer as a consequence of the detachment.

4.2.8. Conclusions

In Experiment 1 we studied the behavior of CNx film deposited onto a SiC sticking underlayer. To have a better adhesion, the fabrication process should be: 20s piranha etching before deposition of CNx, 200W and 0.4Pa for the deposition parameters, no post-annealing after the deposition. We also realized the first measurement of EOF that was stopped due to current leakages. The polarizability window limited for CNx onto SiC. Thus, to have a long-term adhesion, we proposed another material that will be presented in the following section.

4.3. Experiment 2: Choice of Metallic Pt as Sticking Underlayer

4.3.1. Aims of Experiment 2

The primary aim of Experiment 2 was to look for other materials that could work as the sticking underlayer to place CNx film onto glass substrate. Such a material should have the following capability: it can stick to both glass substrate and CNx film in a robust way (liquid and air aging tests at least for three days). Thus, all common materials used for microfabrication will be tested. They can be classified into two classes: the dielectrics and the metals. At the end, we will explain why we chose Pt as the sticking underlayer.

4.3.2. Experiment 2.1: Amazing Adhering Aging of Pt as Sticking Underlayer

Testing of Dielectric Materials

Six different dielectric materials have been tested in both air and KCl solution. They were: SiC, Si₃N₄, Al₂O₃, TiO₂, ZnO, and MgO. The first two materials have already been detailed in Section 4.2.2. The three middle materials of the list are transparent when deposited in very thin film. A pre-deposition of SiC film (20 nm) was employed to have a reference. The last one: MgO had a pre-deposition of Nb film (20 nm). All of the materials were deposited to target a thickness about 20 nm. The final CNx film was 110 nm thick. At last, TiO₂ was used to replace SiC sticking underlayer (see more details in Section 4.2.7), and have been used to measure polarizability windows.

Behaviors Materials	Aging in air (after three months)	Degradation micrographs
Si₃N₄		
SiC		

Table 8: Behaviors of CNx film deposited onto different dielectric materials in air.



Table 9: Behaviors of CNx film deposited onto different dielectric materials in 10⁻³M KCl solution.

Behaviors Materials	Aging in KCl	Degradation micrographs
ZnO	Lasting one hour	
SiC/ZnO	Lasting one day	



Table 8 and Table 9 show CNx film deposited on different dielectric materials. In Table 8, those materials had generally bad adhesion with CNx. They cannot last even in air. The pictures show the behavior after three months, when the degradation has already begun. For example, Al₂O₃ started its delamination on the 23rd day. The materials in Table 9 show a long-lasting time (more than three months) in air. Unfortunately, all of them cannot last in KCl solution more than one day.



Figure 4.19: Polarizability window of CNx film deposited onto TiO₂ sticking underlayer.

A measurement of polarizability window of CNx film deposited onto TiO₂ sticking underlayer was performed, as shown in Figure 4.19. Compared to that based on SiC (Section 4.2.7), this one is more symmetric and has a larger polarizability window.

Testing of Metallic Materials

Nine different metals were tested in air or KCl solution: Al, Cr, Nb, Ni, Pd, Ti, Ag, Au, and Ge. The last three metals of this list needed a 5 nm layer of Ti because they cannot stick directly to the glass. All of them were deposited with a 20 nm thickness prior to the final 110 nm CNx deposition.

Behaviors Materials	Aging in air (after three months)	Degradation micrographs
AI		, 2011,

Table	10: Behaviors	of CNx film de	posited onto	different	metals in air.
		••••••			



Similar to Table 8, the metals in Table 10 cannot remain stable in air. Photographs show their status after three months. For both Al and Au, the degradation begun on the 20th day, while the situation was better for Ti and Nb.

Behaviors Materials	Aging in KCl	Degradation micrographs
Ti/Ge	Detaching at once	
Pd	Detaching at once	
Ti/Ag	Lasting one day	_ <u>20 m</u>
Ni	Lasting three days	

Table 11: Behaviors of CNx film deposited onto different metals in 10^{-3} M KCl solution.

Cr	Long lasting	
Ti/Pt	Long lasting	

Table 11 presents only the metals which have already passed the three-month air aging. For both Ge and Pd, once touched by KCl solution, they instantly degraded. The Ge underlayer remained onto the glass substrate, but not the Pd one. We cannot assert that Pd had bad adhesion to CNx, maybe by itself it just cannot stick to glass in aqueous environment. A SEM micrograph also reflected one of the degradations on the surface. Ag and Ni were better than the former materials. A few degradations appeared just one day after in KCl for Ag; and the same situation was observed for Ni after three days in liquid. At the end, the only two materials that could stay steady in air and in liquid electrolyte were Cr and Pt.

A lot of materials have been tested in air and in KCl solution before being considered to be the underlayer part of the flow FET. It seems that the dielectrics are worse than the metals. Among the tested metals, only Cr and Pt have no adhesion issue with CNx. First, we refused to have any conducting material as a sticking layer to avoid the risk of short-cut and faradic loss in the fluidic component. However, after 6 months in air and another 2 months in KCl solution, the CNx still stuck well to Pt. To further understand qualitatively and quantitatively, a series of analyses was performed in the next section.

4.3.3. Experiment 2.2: Analyses of CNx Deposited onto Pt Sticking Underlayer

In Experiment 2.2, a cross configuration was designed to investigate the behavior of CNx deposited onto a Pt sticking underlayer.



Figure 4.20: Top view of the fabrication processes of the cross thin layered Sample 3. 1- The cleaning process. 2- The 5/25 nm Ti/Pt physical vapor deposition. 3- The 20 nm CNx sputtering deposition. 4-Optical micrograph of the fabricated device.

Sample 3 was fabricated based on a 2-inch glass substrate (see Figure 4.20). Two depositions were effectuated on one glass wafer to have a good comparison: first one was a 5/25 nm Ti/Pt film deposition on glass (black rectangle in Figure 4.20-2); second one was a perpendicular 20 nm CNx film deposition over it (tan rectangle in Figure 4.20-3), forming a cross configuration as shown in Figure 4.20-4.





Figure 4.21: 1 μm by 1 μm AFM topography (left) and AFM phase (right) images of Pt area (A) and CNx onto Pt area (B).

Figure 4.21 displays representative images of topography and phase of a CNx film deposited onto Pt. Each measurement presented topography and phase image simultaneously. Figure 4.21A shows the area marked as "a" (see Figure 4.20-3), which was a bare Pt film onto Ti. Figure 4.21B shows the area "b" (see Figure 4.20-3), where CNx was deposited onto Pt. Both of the topographies (left-hand) present the homogenous hard grain cores surrounded by soft peripheries. And both of the phase images (right-hand) follow this morphology. If we compared Figure 4.21A to Figure 4.5B (SiC onto glass) and Figure 4.5D (Si₃N₄ onto glass), it can be seen that, the grains of Pt film are smaller and much homogenous. Similarly, CNx onto Pt appeared much uniform than that in Figure 4.5C (CNx onto SiC) and Figure 4.5E (CNx onto Si₃N₄). The root mean square roughness of Pt film was measured to be 0.462 nm. It was much smaller than the roughness of SiC surface without piranha treatment (as shown in Table 3). To conclude, Pt film drastically enhances CNx film adhesion onto glass substrate and the surface exhibits a low roughness.



Figure 4.22: Tilted SEM micrographs of the CNx/Pt interface.

SEM observations have also been done to study the interface between CNx and Pt film. In parallel an EDS analysis of chemical composition of different areas has also been carried out. Figure 4.22 shows two SEM images of the interface between CNx and Pt films.

Mass proportion (%)	С	Ν	0	Na	Si	Ti	Pt
Pt onto Ti-glass substrate area	0	0	24.77	0	13.54	2.37	59.32
CNx onto glass substrate area	8.9	8.37	55.75	0	26.98	0	0
CNx onto Pt area	7.71	3.27	24.51	2.55	11.17	0	50.78

Table 12: EDS analyzed chemical composition of three different areas of Sample 3.

Three EDS analyses were performed on these areas: Pt onto Ti and glass substrate, CNx onto glass substrate, and CNx onto Pt. The results were shown in Table 12. Since the effective depth of detection by EDS is in the range of hundreds of nanometers to a few micrometers, and for our sample the maximal thickness was around 40 nm, thus, it came up with such a result: in the area of Pt onto Ti and glass substrate, Pt was the most composed element, meanwhile titanium, oxygen and silicon were also detected because of the Ti and glass substrate. As the same reason, only carbon, nitrogen, oxygen and silicon were measured in the area of CNx onto glass substrate. However, in the area that CNx was deposited onto Pt, sodium was also detected. To explain, there are two possible reasons, either sodium took place of titanium (for same reason, the analysis confused these two elements); or the analyzed area was contaminated by sodium during the clean room process. Besides, the proportion of carbon was only around 8%, for a carbon doped nitrogen film, it was really strange.





Figure 4.23: XPS analyzed curves of carbon 1s, nitrogen 1s, and oxygen 1s respectively.

X-ray photoelectron spectroscopy (XPS) was employed to precisely analyze the composition of CNx onto Pt since it is a surface chemical analysis technique. XPS measures the kinetic energy and number of electrons escaping from 1 nm to 10 nm below the surface of the illuminated material by X-rays. Five different areas of CNx deposited onto Pt have been analyzed by XPS, the results were shown in Figure 4.23. All the four detected area had an atomic proportion of each element being 9% of oxygen, 31% of nitrogen, and 60% of carbon, except one area had a little difference being 8% of oxygen, 32% of nitrogen and the same proportion of carbon. It was obvious that carbon was the most concentrated element in CNx film and the ratio of nitrogen to as-deposited material was around 30%, which was higher than what we wanted. Indeed, we know that the 14.9% that makes $CN_{14.9\%}$ behave like a dielectric and also exhibit a large polarizable window (over ±3V). The undesirable C/N ratio going together with the appearance of oxygen may be due to the contaminated chamber and/or target of the deposition machine. This high concentration in nitrogen is disturbing since it may affect the adhesion between SiC underlayer and CNx film. Besides, the small polarizable window and the dielectric property for such a rich nitrogen CNx is not suitable to fabricate a transistor.

4.3.4. Conclusions

The Experiment 2 showed a remarkable adhesion ability of sticking underlayer Pt. As we can see from Figure 3.2-10 in Section 3.2.1, if Pt replaces SiC as the underlayer, it will short-cut the two gate electrodes. To avoid this problem, two novel transistor architectures will be presented in the next section.

4.4. Experiment 3: New Role of CNx — An Insulating Layer

4.4.1. Aims of Experiment 3

The primary aim of Experiment 3 was to solve the contact problem between Pt sticking underlayer and gate electrodes. Thus, two architectures were designed: the first one has only one layer of CNx that is sandwiched between the underlayer and the electrodes; the second one has two CNx layers, one plays as an insulating layer another plays as a polarizable layer. In this section, both of them will be investigated successively.

4.4.2. Experiment 3.1: Isolation and Polarization Together in One-Layer CNx

In the Experiment 3.1, the CNx film is not only a simple polarizable interface but it is also used as an insulating layer.



Figure 4.24: Cross-sectional fabrication processes of Sample 4. 1- Ti/Pt sticking underlayer deposition. 2- CNx polarizable and isolating layer deposition. 3- Ti/Pt electronic circuit layer deposition. 4- Si₃N₄ isolating layer deposition.

Figure 4.24 shows the fabrication processes of Sample 4. As we can see in step 1, a layer of Ti (5 nm)/Pt (5 nm) replaced the former SiC sticking underlayer. The CNx film (around 130 nm) in step 2 was a little bit larger than the underlayer thus it covered totally the underlayer and thus avoided its contact to the

electrodes on the top (see step 3). The current shortcut between the reference and gate electrodes would also happen because those gate electrodes were exposed to the electrolyte, therefore, another insulating cover was necessary. Here, we used Si_3N_4 material to realize this function, since it is absolutely insulating and optically transparent for a thickness of 40 nm.



Figure 4.25: Figure explaining of the first main problem in the fabrication process of Sample 4. (A)-The profile of configuration. (B)- The inconsistent measured profile (due to an over-etch of CNx because we used the RIE prior to the electrode deposition). (C)- SEM micrograph of the interface between CNx surface and gate electrode. (D)- The expected and measured profile after skipping RIE step.

Sample 4 was never used for EOF measurement or polarizability window testing due to a series of problems during its fabrication. The first main problem was the measured profile being inconsistent with what we expected. Figure 4.25 describes this phenomenon. As we can see, Figure 4.25A shows the profile of configuration, the measurement effectuated by profilometer Dektak® began from flag A to flag B. Theoretically, the measured profile in Figure 4.25B should be the same as Figure 4.25A, which meant following the yellow dash line where the gate electrode located. On the contrary, it went down almost 40 nm instead of going up. It was counterfactual that the relative height of electrode was lower than CNx film. And the only possible reason came from the 60s RIE before electrode deposition. The RIE plasma etched too much CNx. Figure 4.25C confirmed this hypothesis. The black area represented CNx while the white area was Pt. It can be seen that the Pt entered into CNx area, which meant that the CNx had been etched before depositing electrode. Technical data displays that the etching rate of SF₆/O₂ plasma is 35 nm/min, so our hypothesis seems to be the good one. A control experiment was

performed in the same process with the exception of the RIE step just before electrode deposition. At this time, the measured profile shown in Figure 4.25D was definitely corresponding to what it should be. Therefore, the first problem was settled.



Figure 4.26: Optical micrographs of Sample 4 and its second problem. (A)- Top view of central channel and its potential fracture at the edge. (B)- Image of a broken gate electrode. (C)- Image of a continuous gate electrode after a deposition with a tilt of the substrate.

Since a part of gate electrode was deposited on a cliff of 130 nm in height, there was a great possibility that a fracture will happen because of the height difference (see red circles in Figure 4.26A). Actually, it did happen. A resistance measure between two points in Figure 4.26B shows a value of 450 k Ω . For such a good conductor as platinum, without any discontinuity in the conductive circuit, the 450 k Ω value is too high. The solution is to have a tilt during the electrode deposition. Figure 4.26C displays a photograph with a tilt of 20° (between the target and the source). The measured resistance was too small to be read, it means that we finally have a continuous conductive circuit. Thus, the second problem was settled too.

The Experiment 3.1 presented one-layer CNx working as an insulating and polarizable layer at the same time. During the experiment, two major problems have been technically solved. However, when I did those experiments at that time, our laboratory did not have such machine that could deposit with a tilt. So, I had to go to another laboratory to use their machine. The cost and loss of time were so high that I decided to try another configuration. This ultimate configuration has a two-layer CNx structure, as described below.

4.4.3. Experiment 3.2: Isolation and Polarization Separated in Two-Layer CNx

In Experiment 3.2, a new configuration was designed to have two layers of CNx, one functioned as an insulating layer and another worked for polarization. Measurements of polarizability window and EOF with this configuration have also been done.



Figure 4.27: Cross-sectional view of fabrication processes of Sample 5. 1- Ti/Pt sticking underlayer deposition. 2- The first deposition of CNx layer for isolation. 3- Ti/Pt electronic circuit layer deposition. 4- The second deposition of CNx layer for polarization.

The fabrication process of Sample 5 was described in Figure 4.27. Compared to the fabrication process of Sample 4, there was no big difference except the first deposition of fine CNx film (about 20 nm) played as an insulating layer. The electrodes were deposited onto it. The second CNx film was much thicker than the first one, reaching about 120 nm.




Figure 4.28: Major reasons that blocked EOF measurement. (A)- Detachment of the CNx underlayer contacting to glass substrate. (B)- Break of the gate electrode at the edge of the central channel. (C)-Detaching progress of the CNx polarizable layer. (D)- Formation of bubble due to the electrochemical reactions.

EOF and polarizability window measurements were performed on Sample 5. However, the experiments cannot remain long time because two different aspects. First, the area that the CNx underlayer contacting to glass substrate detached (see arrows in Figure 4.28A), this problem led to two major consequences: the gate electrode broke at the edge of central channel (see arrow in Figure 4.28B); the current leakage occurred between Pt underlayer and reference electrodes that will cause Joule effect and further degrade this CNx underlayer. Second, the polarizable CNx layer on the top detached as time goes by (see Figure 4.28C). This one led to the current leakage between reference and gate electrodes that will excite the electrochemical reaction and produce bubble formation (see Figure 4.28D), in the end, it will cause further degradation of the CNx polarizable interface.



Figure 4.29: Polarizability window of Sample 5.

Figure 4.29 shows the polarizability window of this architecture. The concentration of KCl solution was 10^{-2} M. It confirmed that the CNx interface could nearly polarize within a range of -1V/+1V.

4.4.4. Conclusions

Two architectures were designed and tested to avoid any unwanted electric contact between Pt sticking underlayer and the gate electrodes, where a CNx thin layer also worked as an insulating one. Experiment 3 showed that the two-layer CNx architecture provided a large polarizability window. However, as long as the contact between CNx and glass exists, the delamination of CNx film would never stop. For this reason, a new configuration will be presented in the next section.

4.5. Experiment 4: Innovative Configuration Avoiding Any Unwanted Electric Contact and CNx Detachment

4.5.1. Aims of Experiment 4

An innovative configuration was designed to avoid any unwanted electric contact as mentioned-above in Section 4.4. Owing to the success of Pt underlayer and the resulted good robustness of the thin layer assembly, we will keep using Pt. In Experiment 4, we will present a feasible, practical and reproducible fabrication and characterization pathway. Two materials were used for the testing: Si₃N₄ as an absolute insulating, and SiC that is a relative insulating material.



4.5.2. Experiment 4.1: Employment of Absolutely Insulating Si₃N₄ Material

Figure 4.30: Cross-sectional view of the fabrication process of Sample 6. 1- Ti/Pt sticking underlayer deposition. 2- Insulating bars deposition. 3- Insulating circuit layer deposition. 4- Ti/Pt electronic circuit layer deposition. 5- CNx polarizable layer deposition. 6- "Bars on top" configuration.

Figure 4.30 presents the fabrication process of Sample 6. The first step was always the deposition of 5/10 nm Ti/Pt sticking underlayer. While the two little insulating bars in the second step was a new structure, its aim was to avoid the contact between the underlayer and the conducting liquid electrolyte. These two bars were designed to be only 10 μ m in width because that was the exact

distance between the edge of reference electrode and the border of underlayer. That meant it would be better to deposit half of bar on the central channel and another half on the glass substrate, and this could be realized by the SUSS MicroTec MJB4 aligner. The thickness of bars was 20 nm. Here, we chose Si_3N_4 material, whereas in the Experiment 4.2 it would be replaced by SiC. During the fabrication, we tried two different orders in the process of deposition: either as shown in Figure 4.30, the deposition was done just after underlayer deposition, we call them "bars underneath". The other pathway was: the bars deposition was carried out during the last step, after CNx layer deposition, we call them "bars on top". In this section, we will discuss about both situations. The third step was the deposition of another insulating layer, this layer shared the same configuration of the electronic circuit (same mask). Its function was to avoid the contact between the underlayer and the gate electrodes. Its thickness was around 20 nm. Just after the insulating layer deposition, the electronic circuit deposition was done. The last step was the deposition of the CNx layer. The last figure shows the situation that the bars were deposited at the end.

Here, we introduce "bars on top" first.



Figure 4.31: Optical micrographs of Si₃N₄-based insulating "bars on top". (A)- Top view of the right entrance of the central channel of the Wheatstone bridge before connecting the electronic source meter units. (B)- After a polarization attempt in 10⁻³M KCl solution.

The insulating bars were deposited after CNx deposition with a 29 nm thickness (see Figure 4.31A). Half of the bar was on the CNx layer and another half was on the glass with a height difference of 120 nm. Such structure was very fragile, especially in the liquid electrolyte. Figure 4.31B confirmed this thought, once the device was connected to electronic instrumentation and immersed in KCl solution, the bar on the top was destroyed. The only remaining insulating part was directly on the glass. More disturbing was that the CNx layer and the Si₃N₄/Pt gate electrode also detached. This phenomenon is a combination of several reasons: First, because the charge permeability of the fragile insulating bars was too high, electrolyte ions penetrated into the structure continuously. These leaking currents led to a shortcut between electrodes and the conductive Pt underlayer. This mess was a result of the charge permeation into solid state insulators and the poor adhesion between CNx and Si₃N₄; Third, the Joule effect caused by shortcut aggravated this degradation; Fourth, potential applied to the gate electrode (-2V to +2V) was larger than its tolerance (-1V to +1V) and reduction-oxidation reactions took place.

Now we will talk about "bars underneath".



Figure 4.32: Optical micrographs of Si_3N_4 -based insulating "bars underneath" and its voltammogram. (A)- Deposition of two bars just after the lift-off of the sticking underlayer. (B)- Top view of the left entrance of the central channel of the Wheatstone bridge. (C)- Measured result of polarizability window in $10^{-3}M$ KCl solution (the measured surface area is $6.0275*10^{-3}$ cm²).

Figure 4.32A shows the deposition of insulating bars onto the underlayer. Figure 4.32B shows the final microfabricated central channel. Compared to the structure "bars on top", this one was much firmer since there was a smaller height difference. Moreover, the contact area between CNx and Si₃N₄ was reduced. A measurement of polarizability window is presented in Figure 4.32C with 10^{-3} M KCl solution. The voltammogram shows a large and symmetric window of polarizability (from -1.5V to +1.5V). However, working with the Si₃N₄ was also limited, since the same situation happened as mentioned for "bars on top".

The Experiment 4.1 presented an innovative architecture: the gate electrodes are buried and the CNx layer should not detach because it is directly onto the Pt sticking underlayer. However, the Si_3N_4 insulating caps were permeable to the charge and let current leakage took place and destroyed the component. Thus, in the next section, we will introduce SiC to replace Si_3N_4 .

4.5.3. Experiment 4.2: Employment of Relatively Insulating SiC Material

In the Experiment 4.2, we will come back to SiC material, this material was disappointing as an intermediate sticking layer in Section 4.2. Here, we are eager for evaluating its insulating capacity.



Figure 4.33: Optical micrographs of SiC-based insulating "bars on top". (A)- Top view of the right entrance of the central channel of the Wheatstone bridge. (B)- Bubbles formation during the EOF measurement in 10⁻³M KCl solution.

In the case of "bars on top", the device also encountered current leakage phenomenon. In Figure 4.33A, the area on the top of central channel has already begun to detach. Once again, the charge permeation of the bars was too high to avoid the shortcut (see Figure 4.33B). The device was used for EOF measurement in 10⁻³M KCl solution, however the experiment was forced to stop because of bubble generation.





Figure 4.34: Micrographs of SiC-based insulating "bars underneath" before (A) and after (B) experiment, and the voltammetry results of polarizability window (C).

On the contrary, the "bars underneath" configuration based on SiC insulating caps was much better. The bar (marked in red rectangle) was deposited and sandwiched very well between underlayer and CNx film before experiment (see Figure 4.34A). The bar remained even after the end of the experiment (see Figure 4.34B), a whole day lasting in liquid electrolyte. However, the measurement results of polarizability window (see Figure 4.34C) was not quite large as that in Figure 4.32C.

4.5.4. Conclusions

The novel design of Experiment 4 is mainly reflected in two aspects: first, by adding an insulating layer under the electronic circuit layer, the undesirable current leakages and shortcut are avoided. Besides, the CNx film has no need to play as insulating and to be larger than the sticking underlayer. In other words, it shares the same size as the latter that avoids to touch the glass substrate, reducing adhesion issues; Second, by adding an extra pair of bars at the extremity of the central channel, the unwanted shortcut between the two extremities of the transistor is also stop. Under the scenario, we have tried two materials with two different process orders for the deposition of bars: "bars underneath" worked better than "bars on top"; CNx on SiC was better than on Si₃N₄. The architecture based on Si₃N₄ has a larger window of polarizability than that on SiC. Such a result cannot satisfy our curiosity: is there a material that could better realize the function of the bars and provide a large range of polarizability window at the same time? Is there any chemical modification of the CNx during the microfabrication process? Driven by this thought, our attention is turned to those photoresists as potential insulators. Therefore, in Annex A, an investigation based on the integration of photosensitive resin will be presented.

4.6. Conclusions

Firstly, we investigated CNx polarizable layer deposited onto a SiC sticking underlayer. After some improvements, we finally got the first measurement of EOF. Meanwhile, this architecture presented an asymmetric and narrow polarizability window. Secondly, we tested CNx deposited onto Pt sticking underlayer. The good point was that after several months in KCl solution, the CNx film still adhered firmly onto the glass. To avoid any electric shortcut through this metallic underlayer, we designed and fabricated a series of samples. The last challenge in the flow FET fabrication was to introduce two insulating bars at both extremities of this Pt conductive underlayer. And we gave a pathway to have a robust component architecture. The integration of polymers as the two insulating bars will be detailed in Annex.

REFERENCES:

- [1] "Silicon carbide," <u>https://en.wikipedia.org/wiki/Silicon_carbide</u>.
- [2] J. B. Casady and R. W. Johnson, "Status of silicon carbide (SiC) as a wide-bandgap semiconductor for high-temperature applications: a review," *Solid State Electron*, vol. 39, pp. 1409-1422, 1996.
- [3] P. Eaton and P. West, "Atomic force microscopy," Oxford university press, Oxford, UK, 2010.
- [4] J. Tamayo and R. Garcia, "Deformation, contact time, and phase contrast in tapping mode scanning force microscopy," *Langmuir*, vol. 12, pp. 4430-4435, 1996.
- [5] S. N. Magonov and D. H. Reneker, "Characterization of polymer surfaces with atomic force microscopy," *Annu. Rev. Mater. Sci.*, vol. 27, pp. 175-222, 1997.
- [6] K. D. O'Neil and O. A. Semenikhin, "AFM phase imaging of electropolymerized polybithiophene films at different stages of their growth," *J. Phys. Chem. C*, vol. 111, pp. 14823-14832, 2007.
- [7] J. C. Byers, P. Tamiasso-Martinhon, C. Deslouis, A. Pailleret, and O. A. Semenikhin, "Atomic force microscopy studies of carbon nitride (CNx) films deposited on a conducting polymer substrate," J. Phys. Chem. C, vol. 114, pp. 18474-18480, 2010.
- [8] M. Holmes, J. Keeley, K. Hurd, H. Schmidt, and A. Hawkins, "Optimized piranha etching process for SU8-based MEMS and MOEMS construction," J. Micromech. Microeng., vol. 20, pp. 115008-115016, 2010.
- [9] H. Kakati, A. R. Pal, H. Bailung, and J. Chutia, "The influence of RF power and gas pressure on the surface characteristics of aluminium oxide deposited by RF magnetron sputtering plasma," *J. Phys. Conf. Ser.*, vol. 208, pp. 012102-012106, 2010.
- [10] A. Chaoumead, Y-M. Sung, and D-J. Kwak, "The effects of RF sputtering power and gas pressure on structural and electrical properties of ITiO thin film," *Adv. Cond. Matter Phys.*, vol. 2012, 2012.

- [11] D. Li, S. Lopez, Y. W. Chung, M. S. Wong, and W. D. Sproul, "Ionized magnetron sputter deposition of amorphous carbon nitride thin films," J. Vac. Sci. Technol. A, vol. 13, pp. 1063-1066, 1995.
- [12] P. Yang, S. C. H. Kwok, R. K. Y. Fu, Y. X. Leng, J. Wang, G. J. Wan, N. Huang, Y. Leng, P. K. Chu, "Structure and properties of annealed amorphous hydrogenated carbon (a-C:H) films for biomedical applications," *Surf. Coat. Technol.*, pp. 747-751, 2004.
- [13] Y. Fu, H. Du, S. Zhang, and Y. Gu, "Stress and surface morphology of TiNiCu thin films: effect of annealing temperature," *Surf. Coat. Technol.*, vol. 198, pp. 389-394, 2005.
- [14] V. Kulikovsky, V. Vorlicek, R. Ctvrtlik, P. Bohac, L. Jastrabik, and H. Lapsanska, "Effect of air annealing on mechanical properties and structure of amorphous B₄C films," *Surf. Coat. Technol.*, vol. 205, pp. 4052-4057, 2011.
- [15] H. F. Poulsen, J. A. Wert, J. Neuefeind, V. Honkimaki, and M. Daymond, "Measuring strain distributions in amorphous materials," *Nat. Mater.*, vol. 4, pp. 33-36, 2005.
- [16] "Sheet resistance," <u>https://en.wikipedia.org/wiki/Sheet_resistance</u>.
- [17] "Four-terminal sensing," <u>https://en.wikipedia.org/wiki/Four-terminal_sensing</u>.

Chapter 5: General Conclusion and Future Work

Chapter 1 introduced the concept of the capillary electrophoresis. This bibliographic part shows that real-time control by integrating a fluidic transistor in the separation channel is advantageous for high resolution separations. Based on the novel concept of flow field effect transistor (FFET) device made of polarizable interface (PI) in direct contact with the liquid electrolyte, we integrated such transistors in microfluidic Wheatstone bridges (μ FWB) to measure the EOF modulation. CNx was chosen to be the polarizable material. Therefore, the aim of this thesis was to find the most robust microfabricated assembly to integrate CNx thin film onto a microfluidic channel. We had to improve the adhesion of the polarizable interface onto the glass and to protect the gate electrodes from any possible shortcut or faradic loss to avoid the destructive reduction-oxidation reactions. It was the necessary conditions to obtain a robust and functional fluidic component.

Chapter 2 has presented the design, fabrication and experimental validation of a PCB card. It replaced the former two heavy electronic boxes necessary to modulate EOF. This strategy allows us to drastically miniaturize the gate voltage controllers and we should be able to integrate such small electronic card with the fluidic network in order to build hybrid microelectronic/microfluidic device in the near future.

Chapter 3 gave an overview of the whole fabrication process. It included the PI-FFET fabrication, microfluidic channel fabrication, and sealing of the microfluidic chip. The whole automated experimental characterization set-up used for EOF measurement was also described. All the electronic, optic and fluidic instrumentations were presented. This complex instrumental bench includes specific experimental launching procedures with a Matlab program and automated data processing for real time EOF measurements.

Chapter 4 described the core of my experimental work. First of all, we studied CNx films deposited onto SiC sticking layer. After several improvements, the first EOF modulation measurement was obtained. Then we studied CNx deposited onto a Pt underlayer, this metal was selected because it provides a robust adhesion between the CNx and the glass. We designed two architectures of PI-FFET to avoid unwanted faradic exchanges between the conductive Pt underlayer and the PI-FFET electrodes. In the first architecture, CNx was not only the polarizable layer but also the insulating layer. This design prolonged lifetime of device but it was not enough. Thus, a novel hybrid architecture was designed by integrating polymeric insulating pads at the two extremities of the transistor. This design avoided faradic loss in liquid electrolyte as well as faradic current into the electronic circuit of the device.

In summary, this thesis includes a large number of significant studies followed by aging experiments and characterizations. It highlights the possibility to perform an efficient EOF modulation via PI-FFET device during electrophoresis. Unfortunately, PhD work has a limited duration and late we found a way to introduce insulating polymer caps as mentioned-above but this additional step led to CNx surface contamination. Nevertheless, seeking for another photoresist or using RIE as a final step must be evaluated. We also know that several polarization cycles of the interface prior to any separation may improve the CNx surface state, it is another possible outlook. We believe this sticking layer/electrically polarizable/polymeric hybrid architecture will be the most robust existing polarizable transistor for strong and long-term adhesion onto glass substrates. Further chemical characterizations

have to be done at each step of the microfabrication process. We have to protect the CNx layer from any possible contamination that limits the chemical evolution of this crucial interface.

From a personal point of view, this three-year PhD work allowed me to acquire a lot of knowledges and technique skills. Because microfluidic is a multidisciplinary field, it was a real challenge and I hope this important period of scientific career will help me to keep an open mind and vision for my future.









Annex: Investigation of Insulating Photosensitive Resins

Seven photosensitive resins in our lab were chosen to be tested to evaluate their adhesion abilities. They were: positive photoresists AZ 9260, S 1805, S 1828; negative photoresists maN 2405, nLof 2070, SU8 2002; and reversable photoresist AZ 5214. These resins were inherently insulating polymers. The photoresist that was ultimately selected must be available to fulfil three requirements simultaneously before it can be used: adhering firmly to glass, platinum, and CNx. Therefore, the primary process was designed as shown in Figure A1.



Figure A1: Process of Experiment 5 for each photoresist.

Each photoresist must undertake a series of tests. First, it was deposited onto bare glass substrate, one sample was left in the air and the other was immersed inT 10⁻³M KCl solution. If it could bear both situations, then passing to the second step: deposition onto Pt underlayer. The testing repeated in the same way until reaching to the third step. If the photoresist deposited onto CNx could still have good adhesion in both air and KCl solution, then this resin was qualified for our device. In the following experiments, the duration in air and KCl was set to three days.

Testing of Positive Photoresists



Figure A2: Optical micrograph of the testing pattern with different sizes of square.

Three positive photoresists were tested successively with the pattern shown in Figure A2. There are four different sizes of square, among them the largest size is 280 μ m by 280 μ m, while the smallest size is 38 μ m by 38 μ m.



Figure A3: Optical micrographs of AZ 9260 deposited onto glass substrate in both air and KCl solution.
(A)- Picture taken just after development. (B)- Picture taken after three days in air in clean-room environment. (C)- Picture taken after extra three days in 10⁻³M KCl electrolyte in clean-room environment. (D)- Zoom of picture after three days in KCl.

AZ 9260 positive photoresist belongs to AZ[®] 9200 family, which is designed for a higher resolution thick resist requirement [1]. The film thickness and resolution of AZ 9260 product on Si wafer with set program in our lab could reach to 8 μ m and less than 5 μ m respectively. The adhesion ability testing of AZ 9260 was performed on glass substrate, the results are shown in Figure A3. Figure A3-A illustrates a picture of well-done development. And after three days in the air, these patterns still attached firmly to glass (see Figure A3-B). Then we put the sample in 10⁻³M KCl solution. After another three days, as we can see the arrows in Figure A3-C and D, these patterns began to detach from substrate. Due to the behavior of AZ 9260, there was no need to continue on Pt and CNx film.



Figure A4: Optical micrographs of S 1805 deposited onto glass substrate in both air and KCl solution.
(A)- Picture taken just after development. (B)- Picture taken after three days in air in clean-room environment. (C)- Picture taken after just one extra day in 10⁻³M KCl electrolyte in clean-room environment.

Both S 1805 and S 1828 resists belong to the Dow[®] MICROPOSIT[™] S1800[™] G2 positive photoresists series that is employed for advanced IC device fabrication satisfying the microelectronic industries' requirements [2]. The S1800 series have excellent adhesion to Si wafer, but in our case, we tested it on glass substrate. The results shown in Figure A4 presented bad adhesion between these two materials. Figure A4-A shows a good status just after development, however after three days in air, those smaller patterns detached and moved because of air flow, as indicated by the black arrows in Figure A4-B. After another one day in KCl aqueous electrolyte, the whole film of resist degraded (see Figure A4-C). It's obviously that the photoresist S 1805 cannot adhere to glass substrate during microfluidic experiments.

Compared to S 1805, S 1828 had a much thicker film (about 2.4 μ m) under the same spin-coating condition, while the former was 450 nm. Based on the results of S 1805, we introduced "primer" in the following experiments.

Some substrate surfaces, most notable Si and SiO_2 are naturally hydrophilic. Unless this water layer is removed before spin-coating the resist, it will cause delamination of the photosensitive film or etch undercutting. To prevent photoresist delamination during development or wet etching, the hydrophilic surface must be converted to a hydrophobic state, for which we often prime substrate for "dehydration bake" or "soft bake" before spin-coating photoresist. But this is not enough for some resists that badly adhere to some substrates typically SiO₂ and glass, as the adhesion of resists onto different kind of substrates may vary [3]. To solve this issue, applying HMDS becomes a common method to turn the surface in a hydrophobic state [4]. HMDS or called "primer", is one of the bestknown chemical pretreatments for enhancing photoresist adhesion to silicon, glass, quartz and other difficult surfaces [5]. The principle of HMDS work is very simple, the Si atoms of HMDS fragment chemically bond to the O atoms of oxidized surface under heating and accompanied by releasing ammonia (NH₃); the methyl groups (-CH₃) of HMDS then form a hydrophobic surface [6]. Usually, HMDS works as vapor phase, but it is sometimes applied in liquid phase too, as with spin-coating. In this case, the results are often less predictable because having an optimum monolayer of HMDS is difficult [4]. After resist coating and during soft bake, this thick HMDS releases a lot of NH₃ gases, which diffuse into the substrate-near resist and partially crosslink it [6]. As a consequence, the development rate decreases, as well as the resolution, and the resist profile is deteriorated [6]. To reduce this deterioration, it would be better that having a soft bake at 110 to 120°C before resist coating. Another error should be avoided is "over-priming", which means the surface becomes excessively hydrophobic [4]. In this case, the photoresist will not cover the whole surface. Bubbles and voids are generated and trapped at the resist/substrate interface, leading to surface contamination and generation of pattern defects [4]. Primer could improve the adhesion whereas it may also contaminate the surface chemistry of the CNx.



Figure A5: Optical micrographs of **S 1828** deposited onto glass substrate in air and KCl solution successively. (A)- Picture of the sample with primer treatment before spin-coating the resist and after three days in air and another three days in 10⁻³M KCl electrolyte in clean-room environment. (B)-Picture of the sample without primer and just after its development.

Owing to primer employment, the resist S 1828 remained on the glass substrate after three days in air and even another three days in KCl solution, as it was demonstrated in Figure A5-A. However, if we did not use primer, the resist cannot undertake even during development (see Figure A5-B).

Testing of Negative Photoresists

Three negative photoresists were tested successively with the same pattern as shown in Figure A2.



Figure A6: Optical micrographs of **maN 2405** deposited onto glass substrate in air and KCI solution successively. (A)- Picture of the sample without primer and just after its development. (B)- Picture of the sample including primer treatment after three days in air and another three days in 10⁻³M KCI electrolyte in clean-room environment.

The maN 2405 resist belongs to the ma-N 2400 negative photoresist family. It is well suited for electron-beam lithography as it has excellent pattern resolution of downing to 30 nm. And it also has good thermal stability [7]. The maN 2405 is a thin resist, by using our program, its thickness could down to 420 nm. Like S1800[™] series, maN 2405 adhered badly to glass substrate, which can be seen in Figure A6-A. However, by coating a layer of primer, after three days in air and another three days in KCl solution, it still adhered well to glass as seen in Figure A6-B.

The nLof 2070 resists is one of the members in AZ[®] nLOF 2000 negative photoresist series, which are designed for lift-off technique. This kind of resist has some remarkable properties, for example, it has very high thermal stability up to temperature of 250°C and more; it also has high chemical stability against many organic solvents and strong alkaline media; finally, it is electron-beam sensitive that can be applied to e-beam lithography [8]. The thickness of the series varies a lot, in our lab, the nLof 2070 has a thickness of 5 μ m.



Figure A7: Optical micrographs of **nLof 2070** deposited onto glass substrate in both air and KCl solution. (A)- Picture taken just after development. (B)- Picture taken after three days in air in clean-room environment. (C)- Picture taken after another three days in 10⁻³M KCl electrolyte in clean-room environment.

Figure A7-A shows a photograph of developed sample, Figure A7-B shows the status of this sample after three days in air. In both pictures, the resist stuck well to glass. However, after three days in KCl solution, it began to degrade. We see a distortion of the patterns in Figure A7-C. Noted that the resist was negative, so the square patterns were holes.

SU-8 series is an epoxy-based negative photoresist, mainly used in the microfluidics for PDMS replica fabrication [9]. There are several types, here we used SU8 2000. Compared to SU8 3000, the former has much constraint, less viscosity, and less air bubble generation during the spin-coating. In the same series of SU8 2000, there are also different types: SU8 2002, SU8 2005, SU8 2050, and *etc.* These last numbers indicate different thickness of SU8 film. For example, the number "2" in 2002 means the thickness is around 2 to 4 μ m with a classic and defined spin-coating. In this experiment campaigned with SU8 2002, we obtained a film thickness of 1.25 μ m.



Figure A8: Optical micrographs of **SU8 2002** deposited onto glass substrate in both air and KCl solution. (A)- Picture taken just after development of the sample without primer. (B)- Picture taken after development of the sample with primer. (C)- Photograph of large stable grids after three days in air and 10⁻³M KCl electrolyte successively in clean-room environment. (D)- Photograph of narrow spaces in the same condition as (C).

The mask we used was different to the previous one, it was designed by different sizes of squares pattern. Thus, the pattern after development will have different widths of grids (see Figure A8). Similar to the previous resists, SU8 2002 adhered awfully to glass substrate. The behavior of the resist without primer is shown in Figure A8-A. It can be seen that some grid patterns have not been developed enough. On the other side, some others have been over-developed and they started delamination. To improve the adhesion strength, we lithographed the pattern with primer. Figure A8-B presents the resist with a pre-coating of primer, this picture was taken just after development. Most of the patterns were fine, except some of them got rounded borders. Either these parts were over-primed, or they were over-developed. Figure A8-C and D display the resist with primer after three days in air and KCI successively. For the pattern of large grids (C), the resist was in good status. Whereas, for the one of narrow spaces (D), the resist started to degrade.

Testing of Reversable Photoresist AZ 5214 E



Figure A9: Optical micrographs of **AZ 5214 E** deposited onto glass substrate followed by air and KCl solution aging in clean room. (A)- Picture taken just after development. (B)- Picture taken three days after in air. (C)- Picture taken another three days after in 10⁻³M KCl electrolyte.

The AZ[®] 5214 E is a reversable photoresist commonly used for the lift-off, it has been detailed in Section 3.2.1. In this experiment, we wanted to test it in a positive way. The thickness of the resist was about 1 μ m. As this resist was the most commonly used during my thesis work onto glass substrate, I expected that it will have a good adhesion, as shown in Figure A9-A and B. The former shows the case just after development and the latter displays that after three days in air. However, after we put the sample in KCl aqueous solution for another three days, almost all the square patterns detached (see Figure A9-C).

Based on the experiments, there was no photoresist that could undertake in KCl electrolyte without primer. In short, almost all the resists had good adhesion thank to the primer deposition. We chose one of them to be assembled on Pt and CNx. The primer coating and the positive resist S 1828 stuck well to Pt and CNx film in the air even after a three-month aging. The next question is: do the primer indeed contaminate the surface of the CNx polarizable layer? This issue may result in a change of the electroosmotic flow and/or charge permeation at the liquid solid interface. Therefore, a chemical analysis of the CNx after a primer treatment was done by XPS. The result showed a percentage of atom of the primer: 62% of O, 30% of Si, 4% of C, 1.5% of K, 1.4% of Na, 0.5% of Ti, 0.4% of Zn, and 0.2% of N. Further XPS analyses should be performed to compare the chemical compositions with the previous component. Such composition to our knowledges is not suited for large polarizability window. We have

to find a way to fully remove residual traces of primer. This is the only way to introduce resists to build the insulating bars in the component nanofabrication. The final insulating step of the flow FET transistor with polymers could be a success by finishing the fabrication process with a short RIE plasma. It will attack the CNx surface faster than the rest of the component and thus could finally provide a clean CNx interface.

		Positive			Negative			Reversal
Processes	Resists	AZ 9260	S 1805	S 1828	maN 2405	nLof 2070	SU8 2002	AZ 5214 E
Spin- coating	Speed (rpm)	2400	4000	4000	4000	4000	4000	4000
	Acceleration (rpm)	300	2000	2000	2000	2000	2000	2000
	Duration (s)	60	30	30	30	30	30	30
	Thickness	8 µm	450 nm	2.4 µm	420 nm	5 µm	1.25 μm	1.4 µm
1 st annea- ling	Temperature (°C)	110	125	125	90	105	65 then 95	125
	Duration (s)	480	60	60	90	90	60 then 120	90
Expo- sure	Power (mW)	10	10	10	10	10	10	10
	Duration (s)	130	10	70	40	34	15 (without filter)	17
2 nd	Temperature (°C)	Nono	Nono	Nono	Nono	105	65 then 95	None
ling	Duration (s)	None	None	None	None	90	60 then 120	NUTE
Develop -ment	Developer	AZ 400K: water = 1:4	MF26A	MF26A	MF26A	MF26A	SU-8 developer	AZ MIF 826
	Duration (s)	360	30	70	20	40	85	30
Rinsing	Solution	Water	Water	Water	Water	Water	IPA	Water

Table 13: UV lithography process of different photoresists.

Table 14: Adhesion capability of different photoresists onto glass substrate.

	Conditions	Withou	t primer	With primer		
Resists		In the air	In KCl solution	In the air	In KCl solution	
	AZ 9260	Yes	No	Unknown		
Positive	S 1805	No	No	Unknown		
	S 1828	No	No	Yes	Yes	
	maN 2405	No	No	Yes	Yes	
Negative	nLof 2070	No	No	Yes	No	
	SU8 2002	No	No	Yes	It depends	
Reversal	AZ 5214 E	Yes	No	Unknown		

Table 13 shows a summary of UV lithography processes of different photoresists. Table 14 presents the adhesion capability of different photoresists in various cases "without primer" or "with primer" onto glass substrate, three days in the air and another three days in 10⁻³M KCl solution. From this table, the liquid KCl aging is selective regarding to air aging. Except two resists of AZ family, most of the resists did not last on the substrate without primer treatment. However, after introducing the primer, most of them remained stable in air and liquid.

REFERENCES:

- [1] "AZ[®] 9200-Series," <u>https://www.microchemicals.com/products/photoresists/az_9260.html</u>.
- [2] "Dow[®]MICROPOSIT[™]S1800[™]," <u>http://www.capitolscientific.com/Dow-Electronic-Materials-</u> <u>MICROPOSIT-S1805-Positive-Photoresist-Multipurpose-g-Line-and-Broadba_2</u>.
- [3] "Adhesion promoter HMDS and diphenylsilanedio (AR 300-80)," <u>http://www.allresist.com/process-chemicals-adhesion-promoter-hmds-and-</u> <u>diphenylsilanedio/</u>.
- [4] "Photoresist adhesion and HMDS (hexamethyldisilazane) processing," <u>http://www.imicromaterials.com/index.php/technical/HMDS</u>.
- [5] "MCC primer 80/20," <u>http://microchem.com/products/images/uploads/Rev.1-</u> <u>MCC Primer_80-20.pdf</u>.
- [6] "HMDS," <u>https://www.microchemicals.com/products/adhesion_promotion/hmds.html</u>.
- [7] "ma-N 2400," http://microchem.com/PDFs_MRT/ma-N%202400%20overview.pdf.
- [8] "AZ® nLOF 2000 Serie," https://www.microchemicals.com/products/photoresists/az_nlof_2070.html.
- [9] "SU-8," <u>http://microchem.com/Prod-SU8_KMPR.htm</u>.

List of publications

Posters of Conference:

- Q. Zhang, M. Zhang, A. Pallandre, L. Djeghlaf, and A-M. Haghiri-Gosnet, "Integration of a miniaturized electronic interface for a lab-on-a-chip bearing micro-fluidic transistors," 19th Journées Nationales du Réseau Doctoral en Micro-nanoélectronique (JNRDM), Toulouse, France, 2016.
- 2. Q. Zhang, M. Zhang, A. Pallandre, L. Djeghlaf, and A-M. Haghiri-Gosnet, "Lab-on-a-chip bearing a micro-fluidic transistor for surface state biasing," *11th Colloque National du Groupement de Recherche (GdR) System-on-Chip & System-in-Package (SoC-SiP)*, Nantes, France, 2016.
- 3. Q. Zhang and M. Zhang, "Lab-on-a-chip bearing a micro-fluidic transistor for surface state biasing," 20th Journées Nationales du Réseau Doctoral en Micro-nanoélectronique (JNRDM), Strasbourg, France, 2017.
- 4. Q. Zhang, A. Pallandre, A-M. Haghiri-Gosnet, and M. Zhang, "Characterizations of polarizable interface CNx adhering to different sticking underlayers in micro-fluidic device," 13th Colloque National du Groupement de Recherche (GdR) System on Chip Systèmes embarqués et Objets Connectés (SoC2), Paris, France, 2018.
- 5. Q. Zhang, L. Djeghlaf, M. Zhang, A. Pallandre, and A-M. Haghiri-Gosnet, "Integration of polarizable CNx microelectrodes in a microfluidic flow-FET device," 44th International Conference on Micro and Nanoengineering (MNE), Copenhagen, Denmark, 2018.

Article Review:

 Q. Zhang, M. Zhang, L. Djeghlaf, J. Bataille, J. Gamby, A-M. Haghiri-Gosnet, and A. Pallandre, "Logic digital fluidic in miniaturized functional devices : Perspective to the next generation of microfluidic lab-on-chips," *Electrophoresis*, vol. 38, pp. 953-976, 2017.

Résumé

Les examens médicaux et les diagnostics se basent souvent sur de l'analyse de traces à partir de mélanges biologiques plus ou moins complexes. Les méthodologies qui sont employées nécessitent ou nécessiteraient des traitements d'échantillons multiplexés suivis de séparations à haute résolution en amont des étapes de détection visant l'identification-quantification de biomarqueurs. L'électrophorèse est une technique puissante permettant de séparer des biomarqueurs présents dans les liquides biologiques. L'électrophorèse de zone libre transporte des molécules en milieu liquide sous l'influence de deux contributions : la mobilité électrophorétique directement liée au rapport poids/charge des molécules séparées et la mobilité électroosmotique (EOF), qui n'est que le mouvement du liquide provoqué par la migration des ions du tampon. C'est ce dernier flux EOF qui permet d'optimiser la résolution analytique de la séparation et donc de simplifier le mélange avant sa détection. La plupart du temps, les analystes modulent le flux EOF en ajustant le pH de la solution, ou en modifiant la force ionique du tampon ou en utilisant simplement des traitements de surface (monocouches auto-assemblées, surfactants, polymères, matériaux sol-gel, etc.). Toutes ces méthodes visent à ajuster l'état de charge électrostatique de l'interface à l'intérieur du canal microfluidique tout en réussissant parfois une réduction de l'adsorption non spécifique des analytes. Cependant, ces stratégies ne permettent pas d'ajuster en temps réel la charge de surface qui est directement reliée au flux EOF. Notre transistor microfluidique, qui possède une interface polarisable diélectrique peut contrôler dynamiquement le flux EOF. Ce concept repose sur une modulation en temps réel du potentiel zêta au niveau de l'interface solide/électrolyte avec une tension de l'ordre du volt en intégrant deux électrodes de grille externes, permettant un ajustement analogique de l'EOF et ceci indépendamment du champ transverse électrophorétique. Le carbone amorphe azoté (CNx avec x = 15% mol/mol) a été choisi comme matériau polarisable diélectrique. Comme le CNx ne peut pas être déposé directement sur un substrat de verre à cause de sa faible adhérence, deux matériaux différents ont été proposés comme couche d'accroche : le carbure de silicium (SiC) et le platine (Pt). Dans ce travail, nous avons étudié le comportement de films de CNx déposés sur ces deux matériaux différents et pour des architectures différentes. Nous avons observé une faible adhésion du CNx sur le SiC (les couches minces en CNx se sont rapidement décollées dans l'électrolyte liquide). Par contre, le Pt s'est révélé être une bonne couche d'accroche pour le CNx. Nous avons prouvé que certaines architectures hybrides incluant du Pt dans la couche d'accroche sont incroyablement robustes. Même après deux mois dans une solution millimolaire de KCl, le CNx adhérait toujours au verre sans aucune trace de délamination. Cependant le Pt étant un excellent conducteur, ce type de couche d'accroche peut alors court-circuiter l'électrolyte liquide sur plusieurs centaines de microns annulant ainsi tous les bénéfices du transistor fluidique. Pour donc éviter toute perte faradique dans l'électrolyte liquide ou vers les circuits conducteurs du dispositif, nous avons développé une architecture hybride intégrant des blocs isolants polymères aux deux extrémités du transistor. Nous pensons que cette architecture « couche d'accroche isolée/couche électriquement polarisable/électrodes de grille enterrées/polymère » constitue le transistor fluidique existante le plus robuste. En effet, la génération précédente atteignait péniblement une durée de vie d'une dizaine de jours. A l'issue de ces travaux, nous pensons être en mesure de proposer un composant fluidique complexe et robuste qui permet une modulation en temps réel de la charge de surface lors de migrations électrophorétiques.

CNx déposé sur SiC couche d'accroche diélectrique

Nous avons d'abord étudié le comportement du film de CNx déposé sur la couche d'accroche diélectrique de SiC. Nous avons effectué plusieurs expériences sur le processus de fabrication afin d'améliorer leur adhésion. La vue en coupe transversale du transistor fluidique fabriqué total est illustrée à la Figure 1. La fabrication consiste en trois fois de lithographie UV, de dépôt et de lift-off.



Figure 1: La vue en coupe transversale du transistor fluidique fabriqué total.

Les résultats des expériences ont montré que pour obtenir une meilleure adhérence, le procédé de fabrication devait être le suivant: 20s piranha etching en surface de SiC avant le dépôt de CNx, 200W et 0,4 Pa comme puissance de pulvérisation et pression de gaz pour les paramètres du dépôt, et sans recuit après le dépôt. Nous avons également réalisé une mesure de la modulation du EOF basée sur cette architecture, comme illustré à la Figure 2. Même si elle a été arrêtée en raison de fuites de courant.



Figure 2: La courbe de mesure de la modulation du EOF en fonction de la tension de grille dans un électrolyte de 10⁻³M KCl.

La fenêtre de polarisabilité de cette architecture a également été mesurée (voir la Figure 3). On peut voir que toutes les courbes sont asymétriques, ceci est dû à la nature différente des réactions électrochimiques qui se produisent à l'anode et à la cathode.



Figure 3: La fenêtre de polarisabilité du film CNx déposée sur la couche d'accroche SiC.

Les deux pics apparaissent dans le rouge et le bleu foncé indique la réduction du dioxygène. Les raisons peuvent venir de deux possibilités. Le premier est la dissolution de l'oxygène gazeux dans la solution de KCl non saturée d'argon. Le second est la présence de O dans le film CNx, ce qui peut être démontré à la Figure 4. Cette apparence de O et le rapport indésirable C/N peuvent être dus à la contamination de la chambre et/ou de la cible de la machine de dépôt. Cela peut affecter l'adhésion entre la couche d'accroche SiC et la couche polarisable CNx.



Figure 4: La courbe analysée par XPS sur carbone 1s, azote 1s et oxygène 1s.

CNx déposé sur Pt couche d'accroche métallique

En raison du dépôt de CNx sur Pt qui a démontré une capacité d'adhésion durable (6 mois à l'air et 2 mois dans solution de KCl sans dégradation du CNx), nous avons choisi le Pt comme la couche d'accroche. En raison de sa propriété conductrice, afin d'éviter tout court-circuit électrique à travers cette couche d'accroche métallique, nous avons conçu et fabriqué une série d'échantillons.



Figure 5: La vue en coupe transversale de l'architecture CNx à deux couches.

La Figure 5 illustre l'architecture CNx à deux couches. Comme son nom l'indique, il existe deux couches de CNx. La première inférieure fonctionne comme une couche isolante pour isoler la couche d'accroche conductrice et les deux électrodes à grille. Le second supérieure sert de couche polarisable.



Figure 6: La fenêtre de polarisabilité du film CNx de l'architecture CNx à deux couches.

Nous n'avons effectué qu'une seule mesure de sa fenêtre de polarisabilité, comme le montre la Figure 6. Nous pouvons le voir, elle nous a fourni une plage symétrique allant de -1 à + 1V. Cependant, comme le film de CNx était plus grand que la couche d'accroche, la zone dans laquelle le CNx et le substrat de verre en contact s'est détachée pas à pas et a entraîné des fuites de courant. Ainsi, une nouvelle architecture avec deux barres isolantes intégrées aux extrémités de la couche polarisable centrale a été conçue et fabriquée comme le montre la Figure 7.



Figure 7: La vue en coupe transversale de l'architecture à deux barres isolantes.

Cette architecture à deux barres nous a fourni une fenêtre de polarisabilité plus grande et plus symétrique allant de -1,5 à +1,5 V par rapport à celles précédentes (voir la Figure 8). De plus, il n'y a plus de décollement du film CNx du substrat du transistor dans l'air.



Figure 8: La fenêtre de polarisabilité du film CNx de l'architecture à deux barres isolantes.

En résumé, cette thèse comprend un grand nombre d'études significatives suivies d'expériences de vieillissement et de caractérisations. Il met en évidence la possibilité d'effectuer une modulation efficace du EOF via un dispositif PI-FFET pendant l'électrophorèse. Malheureusement, le travail de thèse a une durée limitée et nous avons trouvé tardivement un moyen d'introduire des barres en polymère isolant, mais cette étape supplémentaire a conduit à une contamination de la CNx surface (voir la Figure 9).



Figure 9: La vue en coupe transversale de l'architecture à barres isolantes en polymère.

Néanmoins, la recherche d'une autre polymère ou l'utilisation du RIE comme étape finale doit être évaluée. Nous savons également que plusieurs cycles de polarisation de l'interface avant toute séparation peuvent améliorer l'état de surface de CNx, c'est une autre perspective possible. Nous pensons que cette architecture hybride "couche d'accroche isolée/couche électriquement polarisable/électrodes de grille enterrées/polymère sera le transistor polarisable existant le plus robuste pour une adhérence forte et à long terme sur des substrats en verre. Des caractérisations chimiques supplémentaires doivent être effectuées à chaque étape du processus de microfabrication. Nous devons protéger la couche CNx de toute contamination éventuelle qui limite l'évolution chimique de cette interface cruciale.